Thermoluminescent Phosphors for Radiation Dosimetry

B.C. Bhatt^a and M.S. Kulkarni^b

Radiological Physics and Advisory Division Bhabha Atomic Research Centre, Mumbai, India ^abcbhatt2003@yahoo.com (corresponding author), ^bkmukund@barc.gov.in

Keywords: Thermoluminescence, OSL, RPL, Radiation Dosimetry, TL Phosphors, Tissue Equivalent, Dose Response, TL Sensitivity

Abstract. The use of thermoluminescence (TL) as a method for radiation dosimetry of ionizing radiation has been established for many decades and has found many useful applications in various fields, such as personnel and environmental monitoring, retrospective dosimetry, medical dosimetry, space dosimetry, high-dose dosimetry. Method of preparation, studies and applications of thermoluminescence (TL) dosimetric materials are reviewed. Several high sensitivity thermoluminescent dosimeters (TLDs) are now commercially available in different physical forms. These commercial TL dosimeters comply with a set of stringent requirements stipulated by the International Electrotechnical Commission (IEC). Specific features of TL phosphors for thermal neutron, fast neutron and high-energy charged particle (HCP) dosimetry are also considered. Some of the recent developments in the field of optically stimulated luminescence (OSL) and radiophotoluminescence (RPL) are also summarized. Comparative advantages of TL, OSL and RPL dosimeters are given. Results of recent studies of TL in nanosized materials are briefly presented. Future challenges in this field are also discussed.

Contents of Paper

- 1. Introduction
- 2. Basic Thermoluminescence Process
- 3. Thermoluminescence Dosimetry
- 4. Preparation of TLD materials and their Characterization
	- 4.1 Lithium Fluoride
		- 4.1.1 LiF:Mg,Ti
		- 4.1.2 LiF: Mg,Cu,P
	- 4.2 Lithium Tetraborate
	- 4.3 Magnesium Borate
	- 4.4 Other Lithium-, Sodium- and Potassium-based Compounds
	- 4.5 Magnesium Orthosilicate-based TL Phosphors
	- 4.6 CaSO4:Dy/Tm TL Phosphors
	- 4.7 Calcium Fluoride $(CaF₂)$
	- 4.8 Al_2O_3 based TL Phosphors
	- 4.9 BeO-based TL Phosphor
	- 4.10 BaSO4:Eu TL Phosphor
	- 4.11 TL of Nanophosphors
	- 4.12 Phosphors based on Other Luminescence Techniques
- 5. Important Areas of Radiation Dosimetry
	- 5.1 Personnel Monitoring
	- 5.2 Environmental Dosimetry
	- 5.3 Neutron Dosimetry
	- 5.4 Dosimetry in Medical Applications of Radiation
	- 5.5 Retrospective Dosimetry
	- 5.6 High Dose Dosimetry
	- 5.7 Space Dosimetry
- 6. Summary
	- References

1. Introduction

The phenomenon of thermoluminescence (TL) has been known for a long time. In 1663 Robert Boyle reported to the Royal Society on the observation of the glow from a diamond when warmed in dark. In 1904, Marie Curie reported the ability of the mineral fluorite to exhibit TL after being exposed to a radium source. Further experimental and theoretical work was carried out by Urbach [1] in 1930, Randall and Wilkins [2] and Garlick and Gibson [3] developed TL models in 1945 and 1948, respectively, which allowed quantitative calculations of thermoluminescence kinetic parameters. Initially, the dosimetry measurements were dominated by ionization chamber measurements and photographic film until resurgence of techniques based on luminescence and other solid state techniques [4]. It is now about 60 years since Farrington Daniels and his research group at the University of Wisconsin (USA) first suggested the use of thermoluminescence (TL) as a technique in radiation dosimetry [5] through studies of LiF as a TL material and it became evident that the desirable properties of the material were the result of the interplay between the complex defects present within the material resulting from the presence of Mg and Ti. This realisation emerged from the work of Cameron and colleagues [6, 7] and this work led eventually to the patenting of TLD-100 by the Harshaw Chemical Company in 1963. Daniels and co-workers also investigated TL properties of $A₁₂O₃$ for its possible use in radiation dosimetry [8]. A TL peak at 236 ^oC depends on sodium impurity and the TL area increases in an approximately linear manner with concentration of sodium ion present as an impurity. All these developments in the field of thermoluminescence dosimetry, in the initial years, till mid 1970s, were also influenced by the pioneering work of Leverenz [9], Curie [10], Aitken [11, 12] and others, and International Conferences on Thermoluminescence and Luminescence Dosimetry held in 1965 [13], 1968 [14, 15], 1971 [16], and 1974 [17].

2. Basic Thermoluminescence Process

When ionizing radiation is incident on an insulating crystal some of the deposited energy is stored in the lattice at defect sites, colour centres, etc. Upon heating the crystal, this stored energy is released and a fraction of it may be emitted as visible light (prior to onset of black-body radiation at higher temperatures, i.e. > 250 °C). This is called thermoluminescence. Within certain limitations, the amount of light emitted is proportional to the radiation dose previously absorbed by the TL material.

Figure 1 gives schematic representation of thermally stimulated luminescence phenomena in an insulating or semiconducting material assuming one trap-one recombination centre model. The absorption of energy from an ionizing radiation source by an insulating or semiconducting material causes the excitation of free electrons and holes and subsequent trapping of these electronic species at defects (trapping states) or metastable states within the material. The subsequent absorption of thermal energy by the metastable trapped charge, say, electron, results in the stimulated relaxation of the system back to its equilibrium condition. During the relaxation process recombination of the

electronic charge with the trapped hole (recombination centre) occurs, and if the recombination is radiative, luminescence is emitted.

Fig. 1 A simple model of the thermoluminescence process: (a) Irradiation with ionization radiation leads to generation of electrons and holes, and trapping of free electrons and holes; (b) Release of electrons from the traps upon heating or optical stimulation of the phosphor material and recombination at the luminescence centre leading to emission of light.

3. Thermoluminescence Dosimetry

In thermoluminescence dosimetry the relationship between the signal and the absorbed dose to be measured must be determined by an appropriate calibration.

Thermoluminescent Dosimeters (TLDs) have found increasing application with the progress made in the development of solid thermoluminescent dosimeters and instrumentation for reading them. Many TLD based systems are now commercially available, and are widely used in routine personal dosimetry, environmental monitoring and clinical radiation dosimetry. The extreme sensitivity of TL for detecting the presence of defects, as few as $10⁷$ within a specimen, is beneficial for detecting low radiation levels which are encountered in personal and environmental monitoring.

Thermoluminescent Dosimeters (TLDs) are increasingly accepted for radiation dosimetry for the following reasons:

- (a) The existence of nearly tissue equivalent thermoluminescent materials;
- (b) Sufficiently high sensitivity and accuracy for both personal and environmental monitoring;
- (c) Commercial availability as small sized solid detectors adaptable for both manual and automatic processing;
- (d) Suitability for beta skin and extremity dosimetry;
- (e) Availability of materials with excellent long term stability under varying environmental conditions;
- (f) Ease of processing;
- (g) Reusability;
- (h) Linearity of response with dose and dose rate over a wide range.

Some general characteristics of the most common thermoluminescent materials used for radiation protection dosimetry are listed in Table 1.

The effective atomic number Z_{eff} (see Table 1) is an indication of the material's energy response. Table 2 shows the photon energy response at 30 keV relative to that at 1.25 MeV for the TL phosphors The effective atomic number of LiF (8.14) is close enough to the value for tissue (Z_{eff} = 7.42) to make it tissue equivalent. Out of the materials given in Table 2, only beryllium oxide and lithium borate have lower values of Z_{eff} than tissue. However, unlike LiF:Mg,Ti, LiF:Mg,Cu,P has relative TL response less than 1 in the photon energy range 30 to 200 keV.

Table 2 Photon energy response at 30 keV relative to that at 1.25 MeV for phosphors with different $Z_{\rm eff}$

4. Preparation of TLD materials and their Characterization

There is a vast literature on the methods of preparation and characterization of TL phosphors [18, 19, 33-43]. In this section, some of these methods are discussed in brief.

TLD materials are prepared by adopting one of the following methods: (i) co-precipitation technique, (ii) solid-state diffusion method, (iii) recrystallization from solution, (iv) growing single crystals from melt, (v) Solution Combustion Synthesis (SCS) method, and (vi) sol-gel method.

In the co-precipitation technique, required amounts of chemical compounds along with trace amount of activator are added to form desired compound. The precipitated compound (after appropriate washing, drying of the product) is sintered at higher temperature to facilitate diffusion of activator and formation of appropriate number of defects in the crystallite material.

In the solid-state diffusion method, the desired materials are intimately mixed and the mixture so formed is sintered at higher temperature for the formation of compound as well as uniform dispersal of the activators in the lattice. Sometimes flux is used to lower the melting point of the compound thereby facilitating better incorporation of the activator.

In the re-crystallization from solution, appropriate amount of chemical compound along with the desired amount of activator are dissolved in a solvent and the solution thus formed is slowly evaporated to dryness to form the required TLD phosphor. CaSO4:Dy and CaSO4:Tm are prepared by this method [44].

Crystal growth from melt is the most popular method for growing single crystals of semiconductors, metals, oxides, halogenides and chalcogenides at large scale. It is classified further under four headings:

(i) Czochralski technique: This is one of the major melt-growth techniques. It is widely used for growing large-size single crystals for a wide range of commercial and technological applications. One of the main advantages of Czochralski method is the relatively high growth rate.

(ii) Bridgman technique: In this technique the crucible containing the molten material is translated along the axis of a temperature gradient in a furnace.

(iii) Verneuil Method: Verneuil method (also called flame fusion technique) is used to grow large quantity of crystals with high melting temperature. It was originally developed for producing synthetic gemstones. Now-a -days the technique is used to grow a variety of high-quality crystals such as corundum, spinel, rutile and strontium titanate, which are widely applied in laser devices and precision instruments, as well as in thin film technologies as substrates.

(iv) Kyropoulos Method: The Kyropoulos method was initially developed for growth of large alkali halide crystals by the German scientist Spyro Kyropoulos. Later large sapphire crystals were also grown by using this method. The main distinction between Kyropoulos and Czochralski is the different crystal shapes and the solid-liquid interface curvature.

Combustion synthesis has been proposed to prepare oxide-based phosphors of smaller size particles. This method involves a highly exothermic reaction between an organic fuel and metal salts (oxidizers) in an aqueous solution. The reaction is initiated at low temperatures (around 500 $^{\circ}$ C) and proceeds to completion in a few minutes. The peak reaction temperature depends on the fuel and oxidizer molar ratio.

Sol-gel technique: Sol-gel method is a chemical technique that uses metal alkoxides (a kind of metal-organic compounds) for synthesis and production of powder or ceramic samples through a series of chemical processes, including hydrolysis, gelation, drying, and thermal treatment.

4.1 Lithium Fluoride. Farrington Daniels and his research group at the University of Wisconsin (USA) first suggested the use of thermoluminescence (TL) as a technique in radiation dosimetry [5] through studies of LiF as a TL material and it became evident that the desirable properties of the material were the result of the interplay between the complex defects present within the material resulting from the presence of Mg and Ti. This realization emerged from the work of Cameron and co-workers [6, 7] and this work led eventually to the patenting of TLD-100 by the Harshaw Chemical Company in 1963. Since then it has been the most widely used TLD material for various applications, particularly for personnel and medical dosimetry. LiF:Mg,Ti dosimeters known as TLD-100, TLD-600, and TLD-700 depending on their preparation from natural lithium or lithium enriched with 6 Li or 7 Li, respectively.TLD-100 consists of Li in its natural abundance (7.5% 6 Li and 92.5% $\frac{7}{1}$, TLD-600 are prepared from pure lithium chemical compound enriched in

 6 Li (95.6% 6 Li and 4.4% 7 Li)), while TLD-700 are prepared by enriching the starting Li-compound in ${}^{7}Li$ (99.93% ${}^{7}Li$ and 0.07% ${}^{6}Li$). The book of McKeever et al. [19] and many other books and review articles describe preparation and properties of LiF dosimeters.

4.1.1 LiF:Mg,Ti. LiF:Mg,Ti dosimeters come in a variety of physical forms, including powder, hot pressed chips, extruded rods, powder embedded Teflon discs or single crystals. Among these the most popular form is probably the hot pressed chips available in the size $3.2 \times 3.2 \times 0.9 \text{ mm}^3$. These chips have been used for personnel monitoring as the TLD badge marketed by Harshaw Chemical company (presently known as Thermo Fisher Scientific) as well as by other commercial manufacturers of TLD personnel monitoring badges. These hot pressed chips are also widely used for medical physics applications.

Harshaw's patent [45] describes two preparation methods for LiF:Mg,Ti TL phosphor powders: the solidification method, and the single crystal method.

