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Signalling strategies for osteogenic differentiation of human umbilical cord mesenchymal stromal cells for 3D bone tissue engineering

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Abstract

Human umbilical cord mesenchymal stromal cells (hUCMSCs) have recently shown the capacity to differentiate into multiple cell lineages in all three embryonic germ layers. The osteogenic differentiation of hUCMSCs in monolayer culture has been reported, while the differentiation in three-dimensional biomaterials has not yet been reported for tissue-engineering applications. Thus, the aim of this study was to evaluate the feasibility of using hUCMSCs for bone tissue engineering. hUCMSCs were cultured in poly(L-lactic acid) (PLLA) scaffolds in osteogenic medium (OM) for 3 weeks, after which the scaffolds were exposed to several different media, including the OM, a mineralization medium (MM) and the MM with either 10 or 100 ng/ml insulin-like growth factor (IGF)-1. The osteogenic differentiation was confirmed by the up-regulation of *Runx2* and *OCN*, calcium quantification and bone histology. Switching from the OM to the MM promoted collagen synthesis and calcium content per cell, while continuing in the OM retained more cells in the constructs and promoted higher osteogenic gene expression. The addition of IGF-1 into the MM had no effect on cell proliferation, differentiation and matrix synthesis. In conclusion, hUCMSCs show significant potential for bone tissue engineering and culturing in the OM throughout the entire period is beneficial for osteogenic differentiation of these cells. Copyright © 2009 John Wiley & Sons, Ltd.

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Keywords umbilical cord stroma; stem cells; osteogenesis; IGF-1

1. Introduction

Bone tissue engineering is a promising interdisciplinary field, in which cells can be integrated into biomaterials to provide a substitute for bone grafts. Indeed, human bone marrow mesenchymal stromal cells (hBMSCs) have been translated into clinical trials via a tissue-engineering approach to treat bone defects successfully in a 7 year clinical trial (Quarto *et al.*, 2001; Marcacci *et al.*, 2007). However, there are some known disadvantages associated

with hBMSCs, such as the relative number of hBMSCs in the marrow, a limited proliferation ability and inferior differentiation potential in aged individuals (Mueller and Glowacki, 2001). Moreover, the invasive and painful harvesting procedure may cause donor site morbidity and complications (Lee *et al.*, 2007).

Recent evidence has shown that human umbilical cord mesenchymal stromal cells (hUCMSCs) are a primitive and multipotent stromal population that shares similar characteristics with hBMSCs (Can and Karahuseyinoglu, 2007; Troyer and Weiss, 2008). hUCMSCs are isolated from the Wharton's jelly of umbilical cords, a tissue routinely discarded after delivery. They are non-haematopoietic cells that can adhere to plastic surfaces for *in vitro* expansion and have many surface markers

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that are identical to those of hBMSCs, such as CD73, CD90, and CD105 (Wang *et al.*, 2004; Sarugaser *et al.*, 2005; Lu *et al.*, 2006; Fu *et al.*, 2006; Karahuseyinoglu *et al.*, 2007; Campard *et al.*, 2008). They are multipotent, differentiating along a variety of cell lineages in all germ layers, such as chondrocytes, osteoblasts, adipocytes, myocytes, neurons and hepatocytes (Wang *et al.*, 2004; Sarugaser *et al.*, 2005; Lu *et al.*, 2006; Fu *et al.*, 2006; Karahuseyinoglu *et al.*, 2007; Campard *et al.*, 2008). Apart from the similarity to hBMSCs, hUCMSCs have a number of particular advantages over hBMSCs, such as extensive availability and supply, no donor site morbidity, fast proliferation and great *in vitro* expansion ability, similar to other fetal stem cells. All of these features render hUCMSCs attractive for tissue engineering as a mesenchymal stromal cell (MSC) source.

