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Introduction

Magnetic resonance imaging (MRI), computed tomography (CT) imaging and ultrasound (US) imaging are the most important imaging techniques in clinical medicine. It is well known that MRI is a noninvasive imaging technique and fit for the tumor diagnosis of internal organs, for example, liver, lung, breast, etc. With the use of MRI contrast agents, some tumors could be early diagnosed. During the past two decades, superparamagnetic iron oxides have attracted a great deal of attention due to their important application as MRI contrast agents.¹–⁷ Recently, molecular imaging, diagnostics and therapy based on nanomaterials have become a promising field, which would have potential applications in clinical diagnostics and therapy for cancer.⁸⁻¹⁰ In particular, MRI contrast agents have been developed towards multimodal imaging and multifunction for imaging and therapy. For example, Gd@Fe₃O₄, PLA@- $Fe₃O₄$ and $Fe₃O₄(\text{a}Au)$ have been investigated as $T₁$ and T_2 -weighted MRI, MRI-US and MRI-CT dual-mode imaging contrast agents, respectively.¹¹⁻¹⁴ Moreover, Fe₃O₄@Au could also be used as MRI contrast agents and photothermal therapy agents.¹⁵–¹⁷ Furthermore, when MRI contrast agents were coupled with photosensitizers, they could be used as

Multifunctional Fe₃O₄–TiO₂ nanocomposites for magnetic resonance imaging and potential photodynamic therapy

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Multifunctional Fe₃O₄–TiO₂ nanocomposites with Janus structure for magnetic resonance imaging (MRI) and potential photodynamic therapy (PDT) were synthesized, in which Fe₃O₄ was used as a MRI contrast agent and TiO₂ as an inorganic photosensitizer for PDT. Their morphology, structure, and MRI and PDT performance were characterized, respectively. Moreover, the location of $Fe₃O₄$ –TiO₂ nanocomposites in MCF-7 cells was also investigated by the staining of Prussian blue and alizarin red, respectively. The results showed that the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites had good T₂-weighted MRI performance, and the MCF-7 cells incubated with nanocomposites could be killed under the irradiation of UV light. Compared with traditional organic photosensitizers, TiO₂ inorganic photosensitizers could have more stable PDT performance due to their nanoscale size and anti-photodegradable stability. Therefore, the as-prepared Fe₃O₄–TiO₂ nanocomposites could have potential applications as a new kind of multifunctional agent for both MRI and PDT. PAPER
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photodynamic therapy (PDT) agents under light excitation with some specific wavelength.¹⁸⁻²⁰ Therefore, in order to realize the real-time imaging and in situ therapy for cancer, it was very interesting to develop a multifunctional agent of MRI and PDT.

Generally, most of the photosensitizers are organic macromolecules or complexes used in PDT.²¹⁻²³ However, they could have a short maintenance time in the body, and they might be decomposed under no light irradiation. It is well known that $TiO₂$ nanoparticles are a kind of typical inorganic photosensitizer, which have been widely used as a photocatalyst in environmental sciences. Under the excitation of UV light, the lightinduced electrons and holes of $TiO₂$ nanocrystals with anatase structure will be divided, and then the contamination could be degraded. Furthermore, $TiO₂$ nanoparticles could also be used as a PDT agent in biomedical fields. Under the irradiation of UV light, the free radicals and singlet oxygen produced by $TiO₂$ nanoparticles could produce light toxicity and then destroy the tissues and cancer cells.^{24,25} Moreover, TiO₂ nanoparticles could be maintained for a longer time in the body than that of traditional organic photosensitizers, and they were nontoxic and stable under no light irradiation. Few investigations have also been reported about the application of $TiO₂$ nanoparticles as inorganic photosensitizers for PDT.²⁵–³²

Therefore, the MRI performance of $Fe₃O₄$ and the inorganic PDT performance of $TiO₂$ nanoparticles were very useful for the development of a multifunctional agent of MRI and PDT. In the process of diagnosis and therapy, UV light was brought into the location of cancer cells using an UV fiber. Then using an

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on-operation MRI technique, the real-time MRI and in situ PDT could be realized. Therefore, the $Fe₃O₄$ -TiO₂ nanocomposites would have important applications in the MRI and PDT of cancer in future.