In the solidification method, lithium fluoride (10⁶ parts by weight), magnesium fluoride **(**400 parts by weight), lithium cryolite (200 parts by weight), and lithium titanium fluoride (55 parts by weight) are mixed in a graphite crucible. The mixture is homogeneously fused in vacuum and the product slowly cooled, then crushed and sieved between 60 and 200 µm.

The single crystal method consists of growth from the melt using either the Czochralski or Stockbarger-Bridgman methods and graphite crucibles using furnace having vacuum or inertatmosphere to grow single crystals. Powders may also be prepared from single crystals by pulverising and sieving between 60 and 200 µm.

Harshaw's patent also describes the preparation of extruded LiF dosimeters. To obtain them, the LiF powder mixture is placed in a neutral atmosphere and pressed at 3.5 x 10^8 Pa at a temperature of 700 °C, pushing the mixture with a piston through a hole which acts as a die. The bar, obtained in this way, is cut in sections to prepare pellets/chips of uniform thickness and finally the faces of the pellets are polished. The extruded dosimeters have identical TL characteristics as the TL phosphor powder (also described in the paper of Azorin et al. [41]). McKeever et al. [19] state that the most sensitive LiF:Mg, Ti material is obtained with approximately 180 ppm Mg^{2+} and 10 ppm Ti^{4+} .

Phosphor embedded PTFE (polytetrafluoroethylene) discs are prepared by mixing fine grains of phosphor (having grain size comparable to or less than that of PTFE powder) with PTFE powder, generally in the weight ratio of 1:3, followed by cold compaction and sintering at about a temperature of 390 \degree C for about 1hour. Alternatively, phosphor emddeded tape may be obtained from a sintered phosphor-PTFE billet from which TL detectors of suitable size and thickness could be obtained.

Another method is described by Portal [46] to prepare sodium stabilized LiF TL dosimeters by using 200 ppm of magnesium fluoride and 1-2 wt% of sodium fluoride.

Sources of LiF:Mg,Ti TLDs include Thermo Fisher Scientific (Harshaw), USA (powder, chips (3.2 x 3.2 x 0.9 mm³; 3.2 x 3.2 x 0.38 mm³), disk (dia. 4.5 mm x 0.8 mm) and rods (dia.1 mm x 6 mm), sold as TLD-100, TLD-600 or TLD-700, Rexon TLD Systems, Inc., USA (www.rexon.com) (in their website it is stated that Rexon is committed to ongoing suppy of TLD products and services pioneered by Teledyne and Victoreen, such as LiF:Mg,Ti (TLD-100, TLD-600 and TLD-700) powder, chips, disks and rods, PTFE/TLD products: disks, ultra thin (50 µm), low energy disks, rods (long, mini and micro), LiF:Mg, Ti (DTG-4, as sintered chips and in ${}^{6}Li$ and ${}^{7}Li$ versions) from Russia, LiF:Mg,Ti from Poland, Krakow: marketed as MTS-N, MTS-6 or MTS-7, depending upon the isotopic content of Li), having dia. 4.5 and 0.9 thickness. These dosimeters are also available as thin layer circular pellets (active layer 0.05 mm), micro cubes (1x1x1 mm³), rods or powder. Solid Dosimetric Detector & Method Laboratory (DML), Beijing, P.R. China offers a

broad spectrum of products: GR-100 series LiF:Mg,Ti with natural, Li-6 or Li-7 composition (www. chinadml.com); Mirion Technologies markets RADOS TLD dosimeters as well as those of Panasonic (TLD 802) and Harshaw TL dosimeters, including dosimetry systems (www.mirion.com); RadPro International GmbH, Germany (www.radpro-int.com) is a distributor of RADOS TLD systems and TLD material of Mirion Technologies and RADCARD (www.radcard.pl) (former TLD Poland). Table 3 gives details of LiF:Mg,Ti from different manufacturers.

Table 3 Details of LiF:Mg,Ti from different manufacturers.

Sensitization is a technique involving pre-irradiation and annealing which produces increased sensitivity in some thermoluminecent materials, such as $LiF:Mg$, Ti and $CaSO₄:Dy$. Additional benefits associated with sensitization such as extended linearity in the dose response curve, reduction in photon energy dependence and reduction in the dose threshold have been reported [55]. LiF:TLD-100 is observed to be up to six times more sensitive after exposure to $10³$ Gy gamma radiation followed by an annealing treatment at $280-300\degree$ C for 60 min. This increased sensitivity is eliminated if the material is subsequently annealed for an hour at 400° C. However, exposing sensitized LiF:Mg,Ti to ultraviolet (254 nm) radiation during annealing at 280-300 $^{\circ}$ C is reported to reduce background effects while maintaining increased sensitivity [55-57, 89]. Charles et al. [56] have indicated that by optimizing this procedure, reductions in dose thresholds of a factor of 2 to 3 can be achieved. Driscoll et al. [22] report to have obtained a sensitization factor of 4 by following simultaneous UV (254 nm) and thermal treatment (270-290 $^{\circ}$ C), however, no overall reduction in dose threshold was observed due to larger variation in the background signal of the samples.

However, they report that dose thresholds of about 10 μ Gy for GR-100M samples (having sensitization factor between 3 and 5) quoted by the manufacturer (Baoli Science and Technology Ltd, China) were confirmed by them. These results confirmed the trend of reduction in dose threshold following sensitization reported by Charles et al. [56]. Jones [58] investigated the comparative performance of sensitized and non-sensitized TLDs when mounted on identifiable plaques for automatic reading. Bhuwan Chandra et al. [59] reported that the PTTL (using 254 nm UV light) in the gamma irradiated (10^3 Gy) sample after subjecting to simultaneous UV and thermal treatment (UV/thermal annealed) persisted even after 4 h of bleaching and remained constant at the level equivalent to 0.53 Gy of $60C$ gamma ray dose. They also observed that the response of peak 5 as a function of UV exposure in UV/thermal sensitized and dark-sensitized LiF (TLD-100) samples were different. The difference in the nature of the two PTTL curves appeared to show that the centres responsible for the PTTL in UV/thermal bleached samples were different from those related to peak 10. Thus, these results cast some doubts on the re-estimation capability of UV/thermal sensitized LiF:Mg,Ti dosimeters. There is no published report on the use of sensitized LiF:Mg,Ti dosimeters for routine personnel or environmental monitoring.

4.1.2 LiF: Mg,Cu,P. The preparation of LiF:Mg,Cu,P phosphor was first reported by Nakajima et al. [60, 61]. Lithium fluoride of special grade was used as the material. This material was mixed in water with activators $CuF₂$ (0.05 mol%), MgCl₂ (0.2 mol%), and ammonium phosphate. The wet mixture in a platinum crucible was heated at 1050 $^{\circ}$ C for 30 min (melting point of LiF is 847 $^{\circ}$ C) in nitrogen gas atmosphere after being dried at about 80 $^{\circ}$ C for 4 h. The melted LiF material in the crucible was rapidly cooled to 400 $^{\circ}$ C during 30 min and the polycrystalline LiF:Mg,Cu,P is obtained. The phosphor was reported to have promising characteristics for use as a dosimeter. It was reported that the phosphor had TL sensitivity about 23 times that of LiF (TLD-600), a linear TL dose response in the range 50 µGy to 10 Gy, a TL emission spectrum in the range 340-410 nm and 5% TL fading in 30 days when stored at 40 $^{\circ}$ C. Wu et al. [62] prepared LiF:Mg,Cu,P phosphor powder by thermal treatment at 900 $^{\circ}$ C for 1h in N₂ atmosphere. Its TL sensitivity was reported to be about 23 times higher than that of LiF (TLD-100). Its TL response was linear from 0.3 mR to 1000 R. Its energy dependence is reported to be similar to that of LiF (TLD-100). The phosphor was reported to be stable and reusable without significant loss of sensitivity. Niwa et al. [63] prepared single crystals of LiF:Mg,Cu,P. It is reported that the TL emitted from a single crystal with 0.25 mole percent phosphorus was one order higher than that emitted from LiF powder sample with the same mole percent phosphorus and the same weight. They report that single crystals could not be grown with phosphorus content more than 0.25 mole percent in the starting/base material.

Wang et al. [64, 65] reported the development of special technology to prepare LiF:Mg,Cu,P TLD in the form of solid chips with high signal to noise ratio, which made it possible to apply these detectors in personnel, clinical and environmental monitoring. LiF:Mg,Cu,P was developed in powder as well as chip form. A special grade of LiF powder was mixed in water with different quantities of MgF₂, CuF₂, and NH₄H₂PO₄. The wet mixture was placed in a platinum crucible. After being dried at about 200 °C for 2 h, it was melted under a nitrogen stream in an electric furnace at 1050 °C for 30 min. The melted material in the crucible was rapidly cooled down to room temperature. The poly-crystallized LiF(Mg,Cu,P) material was powdered and washed with about 1N hydrochloric acid, then washed with distilled water until no chloride ions could be detected. Finally, it was dried at 100 °C for 1 h and was then sieved. Two methods have been used to produce LiF:Mg,Cu,P chips, i.e. hot pressed square chips and sintered circular chips. The dosimetric performances of sintered LiF:Mg,Cu,P chips (circular) are reported to be the same as those of hot pressed square chips, but the production cost of the former is much lower than that of the latter. It is reported [66] that solid chips of 6 LiF/ 7 LiF:Mg,Cu,P have been prepared in the same way. Thin films of LiF:Mg,Cu,P are also produced in Solid Dosimetric Detector & Method Laboratory (DML). All these developments and different methods used by several groups for the preparation of LiF:Mg,Cu,P have been summarized by Zha et al. [24]. Subsequently,

Shen et al. [67] reported that the main features of GR-200A have been improved dramatically by adding a chemical additive and adopting a particular preparation technology. It is reported that the sensitivity of GR-200A has been increased to 65 times as high as TLD-100 from the original 29 times. The residual signal has been decreased to less than 1% from the original of about 2.5% following the 240 $^{\circ}$ C readout. This led to decrease in detection threshold and increase in the signalto-noise ratio. Horowitz and Horowitz [68] used high-purity optical-grade LiF and other necessary salts as dopant and co-dopants to prepare a high sensitivity LiF:Mg,Cu,P TLD phosphor powder. The phosphor was prepared by melting in a nitrogen atmosphere at $1000 \degree C$. Incorporation of oxygen in the molten stage was stated to be absolutely necessary for obtaining high sensitivity phosphor in a reproducible manner.

Niewiadomski [47] reported the development of LiF:Mg,Cu,P (also known as MCP) phosphor powder and sintered pellets. It is also reported that the sintering procedure for the development of MCP pellets was different than that adopted for the development of sintered LiF:Mg,Ti (also known as MTS) pellets. These sintered pellets (circular) were named as MCP-N, MCP-6 or MCP-7, depending upon the isotopic content of Li. These MCP-type ultra-sensitive thermoluminescent dosimeters, available as solid detectors or powder, are 30 times more sensitive to gamma ray doses than MTS-N dosimeters (www.radcard.pl). Formerly known as TLD Poland, presently, these dosimeters are marketed as RADCARD dosimeters. Azorin et al. [41, 69] reported development of LiF:Mg,Cu,P TLD phosphor powder in ININ Mexico. In freshly precipitated pure LiF, aqueous solution of MgCl₂, CuF₂ and $(NH_4)_2HPO_4$ activators, in required concentrations, were added. The dried material was placed in platinum crucible and subjected to thermal treatment at 573 K for 15 min. The temperature was then raised to 973 K and maintained at this temperature for 1h., resulting in the formation of crystalline mass of LiF:Mg,Cu,P. The crystalline material was crushed and sieved to select phosphor powder with grain sizes between 100 and 300 µm. Its TL sensitivity is reported to be about 25 times than that of LiF:TLD-100. Its detection threshold was reported as 65 nGy and linearity in dose response in the range 100 µGy to 100 Gy. Kolotilin et al. [50] used a method similar to that reported by Nakajima et al. [60, 61] for the preparation of LiF:Mg,Cu,P phosphor powder. However, LiF:Mg,Cu,P solid dosimeters were prepared by compaction of powder and sintering, resulting in disks each of dia. 5 mm and 1 mm thickness. Table 4 gives a comparison of TL characteristics of various LiF phosphors prepared by different methods.

TL sensitivity of these LiF: Mg,Cu,P dosimeters was about 20 times higher than that of LiF:Mg,Ti (DTG-4). Its detection threshold was 0.14 mR (1.23 μ Gy) and showed linear response up to 500 R (4.38 Gy). Shinde et al. [70] purified the commercially available LR grade LiF by vacuum distillation method. The purified LiF and dopants Mg, Cu and P in the form of MgF₂, CuCl₂.2H₂O and $NH_4H_2PO_4$ respectively, were mixed thoroughly. The mixture was melted in a platinum crucible at 960 \degree C and quenched to room temperature. The polycrystalline phosphor was thus obtained. The following dopants concentrations were found to be optimum: Mg 0.4 mol%, Cu 0.02 mol%, P 0.85 mol%. Patil and Moharil [71] showed that LiF:Mg,Cu,P could be made using a simple procedure which did not involve use of nitrogen atmosphere and platinum crucible. They used the reactive atmosphere processing (RAP) for doping Cu⁺ successfully in LiF. It may be noted that unlike rare earth (RE) doped CaSO⁴ TL phosphors, none of the laboratories reported to have used the same preparation procedure to develop LiF:Mg,Cu,P phosphor.