hUCMSCs have demonstrated their osteogenic differentiation in two-dimensional (2D) monolayer culture after exposure to chemical signals containing dexamethasone and β -glycerophosphate (Wang *et al.*, 2004; Sarugaser *et al.*, 2005; Lu *et al.*, 2006; Karahuseyinoglu *et al.*, 2007; Wu *et al.*, 2007; Baksh *et al.*, 2007) and osteoinductive biomaterials such as demineralized bone matrix (Honsawek *et al.*, 2006). However, most studies regarding osteogenic differentiation of hUCMSCs are reported briefly in a qualitative way, with histological stains such as Alizarin red S and von Kossa (Wang *et al.*, 2004; Sarugaser *et al.*, 2005; Lu *et al.*, 2006; Karahuseyinoglu *et al.*, 2007; Wu *et al.*, 2007; Baksh *et al.*, 2007). In addition, osteogenic differentiation of hUCMSCs in three-dimensional (3D) biomaterials *in vitro* is scarcely explored in the literature, with only one study using an osteoinductive material, polycaprolactone tricalcium phosphate (Zhang *et al.*, 2008). In our group, we have previously shown that osteogenic differentiation can be achieved in polyglycolic acid (PGA) scaffolds, although the rapid degradation rate of PGA led to a loss of cells and construct integrity (unpublished data). Like PGA, poly(L-lactic acid) (PLLA) has been extensively investigated in tissue-engineering applications, with good biodegradability, biocompatibility and mechanical properties, but is more slowly degraded. This slower degradation is more desirable *in vitro*, although the ideal degradation rate *in vivo* may lie somewhere between PGA and PLLA degradation rates. In a phosphate-buffered saline (PBS) solution at 37 °C, quenched PGA demonstrated a rapid decrease in mass after 10 days (Hurrell and Cameron, 2001), while in another study (Yuan *et al.*, 2002) PLLA meshes had almost no loss of mass after 35 weeks in the same buffer. Therefore, non-woven PLLA meshes were used in the current study as support for cell growth and bone formation during the *in vitro* osteogenesis of hUCMSCs.

The majority of bone tissue engineering studies using BMSCs have been conducted with an osteogenic medium (OM) throughout the entire culture period (up to 6 weeks) (Yoshimoto *et al.*, 2003; Meinel *et al.*, 2004), although osteogenic differentiation of BMSCs can be accomplished in 2–3 weeks, with extensive mineralization (Jaiswal *et al.*, 1997; Pittenger *et al.*, 1999; Sumanasinghe *et al.*,

2008). However, the differentiation factors, including dexamethasone and $1\alpha,25$ -dihydroxyvitamin D₃, may inhibit cell proliferation (Walsh *et al.*, 2001; Atmani *et al.*, 2003; Chen, 2004; Kim *et al.*, 2006) for both BMSCs and osteoblasts. Moreover, it is unknown how the OM affects differentiated MSCs. Thus, in the current study, we cultured hUCMSCs with the OM in slowly degrading PLLA scaffolds for 3 weeks, and then removed osteogenic components (dexamethasone and vitamin D₃) to expose pre-differentiated hUCMSCs to a mineralization medium (MM) and an insulin-like growth factor (IGF)-1-containing MM for an additional 3 weeks. The negative and positive controls were none or continued exposure to osteogenic components, respectively. The goal of this study was to examine *in vitro* osteogenesis with both qualitative and quantitative data and to determine the effects of the medium shift on osteogenically induced hUCMSCs.