In this paper, multifunctional $Fe₃O₄$ -TiO₂ nanocomposites were synthesized, which could be used as a multifunctional agent of MRI and inorganic photosensitizers for PDT. The morphology, microstructure, and magnetic property of $Fe₃O₄$ $TiO₂$ nanocomposites were characterized by transmission electron microscopy (TEM), high-resolution transmission electron microscopy (HRTEM) with energy dispersed X-ray spectroscopy (EDS), X-Ray Diffraction (XRD) and the physical performance measurement system (PPMS). Moreover, the MRI and PDT performances were investigated by MR imaging, relaxivity and the methylthiazol tetrazolium (MTT) assay method. Furthermore, using the staining of Prussian blue and alizarin red, respectively, the location of $Fe₃O₄-TiO₂$ nanocomposites in MCF-7 cells was also observed by using a biomicroscope and a laser scanning confocal microscope. Nanoscale

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Experimental

a Preparation of $Fe₃O₄$ -TiO₂ nanocomposites

In this experiment, ferric acetylacetonate $(Fe (acac)₃)$ and tetrabutyl titanate (TBOT) were used as reaction agents, and oleic acid (OA), oleylamine (OM), n-octyl alcohol and ethanol were used as solvents and dressing agents. All agents were purchased from Aladdin Ltd.

 $Fe₃O₄$ -TiO₂ nanocomposites were synthesized by the solvent-thermal method. First, $TiO₂$ nanoparticles with about 5– 10 nm were synthesized based on the previously reported method. 33 Then the as-prepared TiO₂ nanoparticles were centrifuged and washed with ethanol three times, and were redispersed in *n*-hexane. Next, 0.5 mmol of $Fe (acac)₃$ were dissolved in 4 mL of OM and 12 mL of n-octyl alcohol, and 1 mmol of $TiO₂$ nanoparticles dispersed in *n*-hexane were dropped into the above $Fe (acac)_3$ solution. The mixtures were being stirred for 4 h, and then the temperature was increased to 70 \degree C in order to evaporate the n-hexane. Finally, they were cooled to room temperature, and were transferred into a reaction kettle. The reaction temperature was kept at 240 \degree C, and the time was 2 h. Finally, the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites were centrifuged, washed with ethanol 3 times, and were dispersed into the water phase by PEG coating.

b UV irradiation

First, MCF-7 cells were seeded in a 96-well plate, and then incubated with $Fe₃O₄$ -TiO₂ nanocomposites. Finally, the MTT assay method was used to investigate the cell viability pre- and post-UV irradiation at different times. The power density of UV light was 25 mW $\rm cm^{-2}$, and the distance between the UV light and cells was 20 cm. The concentrations of $Fe₃O₄$ -TiO₂ nanocomposites were 50, 100, 150 and 200 μ g mL $^{-1}$, respectively, and the incubation time of $Fe₃O₄$ -TiO₂ nanocomposites in MCF-7 cells was about 24 h. When they were incubated for 6 h, UV irradiation was carried out, and the irradiation time was

5 min, 10 min, and 15 min, respectively. Furthermore, as control, MCF-7 cells without $Fe₃O₄$ -TiO₂ nanocomposites were also irradiated by UV light with the time of 5 min, 10 min, and 15 min, respectively.

c Staining of cells

Prussian blue and alizarin red dyes were used respectively for the staining of MCF-7 cells. The first part is Prussian blue staining of MCF-7 cells incubated with $Fe₃O₄$ -TiO₂ nanocomposites. The concentration of nanocomposites was 100μ g mL^{-1} , and the incubation time was 24 h. The procedure for Prussian blue staining was followed according to previous articles.^{34,35} The second part is alizarin red staining. The $Fe₃O₄$ $TiO₂$ nanocomposites were stirred with alizarin red solution for 8 h, and then they were centrifuged and washed with water three times. Finally, they were re-dispersed in PBS buffers. The concentration of nanocomposites was 100 μ g mL⁻¹, and the incubation time was 4 h.

d Characterization

The morphology, microstructure and magnetic property of the as-prepared Fe₃O₄-TiO₂ nanocomposites were characterized by using a Tecnai F20 transmission electron microscope (TEM) with EDS accessory, a Bruker AXS D8 X-Ray Diffractometer and Quantum Design Model-9 PPMS. The MR imaging and relaxivity performance of $Fe₃O₄$ -TiO₂ nanocomposites were tested by using a Siemens Avanto MRI scanner system with a magnetic field of 1.5 T and a Mico MR Analyzing system (Shanghai Niumag Corporation) with a magnetic field of 0.47 T, respectively. Finally, based on MCF-7 cells, the cell viability of the asprepared $Fe₃O₄$ -TiO₂ nanocomposites pre- and post-UV irradiation was characterized by the MTT assay method, and the location of nanocomposites in MCF-7 cells was also investigated using the staining of Prussian blue and alizarin red dyes by using a biomicroscope and a Leica laser scanning confocal microscope, respectively.