LiF:Mg,Cu,Na,Si with high TL sensitivity was first developed by Nam et al. [72]. The optimum composition of dopants was found to be Mg 0.6 mol%, Cu 0.8 mol%, and 1.8 mol% each of Na and Si. The new phosphor was reported to have TL sensitivity about two times higher than that of LiF:Mg,Cu,P. For a constant heating rate of 5° C.s⁻¹, the main dosimetric peak of the glow curve appeared at 234 °C. The TL dose response of the peak was reported to be linear from 10^{-4} to 100 Gy, with no observed supralinearity or saturation. It was reported [73] that a personnel TL dosimeter using sintered LiF:Mg,Cu,Na,Si TL detector was designed and based on the experimental results of the new dosimeter, it was found appropriate to estimate personnel dose equivalent for wide range energy of photon fields. The results of Lee et al. [74] showed that Mg plays a role in the trapping of the charge carriers and Cu plays a role in the luminescence recombination process; however, the effect of Na and Si on the glow curve structure and the TL emission spectra is much less than that of Mg and Cu. It was considered that Na and Si each play a role in the improvement of the luminescence efficiency.

Tang et al. [75] (China) also reported development of a new high sensitivity LiF:Mg,Cu,Na,Si thermoluminescent phosphor with low residual signal and good stability to heat treatment. The main dosimetric peak of this phosphor occurs at 197 $\rm{^oC}$ at a heating rate of 1 $\rm{^oC}$ s⁻¹. It is reported that its TL response at both 260 \degree C and 280 \degree C were reproducible within a coefficient of variation of 2% over ten re-use cycles without systematic decrease. It retained the main advantages of LiF:Mg,Cu,P phosphor, and had a lower residual signal and a better stability to heat treatment. However, subsequently, Tang reported [76] that the height of the main peak depends strongly on the annealing temperature. He reported that the thermal susceptibility of LiF:Mg,Cu,Na,Si appeared to be

associated with the Na concentration. The lower the Na concentration, the less sensitive the TL was to annealing temperature. The optimum Na dopant concentration was found to be 0%. Thus the phosphor was discarded for its use in routine dosimetric applications.

Subsequently, Lee et al. [77-79] reported dosimetric characteristics of a new LiF:Mg,Cu,Si thermoluminescent (TL) material developed at KAERI, Korea and compared with those of commercially available LiF:Mg,Cu,P (GR-200A)(China). It is reported that LiF:Mg,Cu,Si thermoluminescence dosimeter (TLD) can be heated up to 573 K without any loss of TL sensitivity or any change in the glow curve structure. High-temperature glow peak in LiF:Mg,Cu,Si was significantly lower than that in GR-200A, consequently the residual signal was only 0.025%, which is about 35 times less than that of GR-200A. The residual signals of LiF:Mg,Cu,P (GR-200A), LiF:Mg,Cu,Na,Si, and LiF:Mg,Cu,Si were reported to be 0.92, 0.15 and 0.025%, respectively. The TL sensitivity of the LiF:Mg,Cu,Si TLD was reported to be about 55 and 1.1 times higher than those of the LiF:Mg,Ti (TLD-100) and GR-200A, respectively [77]. It was concluded that the replacement of dopant P by Si resulted in LiF:Mg,Cu,Si with improved TL properties in which the dual-step annealing method (537 K for 10 min followed by 533 K for 10 min) enabled to overcome the two major disadvantages of LiF:Mg,Cu,P (i.e., (i) a thermal loss in the TL sensitivity when it is annealed at a temperature above 513 K (240 °C), and (ii) a relatively high residual signal). Therefore, the authors strongly believed that LiF:Mg,Cu,P could be replaced by LiF:Mg,Cu,Si in the field of radiation dosimetry. Lee et al. [77] and Kim et al. [80] reported that for the reader annealing using a maximum readout temperature and clamping at $260⁰C$, no significant change in the TL sensitivity and glow curve structure was observed for more than 100 reuse cycles of exposures (5.5 mGy) and readout. However, requirement of dual-step annealing method, for restoration of sensitivities of peaks 1- 4, is indicative of complex nature of defects in this triplydoped phosphor. TL emission spectrum of LiF:Mg,Cu,Si was found to have three emission bands peaking at 355, 385 and 440 nm similar to that of LiF:Mg,Cu,P but differing in the relative intensities [78]. Negligible fading, insensitivity to room light and absence of the effect of pre- or post-storage annealing on the response and the glow curve structure was observed. The dose response for this TL material (LiF:Mg,Cu,Si) was reported to be linear in the range 1 μ Gy to 20 Gy and a sub-linear response was observed for higher doses. The minimum measurable dose value of 0.3 μ Gy as 3 σ of the background readout of unirradiated samples was reported [25]. The reusability of this newly developed TL detector sufficiently satisfied IEC standards [80]. It is also reported [81] that indigenously developed ⁶LiF:Mg,Cu,Si and ⁷LiF:Mg,Cu,Si TLDs provided a better alternative to TLD-600 and TLD-700 for the dosimetry of mixed fields of neutrons and gamma rays.

Recently, Tang et al. [82, 83] have reported development of highly sensitive LiF:Mg,Cu,Si TL discs with good stability to heat treatment, which they report are less sensitive to annealing at a certain temperature than LiF:Mg,Cu,Si developed in Korea [77]. The shape of the glow curve for the new LiF:Mg,Cu,Si disc is similar to that for standard LiF:Mg,Cu,P (GR-200A), and shows minimal differences when annealed in the range from 260 \degree C to 290 \degree C for 10 min. The TL sensitivity for LiF:Mg,Cu,Si is much lower than that for GR-200A, but is 35 times larger than that for TLD-100. The residual signal for LiF:Mg,Cu,Si is about 0.4% following readout at 260 $^{\circ}$ C for 12 s at a heating rate of $15^{\circ}C$ s⁻¹, which is approximately half for GR-200A following readout at 240 $^{\circ}$ C for 12 s. Thus, the temperature between 260 $^{\circ}$ C and 290 $^{\circ}$ C can be used to treat LiF:Mg,Cu,Si. These results indicated that the new LiF:Mg,Cu,Si disc has a good stability to thermal treatments and a lower residual TL signal. On the basis of TL spectral measurements it is concluded that Mg dopant mainly plays a role in the formation of trapping centres, both Cu and Si play a role in the main emission process and Cu also plays a role in reducing the emission around 610 nm. Table 4 gives characteristics of LiF:Mg,Cu,P, LiF:Mg,Cu,Na,Si and LiF:Mg,Cu,Si TL phosphors prepared using different methods. It also gives comparison of dosimetric characteristics of LiF doped with various combinations of the dopants: Mg, Cu, P, Si and Na.

It is worth mentioning here that LiF:Mg,Cu,Si and LiF:Mg,Cu,B materials were first developed and reported by Nakajima et al. in 1978-79 [60, 61]; but, they were not attractive in comparison to LiF:Mg,Cu,P because of their low TL sensitivity. TL sensitivities of LiF:Mg,Cu,Si and LiF:Mg,Cu,B were about 4.4 and 4.3 times, respectively, than that of LiF:TLD-600.

Although the role of Mg in LiF:Mg,Cu,P to provide trapping centres for electrons is well established, there is no consensus about the roles of Cu and P. As per McKeever [84], neither Cu nor Mg are directly involved in the emission process since in the material doped with only Cu, the wavelength of emission is very different from those samples which contain P. He also argued that since it is necessary to have large quantities of P in order to obtain the brightest material, it could be assumed that the TL is emitted from Mg/P phases. Thus P was assigned the role of a luminescent activator. Mahajna et al. [85] claimed that P takes role of Ti in LiF:Mg,Cu,P. Bos et al. [86] proposed the dual role of P, which is involved in the trapping of charge carriers (although the role of Mg is more dominant). It also acts as luminescent centre. Bilski et al. [87] proposed that P is luminescent centre while Cu induces some competitive processes, which reduce the formation of higher order complexes of Mg related defects. According to them, Cu is not involved directly in the TL process. On the contrary, the work of Patil and Moharil [71] shows that $Cu⁺$ is acting as a luminescent centre. They proposed that radiation creates excess electron colour centres and defects associated with trapped interstitial halogen atoms. During heating, the halogen atoms are released from interstitial position and they recombine with electrons. The energy of recombination is efficiently transferred to nearby $Cu⁺$ ion, which acts as luminescent centre. But the above-proposed model doesn't discuss the role of P. Chen and Stoebe [88] concluded that $Cu⁺$ plays a role in the luminescence recombination process in the LiF:Mg,Cu,P material using the extended X-ray absorption fine structure (EXAFS) measurements. According to Shinde et al. [70] phosphorus seems to play a dual role: it acts as a hole trap and also increases the TL sensitivity by assisting the incorporation of Cu ions into the LiF lattice. They also proposed that $Cu⁺$ plays a role in the luminescence recombination process.

Lee et al. [74, 78], Kim et al. [25] and Tang et al. [82, 83] studied the emission spectra of LiF doped with various combinations of the dopants: Mg, Cu, P, Si and Na. The measurements and analysis of the three-dimensional TL spectra of Lee et al. [74] showed that in LiF:Mg,Cu,Na,Si sample, a 385 nm peak wavelength is observed in the low-temperature range $(30-160^{\circ}C)$ and the value of the peak wavelength at the main peak at 210° C is observed to be \sim 366 nm, while a 355 nm luminescence is emitted at the high-temperature range (\sim 250 $^{\circ}$ C). They also report that the emission of LiF:Mg,P is totally different from that observed for $LiF:Mg$, $Cu.P.$ exhibiting a maximum at \sim 405 nm. While the TL spectra of the LiF:Mg,Cu,Na,Si sample and the LiF:Mg,Cu sample, which had no Na and Si dopants, have almost the same luminescent behaviour. The main emission peak at 385 nm was observed in the TL emission spectra of the samples which contain Cu, but the 385 nm emission was not observed in that of the LiF:Mg,Na,Si sample, which did not contain Cu. They also report that the glow curves of the samples that contain the Mg dopant are very similar, since they have the same number of peaks and their temperatures are the same. These curves are very different from those obtained for the LiF:Cu,Na,Si (CNS) sample, which does not contain Mg. Thus, they proposed that Mg plays a role in the trapping of the charge carriers and Cu plays a role in the luminescence recombination process; however, the effect of Na and Si on the glow curve structure and the TL emission spectra is much less than that of Mg and Cu. It was considered that Na and Si each played a role in the improvement of the luminescence efficiency. They reported [74] that the TL intensity of the LiF doped with Mg,Cu was ~30% of that of the sample doped with Mg, Cu, Na, and Si, but that doped with Mg,Na and Si was only 3%. From their results they [74] inferred that the emission of LiF:Mg,P is totally different from that observed for LiF:Mg,Cu,P, exhibiting a maximum at \sim 405 nm. From these results, they proposed that the Cu acts as a luminescent centre and that the Na and Si are not luminescent dopants, because the peak wavelength of the TL emission is not influenced by the Na and Si dopants. They also commented that the

thermoluminescence characteristics of LiF:Mg,Cu,Na,Si TL material are very similar to those of the LiF:Mg,Cu,P material. In the LiF:Mg,Cu,Na,Si material, Na and Si dopants correspond to the P dopant in the LiF:Mg,Cu,P material. They stated that measurement results in their study agreed well with those of Patil and Moharil [71]. Thus, they concluded that the Cu dopant is directly involved in the process of the 385 nm emission. Lee et al. [78] and Kim et al. [25] reported emission spectral measurements for LiF:Mg,Cu,P samples. TL emission spectrum of LiF:Mg,Cu,Si was found to have three emission bands peaking at 355, 385 and 440 nm similar to that of LiF:Mg,Cu,P but differing in the relative intensities. They report that the peak temperature and the TL emission spectra of dosimetric glow peak in all samples having Mg, Cu were always found to be the same irrespective of the third dopant which influenced only the intensity of TL emission spectrum. The emission band peaking at 385 nm was assigned to Cu.