2. Materials and methods

2.1. Isolation and culture of hUCMSCs

IRB approval was obtained for human umbilical cord collection and hUCMSC isolation from KU-Lawrence (No. 15402) and the KU Medical Center (No. 10951). In this study, two human umbilical cords (both female, 15 and 23 cm long) were first cut into 3–5 cm segments, from which vessels were then removed. Cord segments were cut into 1–2 mm³ pieces and incubated at 37 °C in 0.75 mg/ml type II collagenase (298 U/mg; Worthington Biochemical; Lakewood, NJ, USA). A 5 h incubation yielded a homogeneous gelatinous solution, which was then diluted (1 : 8) in sterile phosphate-buffered saline (PBS). hUCMSCs were obtained by centrifugation and then resuspended in an expansion medium containing low-glucose Dulbecco's modified Eagle's medium (DMEM-LG; Invitrogen, Carlsbad, CA, USA), 10% MSC-qualified fetal bovine serum (FBS; Stem Cell Technologies, Vancouver, BC, Canada) and 1% penicillin/streptomycin (PS; Invitrogen). Cells were plated in cell culture flasks at 8000 cells/cm², expanded to 80–90% confluence (recorded as P0 cells) and detached by 1 × trypsin (Invitrogen). Following a previously described procedure (Wang *et al.*, 2008a), P0 cells were cryogenically stored in liquid nitrogen at –196 °C for future use.

2.2. Scaffold preparation, cell seeding and differentiation

hUCMSCs were thawed and expanded in the expansion medium to P4 for cell seeding. Cylinder-shaped scaffolds ($n = 83$), 5 mm in diameter and 2 mm in thickness, were cut out of non-woven PLLA meshes (>95% porosity and 45–55% crystallinity; Biomedical Structures, Warwick, RI, USA). The scaffolds were sterilized in a sterile pouch, using ethylene oxide, and then placed in a fume hood.

Before seeding, scaffolds were wetted with sterile-filtered ethanol followed by two PBS washes, and then immersed for 1 day in the expansion medium. P4 hUCMSCs were resuspended in the expansion medium and then seeded at 25×10^6 cells/ml of scaffold into PLLA scaffolds, using an orbital shaker at 150 rpm according to a previously described protocol (Wang *et al.*, 2008b). The expansion medium was referred as to the control medium (CM) over the following culture period. After a 2 day seeding period (week 0), some of the scaffolds were continuously cultured in the CM and the remaining ones were cultured in the OM by replacing the CM with 1.5 ml OM, consisting of the CM supplemented by 100 nM dexamethasone (DEX; Sigma, St. Louis, MO, USA), 5 mM β -glycerophosphate (β -GP; Sigma), 10 nM $1\alpha,25$ -dihydroxyvitamin D3 (VD3; Biomol International, Plymouth Meeting, PA, USA) and 50 μ g/ml ascorbic acid 2-phosphate (AA2P; Sigma). After 3 weeks there were five different culture conditions: (a) continue culture in the CM; (b) continue culture in the OM; (c) change culture from the OM to the MM, which consisted of the OM without DEX and VD3; (d) change culture from the OM to the MM with 10 ng/ml IGF-1 (I10); or (e) change culture from the OM to the MM with 100 ng/ml IGF-1 (I100). 1 ml medium was changed every other day, except for the complete replacement at weeks 0 and 3.

2.3. Biochemical assays

Constructs ($n = 4$) were homogenized in 1.2 ml papain solution (120 μ g/ml) and then incubated at 60 °C overnight. A PicoGreen kit (Invitrogen) was used to determine DNA contents, according to the manufacturer's protocol. A hydroxyproline (HYP) assay was used to obtain HYP content, using a previously described protocol (Wang *et al.*, 2008a). A conversion factor of 8.5 pg DNA/cell was used to convert DNA content to cell number, and a conversion factor of 11.5 can be used to convert HYP mass to collagen mass, based on our preliminary studies.

Calcium content was quantified by an OCPC (*ortho*-cresolphthalein complex one) method as described in the literature (ter Brugge and Jansen, 2002). Constructs ($n = 4$) were homogenized and suspended in 1 N acetic acid (Sigma) overnight. 50 μ l of this culture sample or a standard solution (0–100 mg/ml CaCl_2 ; Sigma) was added into 250 μ l of working solution. The working solution contained 0.05 mg/ml OCPC solution (1 mg/ml OCPC, 0.0063 N KOH and 0.0031 N acetic acid; Sigma), 0.74 M ethanolamine/boric acid buffer, pH 11 (Sigma) and 2% 8-hydroxyquinoline (5 g in 100 ml 95% ethanol; Sigma). This mixture was incubated at room temperature for 10 min and then read at 575 nm.