Results and discussion

Fig. 1 shows the TEM, HRTEM and EDS images of the asprepared $Fe₃O₄$ -TiO₂ nanocomposites. As shown in Fig. 1(a), the dispersity of $Fe₃O₄$ –TiO₂ nanocomposites was good, and the $Fe₃O₄$ -TiO₂ nanocomposites did not have a core-shell structure. Closer observation of Fig. 1(b) reveals that most of the $Fe₃O₄$ -TiO₂ nanocomposites had a Janus structure, and the single size of the $Fe₃O₄$ -TiO₂ nanocomposites was about 30-40 nm. In Fig. 1(c), the HRTEM image of $Fe₃O₄$ -TiO₂ nanocomposites shows that $Fe₃O₄$ was coupled with $TiO₂$ nanoparticles to form a Janus structure. Moreover, the interplanar distance of two parts was 0.2518 nm and 0.3517 nm, respectively, which corresponded well with the (311) plane of $Fe₃O₄$ and the (101) plane of TiO₂, respectively. Fig. 1(d) shows the EDS spectrum of the $Fe₃O₄$ -TiO₂ nanocomposite. The peaks of C, Cu, O, Fe, and Ti elements could be found, in which the elements of C and Cu were from a copper grid with carbon

Fig. 1 TEM, HRTEM and EDS images of $Fe₃O₄–TiO₂$ nanocomposites. (a and b) TEM; (c) HRTEM; (d) EDS.

films, and the elements of Fe, O and Ti were from the $Fe₃O₄$ -TiO₂ nanocomposite.

The crystal structure and magnetic property of the asprepared Fe₃O₄-TiO₂ nanocomposites were also characterized. Fig. 2(a) shows the XRD spectra of $Fe₃O₄$, TiO₂ and $Fe₃O₄$ –TiO₂ nanocomposites. It could be observed that the peaks of $Fe₃O₄$ $TiO₂$ nanocomposites included the peaks of Fe₃O₄ with cubic structure and the peaks of $TiO₂$ with anatase structure. Fig. 2(b) shows the M-H curves of $Fe₃O₄$ and $Fe₃O₄$ -TiO₂ nanocomposites. The results showed that the as-prepared $Fe₃O₄$ and $Fe₃O₄$ –TiO₂ nanocomposites had superparamagnetism, and the saturation magnetization of $Fe₃O₄$ and $Fe₃O₄$ -TiO₂ nanocomposites was 58.95 and 14.90 emu g^{-1} , respectively.

The MRI performance of the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites was characterized by using a Siemens Avanto MRI scanning system with a magnetic field of 1.5 T. Fig. 3 shows the T_1 - and T_2 -weighted MR images of Fe₃O₄–TiO₂ nanocomposites. From left to right, the Fe concentrations were 0, 0.2, 0.4, 0.8, 1.2, 1.6 and 2 mM, respectively. As shown in Fig. 3(b), the T_2 weighted MR images of $Fe₃O₄$ -TiO₂ nanocomposites were darker, compared with the MR image of water. Moreover, by increasing the concentration of $Fe₃O₄$ -TiO₂ nanocomposites, the MR images got darker and darker. However, in Fig. 3(a), the T_1 -weighted MR images were not changed obviously, compared with that of water. Therefore, the results indicated that the asprepared Fe₃O₄–TiO₂ nanocomposites have good T_2 -weighted MRI performance.

In order to further quantitatively analyze the MRI performance, the MR relaxation properties of $Fe₃O₄$ -TiO₂ nanocomposites were investigated by using a MR analyzing system with a magnetic field of 0.47 T (Shanghai Niumag Micro MR). By MR relaxivity measurement of $Fe₃O₄$ –TiO₂ nanocomposites with different concentrations, the longitudinal and transverse relaxivities (*i.e.* r_1 and r_2 values) of Fe₃O₄–TiO₂ nanocomposites could be calculated. Fig. 4(a) and (b) show the plots of $1/T_1$ and $1/T_2$ versus concentrations of the as-prepared Fe₃O₄-TiO₂ nanocomposites. By calculation, the r_1 and r_2 values of Fe₃O₄-TiO₂ nanocomposites were 1.444 and 54.691 mM⁻¹ s⁻¹, respectively. Because the ratio of r_2/r_1 values was more than 3, the as-prepared Fe₃O₄-TiO₂ nanocomposites had good T_2 weighted MR performance, which also corresponded to that of MR images.