Tang et al. [82] investigated the effect of heat treatments on LiF:Mg,Cu,Si. The shape of the glow curve for LiF:Mg,Cu,Si was reported to be similar to that for standard LiF:Mg,Cu,P (GR-200A), and showed minimal differences when annealed in the range from 260 °C to 290 °C for 10 min. The TL sensitivity for LiF:Mg,Cu,Si was found to be much lower than that for GR-200A, but is 35 times larger than that for TLD-100. The glow curve shape of LiF:Mg,Cu,Si annealed at 260 \degree C for different times shows minimal differences and TL response remains stable. These results indicate that the new LiF:Mg,Cu,Si disc has a good stability to thermal treatments and a lower residual TL signal. The residual signal for LiF:Mg,Cu,Si is about 0.4% following readout at 260 $^{\circ}$ C for 12 s, which is approximately half of that observed for GR-200A following readout at 240 $^{\circ}$ C for 12 s.

Tang et al. [83], on the basis of their results on the 3D TL spectra and glow curves of LiF:Mg,Cu,Si with various Mg, Cu and Si concentrations, reported that the shapes of glow curves in LiF:Mg,Cu,Si, LiF:Mg,Cu and LiF:Mg,Si were similar and the glow curves had peaks at approximately the same temperatures but with significantly different intensities. In the case of LiF:Cu,Si sample, which had no Mg dopant, the glow curve shape was totally different from the others. Thus, they concluded that Mg dopant plays mainly a role in the formation of trapping centres in LiF:Mg,Cu,Si TL material. Tang et al. [83] report that the spectra of LiF:Mg,Cu,Si, LiF:Mg,Cu and LiF:Mg,Si are similar in the range of 300–550 nm. Neither the temperature of the glow peak nor the wavelength of the emission maximum changes with variation of dopants concentrations when Cu is more than 0.01 mol % in LiF:Mg,Cu,Si. The emission in LiF:Mg,Cu,Si with Cu concentration 0.01 mol % is similar to that in LiF:Mg, Si, which also shows some weak emission around 610 nm, and is different from that in LiF:Mg,Cu,Si with Cu concentration higher than 0.01 mol %. Thus, they concluded that both Cu and Si play a role in the main emission process and Cu also plays a role in reducing the emission around 610 nm. However, full characterization in terms of minimum detectable dose, region of linear dose range, etc., is not reported for LiF:Mg,Cu,Si (China).

LiF:Mg,Cu,P phosphors have been thoroughly characterized by Nakajima et al. [60, 61], Wu et al. [62], DeWerd et al. [95], Bhatt et al. [27, 96], Wang et al. [63, 64], Driscoll et al. [52], Prokic and Botter-Jensen [23], Zha et al. [24], Pradhan and Bhatt [97], Mahajna et al. [85], Bilski et al. [87, 89], etc.. LiF:Mg,Cu,Na,Si and LiF:Mg,Cu,Si TL phosphors have been characterised by Nam et al. [72], Jung et al. [73], Lee et al. [74], Tang et al. [75, 76], Lee et al.[78, 79], Kim et al. [25], Rahman et al. [80] and Tang et al. [82, 83].

It was reported by Jung et al. [73] that "a personnel TL dosimeter using sintered LiF:Mg,Cu,Na,Si TL detector was designed and based on the experimental results of the new dosimeter; it was found appropriate to estimate personnel dose equivalent for wide range energy of photon fields". But, there is no published report on use of either LiF:Mg,Cu,Na,Si or LiF:Mg,Cu,Si for routine dosimetric applications. A published report in 2002 by Kim et al. [98] states that CaSO4:Dy dosimeter based Teledyne 300 automatic TLD reading system and a C-300 badge is being used for routine personnel monitoring service in Korea.

It is also pertinent here to mention that of all the LiF:Mg,Cu,P-based phosphors, the one manufactured by Thermo Fisher Scientific (Harshaw, USA) has been tested thoroughly in the configuration of personnel monitoring TLD badge over a large number of cycles of re-use [92-94]. It is reported that the personnel monitoring TLD cards, made from LiF:Mg,Cu,P (Harshaw) TLD chips (the detector element having encapsulation of Teflon), heating up to 260 \degree C during TL readout resulted in about 0.01% sensitivity loss per use over 1000 reads (resulting in 10 % total loss in sensitivity) which is reported to be comparable to the loss of sensitivity in LiF:Mg,Ti (Harshaw) based TLD cards. Moscovitch [92] states that the advantages of LiF:Mg,Cu,P include high sensitivity as compared to LiF:Mg,Ti, almost flat photon energy response, low fading rate and linear dose response. The lack of supra-linearity at higher dose levels is particularly useful for accident dosimetry, and eliminates the source of error usually associated with the application of supralinearity corrections. The main drawbacks are still the relatively high residual signal and the loss of sensitivity for high readout temperatures. However, this does not limit the usefulness of LiF:Mg,Cu,P for low dose levels typical to personnel or environmental dosimetry, but may be a limiting factor for high dose applications such as clinical dosimetry.

4.2 Lithium Tetraborate. Lithium tetraborate $(Li_2B_4O_7)$ doped with manganese (Mn) was first proposed by Schulman et al. in 1967 [99] for TL dosimetry applications as a tissue equivalent material. This material was prepared by melting the raw materials to a temperature higher than the melting point of lithium tetraborate and then rapidly cooling to room temperature. The glassy material thus obtained is fired at a sufficient temperature to crystallize it. The major drawbacks of this material are its poor sensitivity, hygroscopic nature, and relatively large fading. The low TL sensitivity was caused partly by the emission in the 600 nm region of the spectra, which is far from the response region of most photomultipliers.

Recently, Annalakshmi et al. [101] synthesized manganese (Mn) doped $Li_2B_4O_7$ using solid state reaction technique by sintering at 750 \degree C for 3 h in an alumina crucible. It is reported that the glow curve shows a high temperature peak at $250 \degree C$, which is highest among all other lithium borate phosphors studied in the literature. Linear dose response is observed up to 10 Gy. TL intensity was maximum for Mn concentration around 0.32 wt.%. The solid state synthesis route was found to result in non-hygroscopic and low-fading phosphor as compared to other preparation techniques. Li2B4O7:Cu was prepared by Takenaga et al. [20] by sintering technique. To raw lithium borate $(Li_2B_4O_7)$ powder was added a solution of CuCl₂ in acetone or alcohol, and the mixture was then stirred and dried. The $Li_2B_4O_7$ powder containing the activator compound was heat-treated in air in a platinum boat for about 1 h at a temperature of 900-913 °C, which is just below the melting point (917 °C) of $Li_2B_4O_7$. Because of the heat treatment, clear crystals having an almost spherical form were produced from the raw $Li₂B₄O₇$ powder, which was porous and opaque. The heat treatment causes diffusion of the activator into $Li_2B_4O_7$ crystal interiors, as well as re-crystallization and sintering due to diffusion, vaporization and deposition. The use of copper activator instead of manganese in lithium borate [20, 21] overcame the drawback of poor TL sensitivity and red TL emission spectra to an emission spectrum of copper activator, at about 360 nm (see Table 3). However, commercially available $Li₂B₄O₇$: Cu thermoluminescent material from Panasonic Inc. is produced in powder form which is inconvenient for routine dosimetric use.

Prokic and co-workers have developed and characterized sintered pellets (4.5 mm dia and 0.95 mm thickness) of $Li₂B₄O₇$ doped with copper and other co-dopants/co-activators, such as Ag, In, P [48-50]. Generally, sintered forms are preferred due to ease of their handling during routine use. Also, for low dose measurements they give better signal to noise ratio. Prokic [104] reported that the relative photon energy response factors for Li₂B₄O₇: Cu,In and Li₂B₄O₇: Cu,In,Ag were 0.94 and 0.97, respectively at 33 keV compared to that at 1.25 MeV. Thus, they offer flatter photon energy response compared to $Li_2B_4O_7$:Cu due to their better tissue equivalence. Table 5 gives comparison of characteristics of doped $Li_2B_4O_7$ TL phosphors prepared using different methods.

Recently, Patra et al. [112] have reported that luminescence studies, in single crystals of $Li₂B₄O₇$ (LTB) doped with Cu and Ag and Cu, Ag co-doped, revealed a sensitizer role of Ag in the LTB:Cu, Ag crystal. They further report that, despite an energy transfer from $Ag⁺$ to Cu⁺ centers, emission from both the centers participates in the thermally stimulated luminescence (TSL) of codoped crystal. They propose that the LTB:Cu,Ag crystal will be a better and efficient material for TSL dosimeters compared to singly doped LTB crystals. Therefore, to exploit the full potential of the co-doped LTB, a suitable TSL readout system consisting of a PMT having a peak response in the range of 200–600 nm will be necessary. However, no comparative measurements have been provided in this connection. Takenaga et al. [47], Lakshmanan et al. [113-114], Wall et al. [21], Prokic [104], Furetta et al. [105] and others had studied extensively various characteristics of these phosphors for their projected application in radiation dosimetry. Singh et al. [111] have reported synthesis and characterization of $Li₂B₄O₇$: Cu nanophosphor using solution combustion synthesis method. However, its TL sensitivity is very low and dose response in the range 1mGy-5kGy, with linearity over a limited range.

Table 5 Comparison of TL characteristics of $Li_2B_4O_7$ phosphors prepared by different methods.

4.3 Magnesium Borate. Due to its near tissue equivalence ($Z_{\text{eff.}} = 8.4$), rare earth-doped MgB₄O₇ TL phosphors have been investigated by many researchers [115-118] for their possible use in personnel monitoring and other applications. Kazanskaya et al. [115] prepared MgB4O7: Dy (0.1

mol%) sintered pellets. These detectors showed good sensitivity and linear dose response in the dose range 10 µGy to 10 Gy, but these detectors showed 25% fading in 40 days, whereas the MgB_4O_7 : Dy (0.5 mol%) phosphor powder developed by Lakshmanan et al. [116] showed 40% fading in 17 days. Thus, they were not suitable for dosimetric use. Prokic reported development of highly sensitive MgB₄O₇: Dy/Tm sintered thermoluminescent dosimeters [117, 118]. She also developed MgB₄O₇: Dy^{*}/Tm^{*} sintered discs (with a co-dopant as sensitizer). These, MgB₄O₇: RE^{*} sensitized, detectors were more sensitive than the non-sensitized magnesium borate thermoluminescent material [118, 119].

Prokic also developed highly sensitive MgB₄O₇:Mn sintered pellets having linear dose response in the range 10 µGy to 45 Gy and negligible fading in 4 months [120]. Prokic and Furetta et al. [121, 122] report the development and dosimetric characterisation of a new production of $MgBaO₇:Dy,Na$ thermoluminescent material. The detectors showed wide dynamic dose range (90 µGy to 40 Gy), minimum detectable dose of 6 μ Gy and a fading of 8 % in 3 months. It is reported that though previously prepared sensitized magnesium borate TL materials activated with Dy^{3+} or Tm^{3+} , were highly sensitive phosphors, they showed high fading, multiple peak structure of the main peak and slight chemical instability. It is reported that these shortcomings of the magnesium borate phosphors have been entirely overcome by improvement over the original preparative procedure and the development of $MgBaO₇$: Dy,Na TL material with optimum characteristics, maintaining a sensitivity of 6-7 times higher than TLD-100 obtained using a Harshaw 2000A reader [23, 121, 122]. (It is reported that a sensitivity of about 15 was obtained using Alnor Dosacus TLD reader.) These dosimetric characteristics make this TL material very useful for multiple dosimetry applications, particularly in individual monitoring and in various medical dosimetry purposes. MgB4O7:Dy,Na TL dosimeters are successfully used on a large scale for legal personnel dosimetry control in Yugoslavia [121, 122]. The efforts towards development MgB_4O_7 -based detectors by various groups are summarized in Table 6.

Fukuda et al. [126] reported TL characteristics and emission spectra of CaB₄O₇ doped with Dy³⁺, Eu^{2+} , Pb²⁺ and Cu⁺. These phosphors were developed as sintered pellets. For a heating rate of 20^oC min⁻¹, the TL glow peaks can be roughly grouped into three temperature regions: (I) $75\textdegree 110\textdegree C$, (II) 170~190 $^{\circ}$ C, and (III) 255~275 $^{\circ}$ C. Their emission spectra depend on the activator and its valence. The activators release to the luminescence in the following way: Eu^{2+} to 440 nm, Dy^{3+} to 480 and 580 nm, Pb^{2+} to 275 nm, and Cu⁺ to 540 nm, respectively. All the TL glow peaks showed no supralinearity before they saturated at an exposure of about 2.58 C.kg⁻¹ (10^4 R). Peaks appearing at the temperature regions II and III retained memories of irradiation for a storage period of 6 months in the dark at room temperature. However, TL sensitivities of individual phosphors were not reported. Tekin et al. [127] developed sintered pellets of $CaBaO₇:Dv$, $CaBaO₇:Dv$ showed three glow peaks at about 50 °C, 240 °C and 380 °C, the intensity of the 240 °C glow peak being the maximum; TL sensivity of 240 $^{\circ}$ C TL peak was 8 times higher than that of LiF (TLD-100). There are no other detailed reports on the development and characterization of this phosphor.