2.4. Histology

Frozen sections (10 μ m, $n = 2$) were used for histological analysis. Alizarin red S and von Kossa staining were used

to visualize the mineralization. Sections were fixed in 10% phosphate-buffered formalin for 20 min and then rinsed in ultrapure water before staining. For Alizarin red S staining, sections were incubated with 2% Alizarin red S reagent, pH 4.1–4.3 (Sigma) for 5 min. For von Kossa staining, sections were incubated with 1% silver nitrate solution (Sigma) under ultraviolet light for 20 min and then with 5% sodium thiosulphate (Sigma) for 5 min to remove unreacted silver. Finally, all sections were rinsed in ultrapure water and dehydrated through graded alcohols (95% and 100%, twice each).

2.5. RNA isolation and real-time RT–PCR

Total RNA was extracted from cells using 1 ml Trizol reagent (Invitrogen), following the manufacturer's instructions ($n = 4$). Total RNA concentration and purity were determined on a spectrophotometer (Nanodrop; Wilmington, DE, USA). The mRNA samples were then converted to cDNA using a high-capacity cDNA archive kit (Applied Biosystems, Foster City, CA, USA), following the supplier's procedure. TaqMan gene expression assay kits (Applied Biosystems) were used for transcript levels of type I collagen (*CI*), runt-related transcription factor 2 (*Runx2*), and osteocalcin (*OCN*), using a real-time reverse transcriptase polymerase chain reaction (RT–PCR) in an Applied Biosystems 7500 system. TaqMan gene expression assay kits (Applied Biosystems) were Hs00164004_m1 for *CI*, Hs00231692_m1 for *Runx2*, Hs01587813_g1 for *OCN* and Hs99999905_m1 for glyceraldehyde 3-phosphate dehydrogenase (*GAPDH*). A $2^{-\Delta\Delta\text{Ct}}$ method was used to evaluate relative the mRNA expression level for each target gene (Livak and Schmittgen, 2001). Briefly, ΔCt values were obtained by the difference between the Ct values of target genes and the *GAPDH* gene. They were then normalized by subtracting the ΔCt value of the calibrator sample, their respective Ct values in the CM groups, to obtain $\Delta\Delta\text{Ct}$ values.

2.6. Statistical analysis

All data were expressed as means \pm one standard deviation (SD) and analysed by one-way ANOVAs, followed by Tukey's Honestly Significant Difference *post hoc* tests. Statistical significance was determined by a statistical threshold of $p < 0.05$.

3. Results

3.1. Cell number

Over the 6 week culture period, cell number decreased in all groups ($p < 0.05$) compared to week 0 (Figure 1). Despite the cell loss throughout the culture period, the OM groups at weeks 3 and 6 retained 1.67 and 1.50 times more cells in the constructs than the CM groups,

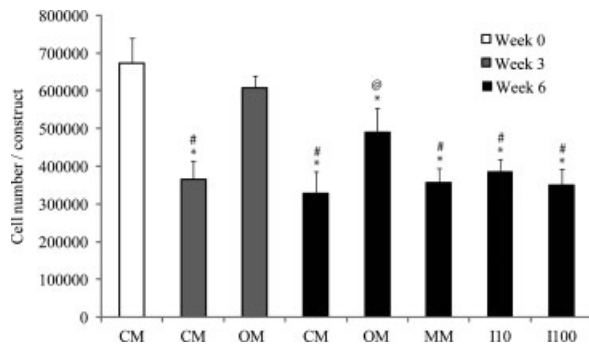


Figure 1. Cell number per construct ($n = 4$). CM, control medium; OM, osteogenic medium; MM, mineralization medium; I10, MM containing 10 ng/ml IGF-1; I100, MM containing 100 ng/ml IGF-1. Cell number decreased with time, while the OM group retained more cells than other groups at each time-point. *Statistically significant difference ($p < 0.05$) from week 0. #Statistically significant difference ($p < 0.05$) from the OM group at weeks 3 or 6. @Statistically significant difference ($p < 0.05$) in the OM group between weeks 3 and 6. Error bars represent standard deviation (SD). A conversion factor of 8.55 pg DNA/cell was used to convert DNA content to cell number