Using the staining method of cells, the location of nanocomposites in cells could be observed and analyzed. In this work, MCF-7 cells were incubated with $Fe₃O₄$ -TiO₂ nanocomposites, which were stained by Prussian blue and alizarin red, respectively. The concentration of $Fe₃O₄$ -TiO₂ nanocomposites was 100 $\mu\text{g}\,\text{mL}^{-1}$, and the incubation time in MCF-7 cells was 24 h and 4 h for the staining of Prussian blue and alizarin red, respectively. Fig. 5 shows the photomicrographs of MCF-7 cells stained by Prussian blue without and with the incubation of $Fe₃O₄$ -TiO₂ nanocomposites. As shown in Fig. 5(a), the MCF-7 cells stained by Prussian blue were not blue when they were not incubated with $Fe₃O₄$ -TiO₂

Fig. 2 XRD spectra and M–H curves of $Fe₃O₄$ –TiO₂ nanocomposites. (a) XRD spectra; (b) M–H curves.

Fig. 3 T_1 - and T_2 -weighted MR images of Fe₃O₄–TiO₂ nanocomposites. (a) T_1 -weighted MR images; (b) T_2 -weighted MR images. Imaging parameters for the FLASH sequence were TR = 600 ms, TE = 7 ms for T_1 and TR = 3000 ms, TE = 90 ms for T_2 , respectively.

nanocomposites. However, as shown in Fig. 5(b), with the incubation of $Fe₃O₄$ –TiO₂ nanocomposites, the colour of MCF-7 cells stained by Prussian blue was blue, which indicated that most of the $Fe₃O₄$ –TiO₂ nanocomposites had entered into MCF-7 cells. In Fig. 5(c), some $Fe₃O₄$ -TiO₂ nanocomposites and their clusters could be observed obviously in the cytoplasm of the labeled cells.

Fig. 6 shows the confocal microscopy images of MCF-7 cells stained by alizarin red without and with the incubation of $Fe₃O₄$ –TiO₂ nanocomposites. Fig. 6(a)–(c) show the images of

Fig. 4 Longitudinal (a) and transverse (b) relaxivities of $Fe₃O₄$ -TiO₂ nanocomposites.

the cell nucleus, alizarin red, and the overlap of the cell nucleus and alizarin red, respectively. In Fig. 6(b) and (c), a red image could not be observed around the cell nucleus, which indicated that the alizarin red dyes could not be stained on the cells when they were not coupled with $Fe₃O₄$ -TiO₂ nanocomposites. However, when MCF-7 cells were incubated with $Fe₃O₄$ -TiO₂ nanocomposites coupled with alizarin red dyes, $Fe₃O₄$ -TiO₂ nanocomposites could be located in the cytoplasm of the labeled cells, as shown in Fig. 6(e) and (f). The results of staining of cells by Prussian blue and alizarin red dyes showed that the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites could be located easily in the MCF-7 cells, which indicated that they had good biocompatibility.

Furthermore, under the irradiation of UV light with different time, the cell viability of MCF-7 cells incubated with $Fe₃O₄$ -TiO₂ nanocomposites was also investigated using MTT assay method. The incubation time of $Fe₃O₄$ -TiO₂ nanocomposites in MCF-7 cells was 24 h, and the concentrations of $Fe₃O₄$ -TiO₂ nanocomposites were 50, 100, 150, and 200 $\rm \mu g \, \rm m L^{-1},$ respectively. As shown in Fig. 7(a), before they were irradiated by UV light, the cell viability was more than 90%, when the concentration of Fe₃O₄–TiO₂ nanocomposites was less than 100 μ g mL $^{-1}$, and the cell viability was still more than 85% when the concentration was between 100 and 200 $\mu{\rm g}\,{\rm mL}^{-1}.$ The results showed that the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites had low cytotoxicity when the incubation time of nanocomposites was 24 h. However, when they were irradiated under UV light for 5 min, 10 min, and 15 min, respectively, it could be observed that the cell viability had decreased obviously with the increase of irradiation time. Moreover, under the irradiation of UV light, the concentration of $Fe₃O₄$ -TiO₂ nanocomposites had an important influence on the cell viability of MCF-7 cells. When the

Fig. 5 Photomicrographs of MCF-7 cells stained by Prussian blue. (a) Control; (b and c) MCF-7 cells incubated with $Fe₃O₄$ -TiO₂ nanocomposites.