Phosphor and	Method of preparation	TL intensity	TL emission peak	Dose response
physical form		relative to	(nm)	(Region of linearity)
		$LiF: TLD-100$		
(0.1) $MgB_4O_7:Dy$	By sintering at $960 \degree C$.	$10-20$ (as compared	470 & 556	10 μ Gy to 10 Gy.
sintered $mol\%)$	(TL peak at 190-200)	to LiF sintered		$(25\%$ fading in 40 d.)
pellets $[115]$	$^{\circ}$ C.)	pellets)		
(0.5) $MgB_4O_7:Dy$	By sintering at 950 $^{\circ}$ C 1.5			1 mGy to 40 Gy for
$mol\%$) phosphor	for 2h. (Main TL peak			200 °C TL peak (40)
powder $[116]$	at \sim 200 °C.)			$%$ fading in 17 d.)
$MgB_4O_7:Dy/Tm$	Prepared by sintering	2	i).480 $&570$ nm for	\sim 10 µGy to 100 Gy.
sintered discs	technique. (TL peak		Dy –doped.	$(10\%$ fading in 60 d.)
[117, 118]	\sim 210 °C.)		ii). 450 nm for Tm-	
			doped.	

Table 6 Comparison of TL characteristics of MgB₄O₇ phosphors prepared by different methods

4.4 Other Lithium-, Sodium- and Potassium-based Compounds. It has been reported [128-130] that the perovskites $(ABX_3,$ where "A" and "B" are cations and "X" is an anion. The "A" and "B" cations can have a variety of charges) are very interesting hosts for their thermoluminescent properties. Eu- or Ce-doped crystals of $KMgF_3$ (a compound which belongs to the perovskite group) were investigated for their possible application as thermoluminescent dosimeters (TLDs) by Furetta et al. [128]. KMgF₃:Eu³⁺ single crystals prepared by Kyropoulos technique showed main TL peak at \sim 613 K. TL sensitivity of these detectors was reported to be 4.4 times than that of LiF:Mg,Ti. TL dose response of these detectors was linear in the range 4 mSv to 1 Sv. Moharil et al. [129] reported that $KMgF_3:Eu^{3+}$ phosphor powder, prepared by solid state diffusion at 1075 K, showed main TL peak at 530 K, which had TL sensitivity 0.20 times than that of CaSO4:Dy. The phosphor showed characteristic Eu³⁺ emission at 577, 595 and 617 nm. The phosphor showed linear dose response in the range 0.01 C/kg to 0.2 C/kg. Bacci et al. [130] reported that optical absorption and emission measurements clearly show that, despite doping of the material with Eu^{3+} ions, only Eu^{2+} ions are incorporated in the crystalline samples. Systematic thermoluminescence experiments indicated that the intensity of the glow peak of the Eu-doped phosphor was linearly dependent on the dopant concentration and on the radiation dose. Kitis et al. [131] reported that TL sensitivity of Pb-doped samples is about 10 times higher than that of Ag-doped.

Kitis et al. [132] reported that the TL response of $KMgF_3$: Ce (660 mol%) was 167 times higher than that of LiF:Mg,Ti. Its main glow peak was centred at about 160 $^{\circ}$ C, with TL emission at \sim 360 nm [133]. The material was reported to have very good thermal stability, no fading and had a linear TL response at very low doses. It may be pointed out here that dopant concentrations much higher than 10 mol% would lead to formation of a separate phase in the doped material, thereby distorting the basic characteristic of the host material., as well as leading to concentration quenching of luminescence. Other authors have reported that 660 mol% of Ce^{3+} in the host resulted in the highest TL sensitivity in the phosphor material. However, doping of 660 mol% in KMgF₃ would require \sim 1300 g of CeF₃ as against \sim 120 g for molar wt. of KMgF₃ as the host material. Therefore, in such a compound luminescence properties will be dominated by CeF_3 host. Also, Z_{eff} of such a compound will be very high as against 13 of KMgF₃. In this context, it may be noted that in another publication [134] by the same group, it was reported that $KMgF_3:Ce$ (1.5 mol%) single crystals

showed TL sensitivity \sim 90 times than that of LiF:Mg, Ti. These detectors showed linear dose response in range 100 µGy to 10 Gy and 3-4 % fading at the end of a storage period of about 100 h. It is commented that the high sensitivity of KMgF3:Ce made it very useful for medical and environmental radiation dosimetry. The presence of 40 K in any sample of KMgF₃ produces a β selfirradiation. A possible contribution of self-dose to the external dose can be accurately estimated in specific cases, e.g., during short monitoring periods in environmental dosimetry. The self-dose irradiation should not be a serious problem in other dosimetric applications where high doses have to be monitored as in the case of clinical dosimetry.

Kitis et al. [136] reported that $LIMgF_3:Ce$ (2.97 mol%) phosphor powder was about 3 times more sensitive than LiF:Mg,Ti. The phosphor showed linear dose response in the range 2 mGy to 10 Gy and no post-irradiation fading in 20 days. Bernal et al. [137] reported the synthesis of $LiMgF_3:DyF_3$ sintered pellets. Li₃PO₄:Mg,Cu [138] and NaLi₂PO_{4:Eu³⁺ [139] phosphor powders showed TL antered pellets. Li₃PO₄:Mg,Cu [138] and NaLi₂PO_{4:Eu³⁺} [139] phosphor powders showed TL} sensitivities 1.2 times that of $CaSO₄:D_V$ and ~ 0.5 times that of TLD-700H, respectively, whereas LiCaAlF₆:Eu²⁺ [140] phosphor powder showed nearly twice that of CaSO₄:Dy.

Phosphor and physical form	Table / Other htmain-, soutuni- and potassium-based compounds grying TD Method of preparation	TL intensity relative to LiF:TLD-100	TL peak (nm)	emission Linear dose range
$KMgF_3:Eu^{3+}$ single crystals $[128]$	Single crystals by Kyropoulos technique. TL peak at \sim 613 K.	4.4 times that of LiF:Mg,Ti	$\frac{1}{2}$	4 mSv to 1 Sv $(Z_{\text{eff}} = 13.0)$
$KMgF_3:Eu^{3+}$ phosphor powder [129]	Solid state diffusion at 1075 K. Main TL peak at 530 K.	20% $\overline{\text{of}}$ CaSO ₄ :Dy.	577, 595 and 617 nm	0.01 to 0.2 C/kg
$KMgF_3:Pb$ single crystals $[131]$	Single crystals by Kyropoulos technique. Main TL peak at ~ 170 $\rm{^0C}$.	Sensitivity of Pb- doped samples is about 10 times higher than that of Ag-doped.	$-----$	0.2 to 100 Gy.
$KMgF_3:Ce$ (660 mol%) phosphor powder [132]	Obtained by the melt of KF and MgF2, in stoichiometric ratio, and the dopant, using Czochralski method in an argon atmosphere.	167 times that of LiF:Mg,Ti	\sim 360 nm [133]	$MDD = 2.1 \mu Gy.$ detectable N ₀ post- irradiation fading in 15 days.
KMgF ₃ :Ce single crystals $[134]$	Using the Czochralski method in an argon atmosphere	92 times that of LiF:Mg,Ti (for Ce of conc. 1.5 $mol\%$).	360 nm	100 μ Gy to 10 Gy. 3-4 % fading at the end of a storage period of about 100 h.
KMgF ₃ :Eu,Ag phosphor powder [135]	Fired at 800 °C for 1h in argon atmosphere. (TL peak around 260 °C)	$\overline{3}$	356 nm	
$LiMgF_3:Ce$ (2.97) $mol\%$) phosphor powder $[136]$	Melting of the component salts.	3.18 times that of LiF:Mg,Ti		2 mGy to 10 Gy. No post- irradiation fading in 20 d.
$LiMgF_3: DyF_3$ sintered pellets [137]	Thermal treatment at 973 K for 5 h in air.			Up to doses of 20 Gy.
Li ₃ PO ₄ :Mg,Cu phosphor powder [138]	Precipitation method and use of 2 wt.% NH_4Cl flux. Treated at 860 °C	1.2 times that of CaSO ₄ :Dy	370 nm	0.13 mGy to 100 Gy.

Table 7 Other lithium-, sodium- and potassium-based compounds giving TL

Recently, Dhoble et al. [141] have published a chapter on "Li-based phosphors for thermoluminescence dosimetry". A number of Li-based TL phosphors, such as LiNaSO4:Cu, LiNaSO₄:Cu, Mg, LiNaF₂:Cu, LiNaF₂:Cu, Mg, Li₂BPO₅:Cu⁺ [142], have been synthesized and studied for their possible application in radiation dosimetry. Most of these have been reported to have linear dose response in the range 1-15 Gy. Also, minimum detectable dose (MDD) has not been investigated for these phosphors. Thus, due to very narrow/limited range of study of dose response, it is difficult to comment on the applicability of these phosphors in radiation dosimetry.

LiCaBO₃:Tm and LiMgBO₃:Tb ($Z_{\text{eff}} \sim 8$) phosphor powders have been prepared by Solid-state diffusion method and their TL sensitivities were reported to be 8 and 4 times, respectively, than that of LiF:TLD-100. Both the phosphors have linear dose response up to 10^3 Gy, negligible storage fading and a simple annealing procedure for reuse [144, 145]. Shinde and Dhoble [146] have reported the preparation and characterization of NaCaPO₄:Dy (0.3 mol) % phosphor powder using combustion synthesis method. Its TL sensitivity was reported to be 1.15 times than that of CaSO4:Dy and linear dose response in the dose range 0.01 Gy to 10 kGy. Its main TL peak occurred at \sim 230 °C and no fading was observed in 5 weeks. More et al. [147] have reported synthesis of $NaCaPO₄:Eu²⁺$ phosphor powder using Solid-state reaction. Its TL sensitivity is reported to be about 4 times than that of TLD-100. The efforts towards development of different Li-based TL phosphors by various groups are summarized in Table 7.

4.5 Orthosilicate-based TL Phosphors. $Mg_2SiO_4:Tb$ is an attractive thermoluminescent material because of its high sensitivity to gamma-rays and chemical stability (Hashizume et al. [29], Prokic and Yukihara [30], Ayyengar et al. [148]). It was first introduced by a Japanese group [29, 149]. The phosphor was subsequently produced on commercial scale and marketed by Kasei Optonix Ltd., Japan. Toryu et al. [149] reported that the gamma radiation sensitivity as well as the gamma: UV response ratio increase with increasing preparation temperature. Samples sintered at 1700 °C gave highest TL sensitivity for X- and γ - rays. Lakshmanan and co-workers [150-152] have done detailed characterization of Mg_2SiO_4 : Tb TL phosphor powder marketed by Kasei Optonix Ltd., Japan. The phosphor was reported to give very high intrinsic TL sensitivity to ultraviolet (UV) (wavelength 253.7 nm) radiation. The intrinsic TL sensitivity of Mg_2SiO_4 : Tb TL phosphor powder to ultraviolet (UV) (wavelength 253.7 nm) radiation was reported [151] to be about 1100 times higher than that of CaSO₄:Dy TLD phosphor. Jun and Becker [153] have reported the preparation procedure for Mg_2SiO_4 : Tb followed by them. Appropriate amount of MgO , SiO_2 and the dopant was dried and this dried mixture was treated at \sim 1700 °C in alumina or platinum crucible followed by powdering and sieving in a grain size fraction $0.1 - 0.2$ mm. TL sensitivity of the phosphor was reported to be 40 times than that of LiF:Mg,Ti (TLD-100). Bhasin et al. [154] reported development of a sensitive Mg2SiO4:Tb phosphor powder. Their method involved intimate mixing of MgO and silica gel (in the molar ratio of 2:1), 10 mg atoms Tb per mol. of $Mg_2SiO₄$. The dried mass was melted in a silica crucible by directly blowing the Burshane-oxygen flame over it (temp. of flame \sim 2750 $^{\circ}$ C). Phosphor powder was separated between 80 and 200 tylor mesh. TL sensitivity of the phosphor was reported to be 79 times than that of LiF:Mg,Ti (TLD-100). Bhasin et al. [154] also reported that the phosphor gave very high intrinsic TL sensitivity to UV (wavelength 253.7 nm) radiation. A freshly prepared Mg_2SiO_4 : Tb sample, after annealing at 500° C, when exposed to a 10 W germicidal Hg lamp at 5 cm induced as much TL as induced by 2000 R of ${}^{60}Co$ gamma rays.