respectively ($p < 0.05$). During weeks 0–3, the cell number decreased by 46% in the CM group ($p < 0.05$), while only decreasing by 10% in the OM group, without statistical significance. In contrast, during weeks 3–6, the cell number decreased in the CM group only by 10% without statistical significance, while decreasing by 19% in the OM group ($p < 0.05$). The medium change at week 3 (from OM to MM, I10, and I100) caused a decrease in cell number ($p < 0.05$) and there were no significant

differences in cell number between the MM, I10 and I100 groups.

3.2. HYP content

In all groups except the CM group, the HYP content per construct and per cell increased over time, with a substantial leap during weeks 0–3 ($p < 0.05$) (Figure 2A, B). In the CM groups, the HYP content per construct did not vary over the 6 week culture period and the HYP content per cell had a slight increase, without statistical significance. The OM group had 4.2 and 3.5 times more HYP per construct than the CM group at weeks 3 and 6, respectively ($p < 0.05$), and had 2.5 and 2.4 times more HYP per cell than the CM group at weeks 3 and 6, respectively ($p < 0.05$). The shift from OM to MM, I10 or I100 did not affect the total HYP content per construct, while this change did lead to an upregulation of HYP synthesis, given that the HYP content per cell was approximately 50% greater in the MM, I10 and I100 groups compared to the OM group at week 6 ($p < 0.05$). Like the cell number, HYP synthesis was not influenced by the addition of IGF-1 into the MM.

3.3. Calcium content

There was a considerable increase in calcium content per construct and per cell with time in all groups over the culture period ($p < 0.05$) (Figure 2C and 2D). Calcium deposition was also observed in the CM group, albeit at