concentration of $Fe₃O₄$ -TiO₂ nanocomposites was less than 100 μ g m L^{-1} , the cell viability was not obviously decreased, both pre- and post-irradiation. However, when the concentration was more than 100 μ g mL $^{-1}$, the MCF-7 cells could be killed obviously under the irradiation of UV light. In Fig. 7, when the concentration of Fe $_{3} \mathrm{O}_4\text{--TiO}_2$ nanocomposites was 200 $\mu\mathrm{g\,mL}^{-1},$ it could be observed that the cell viability of pre-irradiation was about 85%, but was only about 55%, 49%, and 39% at the irradiation time of 5 min, 10 min and 15 min, respectively. Furthermore, the influence of UV light irradiation on the cell viability of MCF-7 cells was also investigated, when they were not incubated with $Fe₃O₄$ –TiO₂ nanocomposites. Fig. 7(b) shows the cell viability of control MCF-7 cells, when the irradiation time of UV light was 0 min, 5 min, 10 min and 15 min, respectively. It could be observed that the cell viability was still more than 90%, compared with that of control MCF-7 cells without UV irradiation. The results indicated that $Fe₃O₄$ -TiO₂ nanocomposites were critical for determination of cell viability under UV light

Fig. 6 Confocal microscopy images of MCF-7 cells stained by alizarin red. (a-c) Control; (d-f) MCF-7 cells incubated with $Fe₃O₄$ -TiO₂ nanocomposites.

irradiation. Moreover, the suitable concentration of $Fe₃O₄$ –TiO₂ nanocomposites and the irradiation time of UV irradiation were very important for the PDT performance. Therefore, the $Fe₃O₄$ - $TiO₂$ nanocomposites could be good inorganic photosensitizers for PDT in therapy for cancer in the future.

Based on the above results, the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites with Janus structure could be good MRI and PDT agents. The Janus structure could be important for the performance improvement of $Fe₃O₄$ -TiO₂ nanocomposites. On one hand, the Janus structure could maintain the magnetism of $Fe₃O₄$ –TiO₂ nanocomposites because the $Fe₃O₄$ magnetic part was not coated by $TiO₂$ nanoparticles, which could improve the MRI performance of $Fe₃O₄$ -TiO₂ nanocomposites. On the other hand, under the irradiation of UV light, the light-induced electrons and holes of $Fe₃O₄$ -TiO₂ nanocomposites with coreshell structure could be easily recombined, which would decrease the yield of free radicals and singlet oxygen.³⁶ However, due to the small interface between $Fe₃O₄$ and $TiO₂$ nanoparticles in Janus structure, the recombination of light-induced electrons and holes would be decreased, which could enhance the PDT efficiency. Furthermore, compared with traditional photosensitizers based on organic macromolecules or complexes, TiO₂-based inorganic photosensitizers had a longer

Fig. 7 Cell viability before and after UV light irradiation. (a) MCF-7 cells incubated with Fe₃O₄-TiO₂ nanocomposites; (b) MCF-7 cells without Fe₃O₄-TiO₂ nanocomposites.

maintenance time in the body and a more stable performance based on their nanoscale size. Therefore, the as-prepared $Fe₃O₄$ –TiO₂ nanocomposites would be an excellent multifunctional agent of MRI and PDT and could have potential applications in the diagnosis and therapy of cancer in the future.

Conclusions

Using the MRI performance of $Fe₃O₄$ nanoparticles and the PDT performance of $TiO₂$ inorganic photosensitizers under the excitation of UV light, $Fe₃O₄-TiO₂$ nanocomposites could be used as a multifunctional agent of MRI and PDT. In this paper, $Fe₃O₄$ –TiO₂ nanocomposites with Janus structure were synthesized. The size of the Janus $Fe₃O₄$ -TiO₂ nanocomposites was about 30–40 nm, and the r_2 value was about 54.691 mM $^{-1}$ s $^{-1}$. Moreover, under the irradiation of UV light, the cell viability incubated with $Fe₃O₄$ –TiO₂ nanocomposites could be decreased from about 85% to 39%, compared with that without UV irradiation. Furthermore, the as-prepared $Fe₃O₄$ -TiO₂ nanocomposites could be located easily in MCF-7 cells. Therefore, the Janus $Fe₃O₄$ -TiO₂ nanocomposites could have potential applications as a multifunctional agent of MRI and PDT for the diagnosis and therapy of cancer in the future.

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