Recently, Prokic and Yukihara [30] have reported development of ultra-high TL sensitive Mg_2SiO_4 :Tb. Mg_2SiO_4 :Tb has been synthesized by sintering technique under the reaction between the stoichiometric amounts of MgO and $SiO₂$ with the addition of optimal Tb₄O₇ activator concentration of about 12 mg atoms Tb per mole of Mg₂SiO₄. It was sintered for 1h at 1660 °C in air under extremely slow heating rate in an electric furnace. Finally, the polycrystalline phosphor was crushed and sieved in the grain sizes between 75 and 200 µm. After cold pressing of polycrystalline material into pellets of 4mm diameter and 0.8mm or 0.4 mm thickness, they were sintered under the same conditions like during the preparation of the crystalline phosphor. The sintered TLD pellets are opaque and very hard. The phosphor has a simple glow curve with main TL peak at about 210 \degree C and very low fading. Its TL sensitivity is reported to be 110 times than that of LiF:Mg,Ti (TLD-100), with a detection threshold of 0.5 μ Gy. Table 8 gives comparison of TL characteristics of Mg_2SiO_4 : Tb phosphors prepared by different methods. Nakajima [155] has published a review dealing with different methods of preparation and study of various characteristics of silicate-based TL phosphors.

4.6 CaSO4:Dy/Tm TL Phosphors. Yamashita et al. [44, 156] reported a simple and an excellent method for preparation of highly sensitive CaSO4:Dy and CaSO4:Tm TL phosphors in 1968. Analytical-reagent-grade CaSO₄.2H₂O and reagent-grade activator material were mixed in a proper ratio and dissolved in sulfuric acid to form saturated solution of CaSO₄. The mixed solution was kept at about 300 \degree C by heating so that crystalline samples appeared as the acid evaporated. Samples thus prepared usually consist of shining crystals 1-3 mm long [156]. In order to reduce the variability of phosphor characteristics, from batch to batch, and to increase stability for repeated uses by post-annealing, the virgin crystals were subjected to pre-irradiation annealing treatment at 700 $^{\circ}$ C for 2h. The crystalline sample, mesh size from 100 to 200, was used for studying the dosimetric characteristics of the phosphors. Yamashita et al. [156] reported that of all the 14 rare earths (REs) used for preparation of RE–doped $CaSO_4$ phosphors, $CaSO_4$:Dy and $CaSO_4$:Tm showed the highest sensitivity with essentially a single peak at about 220 $^{\circ}$ C. Emission spectrum of CaSO4:Tm consists of a main sharp peak at 450 nm with minor ones at 360, 470 and 520 nm, and CaSO4:Dy has two main peaks at 480 and 570 nm. It was reported [44, 156] that the dosimetric characteristics of these two phosphors were excellent except for their non-tissue equivalence (Z_{eff} = 15.3). Minimum detectable exposure was reported to be lower than 200 µR (5.16 10−8 C/kg). Dose response was reported to be linear up to 3000 R and supralinear above this exposure level, whereas CaSO4:Tm was linear up to 300 R and supralinear above this exposure level. These two phosphors showed 1-2% fading per month. Subsequently, Ayyangar et al. [148] reported that the TL sensitivities of $CaSO₄:D_V$ and $CaSO₄:T_m$ prepared by them, following the method suggested by Yamashita et al. [156], were about 38 and 32 times, respectively, than that of LiF:TLD-100.

Several researchers have spent a great amount of efforts improving the TL properties of CaSO₄:Dy and CaSO4:Tm phosphors by studying the influence of starting material, particle size, grinding and activator concentration on the shape of the glow curve [157-162].

Lakshmanan et al. [163] have developed a simplified co-precipitation technique for the synthesis of CaSO4:Dy phosphor, which circumvent the cumbersome procedure, used so far, namely, evaporation of (highly corrosive) concentrated H_2SO_4 . High TL sensitivity (20% more than the present material), uniform microcrystalline morphology, lower grain size suitable for manufacturing dosemeters in solid form, better glow curve structure, lesser glow peak shift and better linearity and simplified preparation technique make the new phosphor a better alternative. The new recipe of CaSO4:Dy based on co-precipitation technique is not only economical but also compatible for large scale production. This novel method of synthesis of CaSO4:Dy TLD powder is suggested to be suitable for manufacturing teflon discs used in personnel monitoring. Recently, Rivera et al. [164] have also suggested preparation of CaSO₄:Dy by precipitation method for gamma radiation dosimetry. Although the method of Yamashita et al. [156] for preparation of Dy - or Tm - doped CaSO4 phosphors is simple, it is not ideal for preparing the phosphor in bulk quanties. The problem basically is of handling and evaporating large quantities of conc. H_2SO_4 which have attendant problems of corrosion and pollution. Also, it was observed that this procedure of open air evaporation of acid gives rise to batch- to- batch variation in TL sensitivity due to contamination by external impurities [165]. Rao et al. [165] devised and standardized a new method which employs distillation of saturated solution, containing required amount of $CaSO₄$ and the dopant, by gradient heating (275-300 $^{\circ}$ C) using air as the carrier gas. Nearly 98% of the H₂SO₄ is recovered, of which more than 90% is 35-36 N. It is recycled for manufacturing subsequent batches. The resulting crystalline product is heated and annealed at 700 °C for 2h to remove any residual traces of H_2SO_4 , as well as to stabilize its TL characteristics for repeated uses [166]. The method of Rao et al.[165] is used for commercial production of the CaSO4:Dy phosphor (600 g per batch) by Renentech Laboratories Pvt. Ltd., Mumbai, India.

Azorin and Gutierrez [167] also used a somewhat similar method for laboratory scale preparation of $CaSO₄:D_Y/T_m$ TL phosphors. Required amounts of $Ca(NO₃)₂$.4H₂O and the dopant were dissolved in conc. $H₂SO₄$ in a flask which is connected to a sealed condenser system with constant air flow as carrier for the acid vapour. A beaker containing a NaOH solution captures and neutralizes the condensed acid. A hot plate is used to provide the heat required to drive the reaction, while the temperature is monitored by chromel-alumel thermocouple. Crystallization can be controlled by varying the temperature and air flow rate. After an evaporation period of about 12 h, single crystals of CaSO⁴ are obtained whose dimensions depend on the starting materials and on the type and concentration of dopants. M. Prokic [28, 117] has developed new sintered thermoluminescent dosimeters for personnel and environmental dosimetry**.** Efforts to develop highly sensitive sulphatebased TL phosphors by various researchers have been summarized in Table 9. However, they have not been fully characterized to assess their performance for personnel and environmental dosimetry**.**

4.7 Calcium Fluoride (CaF2). Calcium fluoride exists in nature as fluorite mineral. Its TL properties were studied by many investigators (McKeever, [18], McKeever et al., [19], Portal [177]). TL glow curve of natural $CaF₂$ exhibits several peaks with a predominant and stable peak at \sim 250 °C; the lower temperature peaks are rather unstable. Although the use of this material for radiation dosimetry has been largely discontinued in many countries, in the past, increasing interest in the fluorite had been due to its high sensitivity, abundance in nature and low production cost. Synthetic CaF₂ activated with manganese (CaF₂:Mn) was developed and studied by Ginther and co-workers in 1950s. CaF₂:Mn (3 mol%) is prepared by co-precipitation of CaF_2 and MnF₂ from the solution of $CaCl₂$ and $MnCl₂$ in ammonium fluoride. The precipitate is dried and heated in a neutral atmosphere oven at 1200 $^{\circ}$ C, ground and sieved in the grain size range 80 to 200 mesh. It is marketed by Harshaw under the trade name TLD-400. It is about 5 times more sensitive than LiF:TLD-100 and has wide dynamic linear dose response – 1 mrad to $2x10^5$ rads, saturation occurs at 10^6 rads. One of the largest users of CaF₂:Mn-based dosimeter (bulb type design based on a single CaF₂:Mn element) has been US Navy since 1975. Recently, it has been reported that CaF2:Mn-based dosimeter has been replaced by LiF:Mg,Cu,P-based four element Harshaw TLD badge due to better dosimetric characteristics of LiF:Mg,Cu,P [94]. Dy-activated calcium fluoride $(CaF₂:Dy)$ is more sensitive than $CaF₂:Mn$. Its TL characteristics were studied by Binder and Cameron [178]. It is marketed by Harshaw under the trade name TLD-200. The TL glow curve consists of six peaks which are difficult to separate. Among these peaks, those at 120 and 140 $^{\circ}$ C exhibit high fading, whereas the peaks at 200 and 250 \degree C are stable and dosimetrically relevant. The phosphor shows 25% fading per month. A post-irradiation treatment at 115 $^{\circ}$ C for 10 min removes the fading effect considerably. $CaF₂:Dy$ serves mostly for measurement of low doses for environmental monitoring applications. Tm-doped calcium fluoride $(CaF_2: Tm)$ has been developed and characterized by Lucas and Capser [179]. 0.35 mol% of Tm gives optimum response and desirable characteristics. Its glow curve shows two prominent peaks at 150 (peak 3) and 250 $^{\circ}$ C (peak 5), the latter peak has supralinear response, whereas the former does not show supralinearity. This material is marketed by Harshaw under the trade name TLS-300. It has been reported [180, 181] that the high temperature (250 °C) glow peak in CaF₂:Tm (TLD-300) gives higher relative TL efficiency for HCP irradiations as compared to the low temperature (150 $^{\circ}$ C) glow peak. This difference in LET dependence of the two peaks (using ratio method) has been used to obtain from one single TLD detector, exposed to HCPs, dose and the radiation quality (Hoffmann et al. [182], Pradhan et al. [183], Lakshmanan et al. [184]). Prokert and Sommer [185] studied the dosimetric chacteristics of a new hypersensitive TL phosphor, $CaF₂:Cu$, prepared at the Moscow State University. However, studies by the authors indicated that Ho was the dominant impurity in the phosphor and that copper may be present as a co-dopant. The dose characteristic showed a linear dose response in the range between 10^{-6} and 10 Gy and the TL sensitivity was found to be 160 times higher than that of LiF-TLD-100. This high sensitivity was projected for potential phosphor to permit precise low dose measurements after short irradiation periods. Furthermore, the high thermal, chemical and mechanical stability were expected to enable multiple uses of the detectors.

4.8 $\mathbf{Al}_2\mathbf{O}_3$ **- based TL Phosphors.** The history of aluminium oxide $(\mathbf{Al}_2\mathbf{O}_3)$ as a radiation dosimeter dates back to the 1950s, when a large number of materials, incuding Al_2O_3 , were investigated to determine their TL properties. Aluminium oxide (alumina) is found in natural mineral form as sapphire and ruby. It may be synthetically produced as either γ - alumina or α -alumina (also known as corundum). Several research groups have tried to synthesize Al_2O_3 doped with different types of dopants, and tested their suitability in radiation dosimetry. However, the development of C-doped introduction of $A₁Q₃TL$ and optically stimulated luminescence (OSL) phosphor was an important landmark in the field of luminescence dosimetry. Table 10 gives Comparison of TL characteristics of Al_2O_3 - based phosphors prepared by different methods.

Al₂O₃:C crystals are grown from the melt (at 2050 °C). The grown samples are usually in the form of long, single crystal rods, which are then cut to size, normally 5 mm diameter single crystal

discs, 1mm thick. Corundum grown by the Verneuil method is used as the raw material. After growth, the material is given a one-time anneal at 950 \degree C for 30 minutes to remove any charge from deep traps. The crystal growth is performed in a highly reducing atmosphere in the presence of graphite. The end result is a high quality, single crystal of α -Al₂O₃ doped with 100-5000 ppm of carbon. The purpose of the highly reducing atmosphere when growing TLD quality material is to induce into the samples large concentrations of oxygen vacancies (F and F^+ centres) by a process known as subtractive coloration. These centres play an integral part in the TL and OSL process. The OSL of this phosphor is also utilized for personnel dosimetry. The α -Al₂O₃:C single crystals (5mm diameter, 1 mm thick) may be obtained from the Urals Polytechnical Institute, Russia, Thermo Fisher Scientific (Harshaw), USA (sold as TLD-500K), Rexon TLD Systems, Inc., USA, and some other commercial suppliers. The α -Al₂O₃:C phosphor powder and single crystals, both being OSL grade materials, are available from Landauer Inc., USA.

Two typical TL glow curves for A_2O_3 : C and $CaSO_4$: Dy phosphors are given in Figs. 2 and 3.