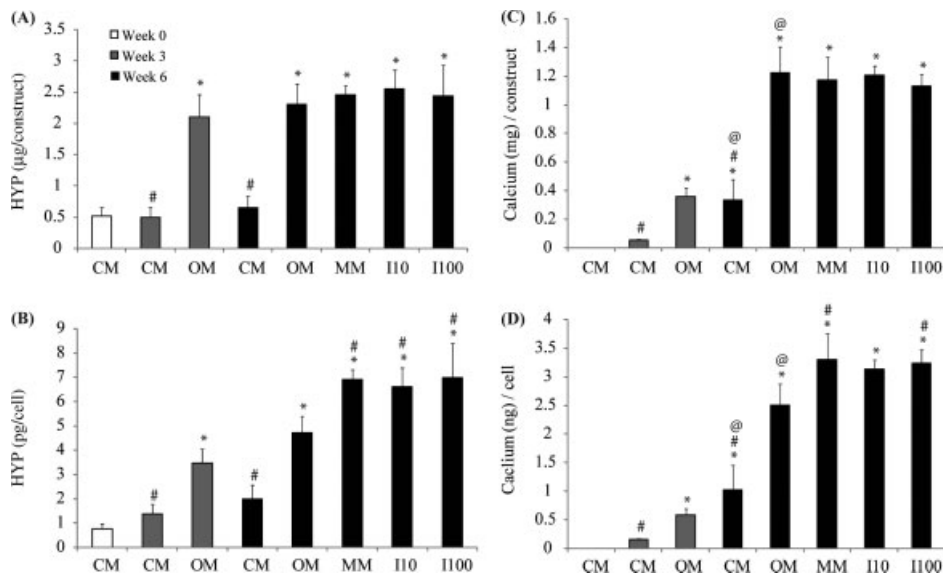


Figure 2. Hydroxyproline (HYP) content per construct (A) and per cell (B) and calcium content per construct (C) and per cell (D) ($n = 4$). CM, control medium; OM, osteogenic medium; MM, mineralization medium; I10, MM containing 10 ng/ml IGF-1; I100, MM containing 100 ng/ml IGF-1. (A, B) The OM group had a substantial increase in HYP content per construct and per cell during weeks 0–3 and the CM group had less HYP content than the other groups. The OM group had a comparable HYP content per construct (A) to the MM and IGF groups, while it had less HYP per cell than the MM and IGF groups (B). (C, D) The calcium content per construct and per cell increased over time in all groups and the OM group had more calcium than the CM group. The MM and I100 groups had more calcium per cell than the OM group, while the calcium per construct was comparable among them. *Statistically significant difference ($p < 0.05$) from week 0. #Statistically significant difference ($p < 0.05$) from the OM group at weeks 3 or 6. @Statistically significant difference ($p < 0.05$) between weeks 3 and 6. Error bars represent SD

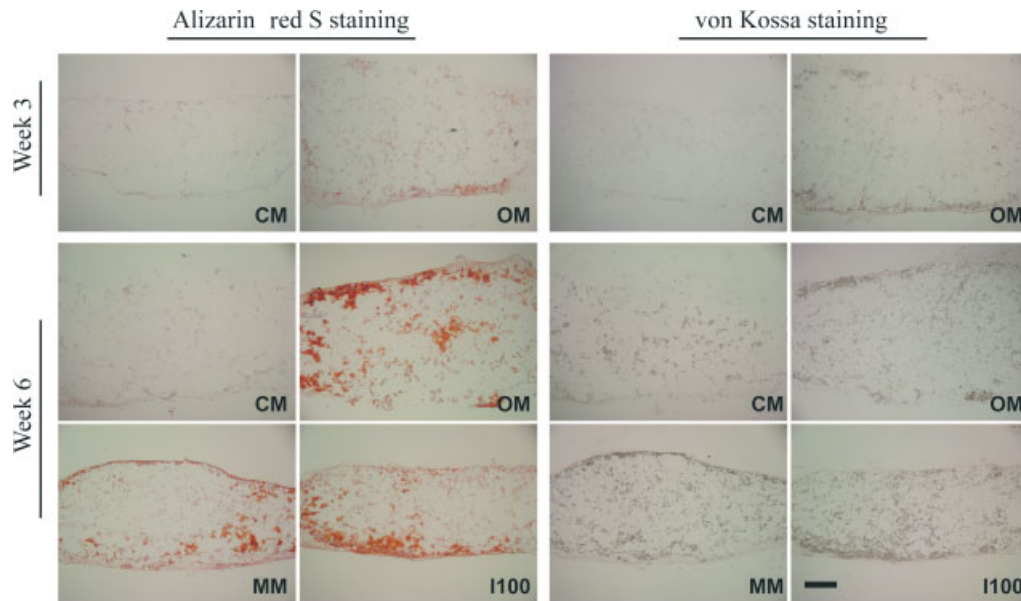


Figure 3. Alizarin red S staining and von Kossa staining at 3 and 6 weeks ($n = 2$). CM, control medium; OM, osteogenic medium; MM, mineralization medium; and I100, MM containing 100 ng/ml IGF-1. Both types of staining revealed positive mineralization with time. Note that the peripheral area in the constructs had stronger staining than the central area. Scale bar = 500 μm

a low level. However, the OM group did exhibit more calcium per construct and per cell than the CM group at weeks 3 and 6 ($p < 0.05$). At week 6, there was no significant difference in calcium content per construct among the OM, MM, I10 and I100 groups, while the MM and I100 groups had 1.32 and 1.29 times more calcium content per cell than the OM group, respectively ($p < 0.05$). No significant differences were observed in calcium content per cell among the MM, I10 and I100 groups.

3.4. Histology

Alizarin red S staining was consistent with von Kossa staining, both of which revealed a positive mineral deposition that increased with time (Figure 3). The CM groups had weaker staining than the OM groups, which was consistent with the calcium quantification. It must be noted that there was a stronger staining at the peripheral area of the constructs than inside the constructs. There were no discernible differences among the OM, MM and I100 groups.

3.5. Gene expression levels of type I collagen (CI), Runx2 and osteocalcin (OCN)

Runx2 and *OCN* gene expression was upregulated in the OM group ($p < 0.05$) (Figure 4). There were no statistically significant differences in *CI* gene expression among all groups. After a change from the OM, the MM group had a lower gene expression of *CI*, *Runx2* ($p < 0.05$) and *OCN* when compared to continuing treatment with the OM medium. The addition of IGF-1 into the MM did

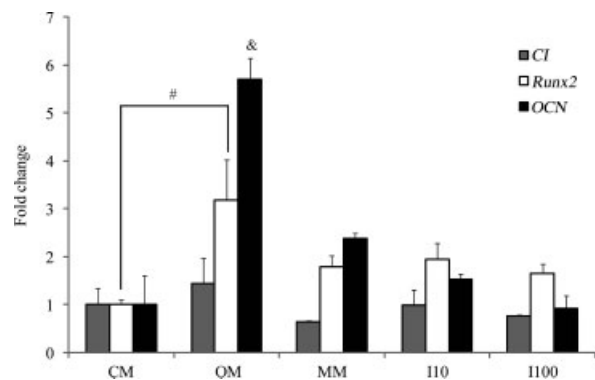


Figure 4. Gene expression (normalized to the CM group) for type I collagen (*CI*), runt-related transcription factor 2 (*Runx2*) and osteocalcin (*OCN*) at week 6 ($n = 4$). CM, control medium; OM, osteogenic medium; MM, mineralization medium; I10, MM containing 10 ng/ml IGF-1; I100, MM containing 100 ng/ml IGF-1. The OM group had higher *Runx2* and *OCN* mRNA levels than the other groups. # Statistically significant difference in *Runx2* gene expression between the OM and CM groups ($p < 0.05$). & Statistically significant difference in *OCN* gene expression between the OM group and all other groups ($p < 0.05$). Error bars represent SD

not statistically affect the gene expression level of *Runx2*, *OCN* or *CI*.

4. Discussion and conclusion

In the field of tissue engineering, it is critical to select a promising cell source that is easy to obtain and provides sufficient cell numbers. hUCMSCs undoubtedly meet these requirements. There is an abundant supply of umbilical cords, with 4.1 million births in the USA alone in 2005 (Martin *et al.*, 2007). After cell isolation,

hUCMSCs can achieve a 300-fold cell increase in seven passages while maintaining differentiation potential (Karahuseyinoglu *et al.*, 2007). *In vivo* transplantation of these cells has demonstrated their regenerative effects on brain injuries and retinal disease in animal models, while immunorejection was not observed in these studies (Jomura *et al.*, 2007; Lund *et al.*, 2007). Previous osteogenic differentiation studies with hUCMSCs have been mainly performed in monolayer (2D) (Wang *et al.*, 2004; Sarugaser *et al.*, 2005; Lu *et al.*, 2006; Karahuseyinoglu *et al.*, 2007; Wu *et al.*, 2007; Baksh *et al.*, 2007). In the current study, we investigated the osteogenesis of hUCMSCs *in vitro* in a 3D biomaterial-based environment, and the effects of different media on osteogenic differentiation, in order to evaluate the use of hUCMSCs for bone tissue engineering.