Fig. 2 Typical TL glow curve of Al_2O_3 : C phosphor

Fig. 3 Typical TL glow curve of CaSO4:Dy phosphor

4.**9 BeO-based TL Phosphor.** Beryllium oxide (BeO) is a material with a long history in TL dosimetry. Special interest in BeO as a potential material for personnel dosimetry is determined by its low effective atomic number (Z_{eff} =7.13), which is very close to that of the biological tissue (Z_{eff}) =7.42). Some of the TL properties of BeO have been reported in literature [19, 177, 191-193]. BeO in powder form is extremely toxic, leading to a condition known as *berylliosis*. Therefore, only specially equipped laboratories can use/handle it in powder form. Sintered pellets (prepared by

sintering at a temperature ~ 1500 °C) are also available which are used as transistor bases in the electronic industry. In this ceramic form, material presents no danger as long as abrasion of the surfaces and therefore production of powder and dust is avoided [19, 177]. Out of all the BeO ceramics manufactured, Crase and Gammage [192] identified BeO ThermaloxTM 995 as the most suitable for TL dosimetry. Dose response curve of the main dosimetric peak (220 $^{\circ}$ C) of BeO (ThermaloxTM 995) is linear-supralinear-sublinear. The linear region extends from approximately 10 mR up to 100 R where it becomes supralinear. The curve starts to saturate at exposure levels of \sim 10^4 R. Sensitivity of BeO is comparable to that of LiF:Mg,Ti [177]. TL emission spectrum of BeO ThermaloxTM 995 consists of a main emission at \sim 335 nm. As per Busuoli et al. [194], a twoelement dosimeter using BeO (Thermalox 995) discs, 4 mm in diameter, had been developed and the dosimetric characteristics of the TL dosimeter were reported. Investigations carried out during the last decade [195] have shown that in the optically stimulated luminescence (OSL) mode, BeO has higher sensitivity than in the TL mode.

4.10 BaSO₄: Eu TL Phosphor. Eu^{2+} - doped phosphors have been investigated for their TL and OSL response. This is possibly due to the allowed nature of $4f^65d \rightarrow 4f^7$ transition on Eu²⁺ ion. Also, the emission spectra of Eu^{2+} doped phosphors lie in the peaking region of the response of commonly available photomultiplier tubes (PMTs). Therefore, Eu^{2+} -doped phosphors yield good PL and TL. Okamoto et al. [196] reported the development of $\text{BaSO}_4:\text{Eu}^{2+}$ TL phosphor and phosphor embedded Teflon TL sheets for study of hadronic and electromagnetic cascade showers in ultrahigh energy interactions. The $BaSO_4:Eu^{2+}$ (Japan) Teflon TL sheet was reported as an effective detector because of its high sensitivity for detection of cascade showers (around 1 TeV), high position resolution of about 50 µm, wide dynamic dose range and little thermal fading of stored TL signal. TL sensitivity of BaSO₄:Eu embedded Teflon disc was reported to be \sim 4-6 times that of CaSO₄:Dy embedded Teflon discs [197,198]. Annalakshmi et al. [199] reported the preparation of $BaSO₄:Eu$ by solid-state reaction in different reducing atmospheres. The TL glow curve of $BaSO₄:Eu²⁺$ showed only a single peak at 513 K unlike other phosphors and the TL intensity is about three to four times higher than that of CaSO4:Dy. The TL dose response of the phosphor was found to be linear up to the dose range of $10³$ Gy beyond which saturation sets in. Although BaSO₄:Eu is not a tissue equivalent material, due to its good TL and OSL sensitivity and wide dynamic range, it can be used for relative dose measurements for applications in radiation dosimetry. Also, its high sensitivity can be used for imaging applications similar to that of CaSO4:Dy and LiF:Mg,Cu,P in TL mode, and of BaFBr:Eu in PSL/OSL mode.

4.11 TL of Nanophosphors. Thermoluminescence (TL) of phosphor materials is successfully used for personnel and environmental monitoring, retrospective dosimetry, as well as for medical physics applications. Commercial TL dosimetry systems providing high sensitivity and low fading have been designed on the basis of these materials and put to successful operation. However, the dose range of these traditional phosphors is normally not over 100 Gy, while higher doses need to be measured in technological and medical applications (e.g. sterilization of medical products, irradiation of food products, etc.). In this connection, various nanophosphors have been synthesized and studied for their possible application in radiation dosimetry. Nanophosphors present a type of phosphors consisting of particles 10-100 nm in size, which include nanopowders, pressed compacts, nanoceramics, thin films on substrates, nanopowder coatings of different thickness, etc. [200]. Nanophosphors, such as CaSO₄:Dy and BaSO₄:Eu, were prepared by Salah and Sahare coworkers [201-205] who studied their TL characteristics with the objective of their application in radiation

dosimetry. TL sensitivity of nanocrystalline phosphors, at low doses, was found to be much less than that of their bulk analogues. But the dose vs. TL response of these nanophosphors did not saturate up to the studied dose of $5 - 20$ kGy. Most of these nanophosphors were prepared by chemical co-precipitation method. It is reported that TL glow curves of the nanophosphors show multiple peaks compared to their bulk analogues, and TL maxima of the dosimetry peak appear

shifted relative to the main dosimetric peak in polycrystalline phosphors. Nanophosphors of LiF:Mg,Cu,P and $Ba_{0.97}Ca_{0.03}SO₄$:Eu may be useful for dosimetry of high LET beams [204, 205].

For nanoparticles, increase in surface to volume ratio would lead to formation of high concentration of surface defects, including F-type surface centres. The appearance of multiple peaks in nanophosphors has also been related to high concentration of surface trapping centres/defects. Specific causes of low luminescence efficiency are not known. For nanophosphors, after gamma or beta irradiation, spontaneous recombination losses may occur, which result in less storage in terms of trapping in metastable states. This could be one of the reasons for observing less intense TL peak in nanophosphors than in their bulk analogues at relatively low doses. Increase in surface defects may lead to increase in non-luminescent relaxation processes. Kortov [200] explained the higher radiation resistance of nanophosphors (which is also the reason for extended dose response) as due to efficient sinking and annihilation of defects at nano-grain boundaries; as a result, accumulation of defects in nanomaterial is retarded. Jacobsohn et al. [206] showed that degree of crystallinity and the presence of impurities, including OH⁻ groups, are detrimental to luminescence efficiency in nanophosphors. In this context, it is interesting to note that nanosheets of CaSO₄:Mn and CaSO₄:Ce, having an average thickness of 35 nm, synthesized by hydrothermal method [207, 208], gave TL sensitivity 8-10 times higher than that of LiF:Mg,Cu,P(GR-200) commercial phosphor hot-pressed chips (about 200 times that of LiF:Mg,Ti(TLD-100)). CaSO4:Mn nanocrystalline phosphor gave three TL peaks at 485, 504 and 526 K, compared to a prominent TL peak at about 373K in polycrystalline phosphor. Its dose response was linear up to 7 Gy, before leading to saturation at higher doses. This indicates that the method of synthesis used plays an important role in determining the characteristics of nanophosphor. The authors have recommended these two highly sensitive phosphors for environmental monitoring. In this context, it may be mentioned here that LiF:Mg,Cu,P(GR-200) gives wide dynamic dose response in the range 1 μ Gy to 10 Gy, its minimum detectable dose was reported to be 60 nGy to 1 μ Gy. Unfortunately, the dose response of the new CaSO4:Mn nanocrystalline phosphor was given in Gy level. Also, minimum detectable dose was not reported for the developed phosphors. Thus, it is difficult to assess applicability of these highly sensitive phosphors for environmental monitoring.

Soft tissue equivalence $(Z_{\text{eff}} = 7.4)$ of diamond (Z=6) and its chemical stability make it an attractive material for dosimetry, particularly for medical applications. Chemical vapour deposited (CVD) polycrystalline diamond films exhibited a prominent TL peak at about 280° C with linear dose response up to 20 Gy [209]. However, the synthesis process and growth conditions can strongly influence the TL signal in CVD diamond. Recently, nano-diamond films grown from Tequila using pulsed-liquid injection chemical vapour deposition (PLICVD) technique has been reported to be promising for the high-dose dosimetry [210]. Nano-diamond thin films show TL glow curve with peaks at 170 and 350 $^{\circ}$ C. The dose response of these films was reported to be linear in the dose range 100 to 1600 Gy. However, direct comparison of TL sensitivities of CVD polycrystalline diamond and nano-diamond films is not readily available in the published literature. Thus, nanophosphors could find many potential applications in the field of radiation dosimetry, such as low-energy beta dosimetry, high-LET dosimetry, and high-dose dosimetry for technological applications.

4.12 Phosphors based on Other Luminescence Techniques. In the last two decades an alternative technique, optically stimulated luminescence (OSL), has been developed, as the optical nature of the readout process does not involve problems of blackbody radiation and thermal quenching. Due to this and some other advantages, OSL is also being used for various applications in radiation dosimetry, such as personnel and environmental dosimetry, retrospective/accident dosimetry and medical dosimetry. The development of Al_2O_3 :C TL/OSL phosphor by Akselrod et al. [26] and later investigation of its suitability for personnel dosimetry using pulsed OSL (POSL) technique of stimulation by Akselrod and McKeever [211], resulted in the development of a personnel dosimetry system based on A_2O_3 :C OSL phosphor. Applications of OSL phosphors in different fields have been highlighted in a number of publications [212-214]. Although radio-photoluminescence (RPL) dosimeters were developed in parallel with TLD systems during 1960s, but high pre-dose and photon energy dependent detector material prevented major breakthrough of the glass dosimetry. However, in mid 1980s, introduction of readout systems using a pulsed UV stimulation, in place of conventional mercury UV lamps, helped in reducing pre-dose by a factor of 100 (from mSv to a few µSv) [215]. This development resulted in the manufacture of improved RPL glass dosimeters and fully automatic RPL reader systems capable of measuring doses in the range 10µSv to 10Sv. Applications of RPL glass dosimeters have been highlighted in a number of publications [216, 217]. Advantages and disadvantages of TL and OSL techniques have been given by McKeever and Moscovitch [218], and Olko [219]. Recently, Bhatt [220] has given comparative advantages of TL, OSL and RPL dosimeters.

5. Important Areas of Radiation Dosimetry

- Personnel monitoring
- Environmental dosimetry
- Neutron dosimetry
- Dosimetry in medical applications of radiation
- Retrospective dosimetry
- High dose dosimetry
- Space dosimetry

5.1 Personnel Monitoring. The primary objective of personnel monitoring/individual monitoring is the measurement or assessment of radiation dose delivered to personnel during their occupational exposure (ICRP-60, 1991) [221]. Examples include workers in nuclear industry, hospital radiotherapy technicians, workers in industrial radiography and high intensity gamma irradiators, etc. In addition, the objectives of personnel monitoring for external exposures include the following objectives [221, 222]:

- 1. It is intended to provide information on the external radiation exposure of individuals working with radioactive materials and/or radiation producing devices;
- 2. Personnel monitoring results provide information on routine exposures, assist in work planning, allow control of the workplace, and provide exposure information in accident situations;
- 3. By means of such monitoring it is hoped to limit the exposure of such personnel to within prescribed limits, which are based on recommendation of international and national bodies;
- 4. Assessment of effective dose and, if appropriate, equivalent doses for compliance purposes;
- 5. In addition, these results assist those responsible for radiation safety in keeping exposures as low as reasonably achievable (ALARA).

As per UNSCEAR 2008 Report [223, 224], about 10 million workers are exposed to radiation from artificial sources, which include medical uses sector, nuclear fuel cycle, industrial uses, miscellaneous uses and military activities. External monitoring of these radiation workers is carried out using personnel dosimetry badges, which include thermoluminescent dosimeters (TLDs), optically stimulated luminescent dosimeters (OSLDs), radiophotoluminescent dosimeters (RPLDs), and film badges [225]. These personnel dosimeters should comply with IEC requirements for "passive integrating dosimetry systems for personal and environmental monitoring" [226, 227]. Due to non-reliability of photographic film for long-term stability of stored information, particularly in tropical climates, this method of personnel dosimetry has nearly phased out and being replaced by TL, OSL and RPL methods of personnel dosimetry.

5.2 Environmental Dosimetry. In the last two decades regulatory authorities in many countries have become more acutely aware of the increasing concern demonstrated by the public with regard to the potential environmental impact of "man-made" radiation exposure such as: (i) controlled releases of gaseous radionuclides from nuclear power stations during day-to-day operations, (ii) low-level waste disposal, (iii) nuclear fuels reprocessing, (iv) incidents of nuclear power station accidents, and (v) activities connected with nuclear power industry. In many countries, TLD systems are in place near nuclear installations for the purpose of monitoring pre-operational levels (background levels) as well as levels above the natural background, which can be linked with the operation of these facilities. Important requirements of TLD materials are: (i) Tissue equivalence is not an issue, (ii) since exposure levels are low, long exposure times are required, and long-term stability becomes vitally important, along with high sensitivity, and (iii) gamma emitters are the main radiation sources of interest. Detection threshold or minimum detectable dose of $\sim 10 \mu Gy$ is expected for environmental monitoring [226, 227].

A number of phosphors, such as $CaSO₄:D_V$, $CaSO₄:Tm$, $CaF₂:D_V$ (TLD-200), and LiF:Mg,Cu,P are quite suitable for this purpose. In India, natural $CaF₂$ filled in 1.5 mm thick brass capsules are used for environmental monitoring for determining pre-operational levels in and around the site of nuclear power stations and subsequently, periodically, after commissioning of the power stations. Performance of these dosimeters for their use in environmental monitoring has been assessed during a series of inter-comparison experiments for environmental dosimetry; their performance was very good [228, 229]. Recently, BARC developed an automated PC based TLD reader system by modifying the existing personnel monitoring card dosimeter from three-element to two-element CaSO4:Dy embedded Teflon TLD disc (each disc covered with 1 mm thick copper filter) for the environmental gamma monitoring [230].