The *Runx2* gene is known to play an essential role in osteoblast differentiation and bone formation (Ducy *et al.*, 1997; Schroeder *et al.*, 2005). The disruption of *Runx2* leads to the termination of intramembranous and endochondral ossification, due to the maturational arrest of osteoblasts (Komori *et al.*, 1997). The *in vitro* osteogenic differentiation of MSCs is accompanied by the upregulation of *Runx2* gene expression at the early stage (Tou *et al.*, 2003). The *OCN* gene is mainly expressed by mature osteoblasts and is responsible for mineralization at the late stage of differentiation. Exposed to the OM, hUCMSCs did show an upregulation of the gene expression of *Runx2* and *OCN* compared to the CM group, indicating osteogenic differentiation of these cells. Compared to the MM, I10 and I100 groups, the OM is also beneficial for osteogenic differentiation due to the higher *Runx2* and *OCN* gene expression. The positive staining of Alizarin red S and von Kossa confirmed the presence of mineralization, suggesting that the hUCMSCs were progressing along an osteogenic lineage. In contrast to mineralization, collagen content increased mainly between weeks 0–3 and was maintained between weeks 3–6. In native normal bone, the nucleation and development of mineral crystals interacts principally with collagen (Landis, 1999). The abundant collagen production may have contributed to the boost of mineralization between weeks 3 and 6.

The OM also promoted cell proliferation and/or inhibited cell loss compared to other media. This effect was mainly due to the presence of DEX and VD3 in the OM, rather than AA2P and β -GP, based on the observation that the MM group had a comparable cell number range with the CM group after switching the medium at week 3. A few studies have demonstrated an inhibitory effect of either DEX or vitamin D3 on cell proliferation (Walsh *et al.*, 2001; Murata *et al.*, 2004; Campbell *et al.*, 1997), although they can induce osteogenic differentiation (Jaiswal *et al.*, 1997; Partridge *et al.*, 1980; Beresford *et al.*, 1980). In monolayer culture, we also observed in a previous study that DEX inhibited hUCMSC proliferation (unpublished data). Thus, the increase in cell number with the OM group in the current study indicated that the combination of DEX and VD3 might have a synergistic

effect on hUCMSC proliferation and/or survival. It must be noted that this stimulation decreased with time, and might reach a plateau in cell number similar to the CM group after a longer culture period, which would be of interest for future investigation.

The MM had no impact on the total collagen and calcium content in the constructs, although these had slightly higher collagen and calcium per cell. Moreover, the shift from the OM to the MM led to a decrease in osteogenic gene expression, including *CI*, *Runx2* and *OCN*. IGF-1 plays an important role as an anabolic agent in bone development at all stages (Linkhart *et al.*, 1996; Ross *et al.*, 1993; Kasukawa *et al.*, 2004) and regulates MSC proliferation and biosynthesis (Jeong *et al.*, 2008; Koch *et al.*, 2005). In the current study, the addition of IGF-1 into the MM had no beneficial effects on cell proliferation, matrix production or gene expression. In the future, the incorporation of IGF-1 at an earlier stage and/or in addition to osteogenic signals, as opposed to in lieu of them, might facilitate the osteogenic differentiation of MSCs (Koch *et al.*, 2005).

In summary, the results demonstrated the osteogenic differentiation of hUCMSCs in PLLA scaffolds, with the upregulation of bone-specific genes and mineral deposition, thus supporting the feasibility of applying hUCMSCs to bone tissue engineering. Therefore, given the numerous advantages over adult stem cells and the successful osteogenesis in 3D biomaterials, hUCMSCs may be a promising alternative for bone tissue engineering. A side-by-side comparison between hUCMSCs and fibroblasts or osteoblasts will be interesting and meaningful to further evaluate the potential of hUCMSCs in bone tissue engineering. In the current study, there was no advantage to removing DEX and VD3 after 3 weeks, as in fact the only group to retain these factors (i.e. the OM group) produced a greater number of cells and expressed the highest level of osteogenic genes. Future strategies may include earlier introduction of IGF-1 and/or extended exposure of DEX and VD3.

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