5.3 Neutron Dosimetry. Fast neutrons are of great interest and importance to radiobiologists and medical and health physicists as they have much larger biological effectiveness as compared to Xand gamma rays; and personnel are more often exposed to significant doses from fast neutrons than they are from thermal neutrons. TL dosimeters are being used for the detection of X-, gamma and beta radiations, and these methods are well established, reliable and quite accurate. However, direct fast-neutron response of TL and other luminescent materials is very small because of poor crosssection of the constituent elements to most of the nuclear reactions at high neutron energies. Al_2O_3 :C has neutron sensitivity lower than ⁷LiF:Mg,Ti (TLD-700) [231]. Thus measurement of dose due to fast neutrons remains one of the challenging tasks in luminescence radiation dosimetry. TL phosphors have been tried for fast neutron dose measurements by:

- i) Irradiating them in contact with hydrogen-rich organic materials used as proton radiators [232];
- ii) Activation of some of the constituent elements of the material using threshold nuclear reactions;
- iii) Use of high LET sensitive TL peaks (e.g. 250 $^{\circ}$ C TL peak in CaF₂: Tm) [183]; and
- iv) Use of Albedo technique.

The most commonly used TLD technique for personnel monitoring in neutron fields, however, is *albedo* dosimetry. Fast neutrons are moderated and backscattered from the body. These scattered thermal neutrons are detected by thermal neutron sensitive TL detectors. By using a pair of TLDs, one having sensitivity to both thermal neutron and gamma rays (e.g., 6 LiF) and other having sensitivity only to gamma rays (e.g., 7 LiF), the net dose due to neutrons (thermal, intermediate and fast) can be estimated together with gamma ray component. Highly sensitive TL or OSL materials could be made neutron sensitive (by mixing with enriched ⁶LiF powder) and other component neutron insensitive (i.e. without mixing with δ LiF powder). Yukihara et al. [233] demonstrated the possibility of producing neutron sensitive OSL dosimeters using a mixture of Al_2O_3 :C and ⁶LiF or ${}^6\text{Li}_2\text{CO}_3$ neutron converters.

5.4 Dosimetry in Medical Applications of Radiation. One of the important applications of TL and OSL dosimetry has been in the field of medical physics for their application in radio-diagnosis, nuclear medicine and radiotherapy. Thermoluminescent dosimeters (TLDs) have become popular in these fields due to their high sensitivity, miniature size, tissue equivalence, high stability to environmental conditions, low TL fading, reusability, linear dose response and sufficient precision and accuracy. Integrating mode of TL phosphors, such as LiF:Mg,Ti, LiF:Mg,Cu,P, Al₂O₃:C, has been widely used for clinical dosimetric measurements, e.g., central axis depth-dose curves, inphantom measurements, in-vivo dosimetry, surface doses, quality assuarance, etc., of high energy photon and electron beams [234]). Applications of OSL phosphors in medical dosimetry are described by Akselrod and McKeever [212], Pradhan [235], and Yukihara and McKeever [214].

5.5 Retrospective Dosimetry. In situations where no direct radiation monitoring data are available, luminescence dose reconstruction obtained using material from the immediate environment of population or from the persons in the vicinity of the incident/accident can be used to validate values obtained from computational techniques. TL technique has been successfully employed in dose evaluation in Hiroshima and Nagasaki Atomic bomb explosion sites in Japan, radioactive fallout of nuclear tests at Nevada test sites in USA, and radioactive fallout from the Chernobyl nuclear reactor accident. The OSL technique has also been applied to retrospective dosimetry using environmental materials from the Chernobyl accident area [236].

OSL properties of memory chip modules (from telephone, ID and credit cards), ceramic resistors from mobile phones and other electronic components from personal electronic devices have shown interesting and promising results for their use in accident dosimetry [237-239]. Recently, the European Radiation Dosimetry Group10 on Retrospective Dosimetry has published a "Review of Retrospective Dosimetry Techniques for External Ionizing Radiation Exposures" [240].

5.6 High Dose Dosimetry. Since, dose vs TL response of all commonly known TL phosphors saturates at about 10^3 Gy, dose response of high temperature TL peak (400 $^{\circ}$ C) as well as phototransferred TL (PTTL) response of the dosimetry peak (230°C) in CaSO4:Dy and CaSO4:Tm has been investigated [241, 242] for high dose dosimetry in the range $10^2 - 10^6$ Gy. Fig. 4(a) shows the dose response of dosimetry (250 °C) and RTL peaks occurring at 400 and 485 °C, as well as PTTL response at the dosimetry peak in CaSO4:Dy [243]. The dose response of high temperature peak $(-400^{\circ}$ C) saturates above a gamma ray dose of $1.2x10^6$ Gy, whereas PTTL response of 230°C peak saturates at a γ -dose of 5 x 10⁵ Gy. Fig. 4(b) shows relative intensity of PTTL peak (250 ^oC) as function of UV (254 nm) exposure duration.

Fig. 4 (a) Dose versus TL response of dosimerty (250 $^{\circ}$ C) and RTL peaks occurring at 400 and 485 \degree C, as well as PTTL response at the dosimetry peak in CaSO₄:Dy. (b) Relative intensity of PTTL peak $(250 \degree C)$ as function of UV (254 nm) exposure duration (adopted from Ref. [243]).

Obryk et al. [244] report that on the basis of the newly discovered behaviour of LiF:Mg,Cu,P detectors at high and ultra-high doses, a new method of thermoluminescence (TL) measurement of radiation doses ranging from micro-Grays up to a mega-Grays has been recently developed at the Institute of Nuclear Physics, Warsaw (Poland). The method is based on the relationship between the TL signal, integrated in the given temperature range and dose. It is quantified by a parameter called the 'ultra-high temperature ratio'. It has been demonstrated that this new method can measure radiation doses in the range of about 1 μ Gy to 1 MGy, using a single LiF:Mg,Cu,P detector. This method was recently successfully blindly tested for 10 MeV electrons up to doses of 200 kGy. It can be used for dosimetry in high-energy accelerators, especially in the Large Hadron Collider at CERN, and has great potential for accident dosimetry in particular.

Recently, Kortov et al. [245] have described advantages and challenges of high-dose thermoluminescent detectors. High-dose luminescent dosimetry is high-temperature one in the majority of cases. It employs TL peaks from deep traps present in the detector material or brought about by high-dose irradiation. Using TL deep traps in Al_2O_3 :C, it is possible to measure the absorbed dose up to 100 kGy. Heating $(900 \degree C, 1 \text{ h})$ of highly irradiated TLD-500 detectors restore their initial properties. Kortov et al. [240] have commented that the thermally assisted- OSL (TA-OSL) method, recently suggested by Soni et al. $[246]$ in Al_2O_3 :C, is an excellent advancement of high-dose luminescent dosimetry with involvement of deep traps.

5.7 Space Dosimetry. The radiation environment in space is a complex mix of charged particles: medium and high-energy protons, electrons, alpha particles and high-energy heavy ions, over wide energy ranges and with varying fluxes [247]. Astronauts working in Low Earth Orbit (LEO) are exposed to a radiation level, which is about 100 times higher than the natural radiation level on Earth and will be further increased for travels to Mars. Due to the variety of routine space crew activities on the International Space Station (ISS) and the Space Shuttle, there is a need to monitor the individual radiation exposures of the crew members for reliable estimation of radiation risk to them. TL and OSL detectors have good efficiency for LET of radiation ≤ 10 keV/ μ m, with decreasing efficiency, although non-zero, for higher LET ($> 10 \text{ keV/\mu m}$) radiation [214, 248, 249]. Therefore, no single dosimeter will provide absorbed dose estimates across the full LET spectrum of space radiation. Thus, combinations of dosimeters are required to estimate the dose equivalent due to space radiation. Currently, this is performed using passive detectors such as thermoluminescent detectors (TLDs) or optically stimulated luminescence dosimeters (OSLDs) and plastic nuclear track detectors (PNTDs). However, suitable correction needs to be applied for the response of TLDs or OSLDs for LET $> 10 \text{ keV}/\text{µm}$.

6. **Summary**

This review discusses in detail the role of 'Thermoluminescent Phosphors' in the field of Radiation Dosimetry. Synthesis of TLD materials, to be used as phosphors, for example, Lithium Fluoride (LiF:Mg,Ti, and LiF: Mg,Cu,P), Lithium Tetraborate, Magnesium Borate, Calcium Fluoride (CaF2), $CaSO_4:Dy/Tm$, Ba $SO_4:Eu$, Magnesium Orthosilicate-based, Al_2O_3 – based, BeO-based TL Phosphors, and their characterization constitutes the core of this review. A good number of highly sensitive and near-tissue equivalent TL phosphor materials have been developed, characterized and recommended for dosimetric use by various researchers. However, these developed phosphors should comply with IEC requirements for "passive integrating dosimetry systems for personal and environmental monitoring". Only then they could be useful for their practical application in radiation dosimetry. As per the present international scenario, LiF:Mg,Cu,P (in TL mode) and $A₁Q₃$:C (in OSL mode) are the vanguards of the luminescence dosimetry programmes. These two phosphors comply with all the IEC requirements of passive integrating dosimetry systems. With the present interest in TL and OSL materials development, it is hoped that new and more sensitive luminescent materials will be available in the coming years for use in field of radiation dosimetry.

Acknowledgements

Authors are thankful to Dr. D.N. Sharma, Director, Health, Safety and Environment Group of BARC, Trombay for the support and encouragement. B.C.B is thankful to DST for the award of fellowship.

References

- [1] F. Urbach, Zur Lumineszenz der Alkalihalogenide, Wiener Ber., IIa 139 (1930) 363-372.
- [2] J.T. Randalls, M.H.F. Wilkins, Phosphorescence and electron traps,Proc. Royal Soc. (Lond.) 184 (1945) 366-407.
- [3] G.F.J. Garlick, A.F. Gibson, The electron trap mechanism of luminescence in sulphide and silicate phosphors, Proc. Phys. Soc. A60 (1948) 547-590.
- [4] D.T. Bartlett, 100 years of solid state dosimetry and radiation protection dosimetry, Radiat. Meas. 43 (2008)133-138.
- [5] F. Daniels, C.A. Boyd and D.F. Saunders, Thermoluminescence as a research tool, Science 117 (1953) 343-349.
- [6] J.R. Cameron, N. Suntharalingham and G.N. Kenny, Thermoluminescence Dosimetry, Univ. of Wisconsin Press, Madison, 1968.
- [7] J.R. Cameron and G.N. Kenny, Thermoluminescent radiation dosimetry with lithium fluoride. Radiat. Res. 19 (1963) 199-200.
- [8] J.K. Rieke, F. Daniels, Thermoluminescence studies of aluminium oxide, J. Phys. Chem. 61 (1957) 629-633.
- [9] H.W. Leverenz, Luminescent solids (phosphors), Science 109 (1949) 183-195.
- [10] D. Curie, Luminescence in Crystals, 3rd Ed., John Wiley & Sons Inc, New York, 1963.
- [11] M. J. Aitken, M.S. Tite and J. Reid, Thermoluminescent dating of ancient ceramics, Nature 202 (1964) 1032-1033.
- [12] M.J. Aitken, D. W. Zimmermann and S.J. Fleming, Thermoluminescent dating of ancient pottery, Nature 219 (1968) 442-445.
- [13] First Int. Conf. on Luminescence Dosimetry, Stanford University, USA, June 21-23, 1965, CONF. 650637, (Ed.) F.H. Attix (1965).
- [14] Second Int. Conf. on Luminescence Dosimetry, Tennessee, USA, Sept. 23-26, 1968, CONF. 680920, (Eds.) J. A. Auxier, K. Becker, E. M. Robinson (1968).
- [15] Thermoluminescence of Geological Materials, Proc. of a NATO Advanced Research Institute on Applications of Thermoluminescence in Geological Problems, Academic Press, London, (Ed.) D.J. McDougall (1968).
- [16] Third Int. Conf. on Luminescence Dosimetry, Riso, Denmark, Oct. 11-14, 1971, Danish AEC Report No. 249, (Ed.) V. Mejdahl (1971).
- [17] Fourth Int. Conf. on Luminescence Dosimetry, Krakow, Poland, August 27- 31, 1974, Institute of Nuclear Physics, Krakow, Poland, (Ed.) T. Niewiadomski (1974).
- [18] S.W.S. McKeever, Thermoluminescence of Solids, Cambridge University Press, 1985.

- [19] S.W.S. McKeever, M.Moscovitch, P.D. Townsend, Thermoluminescence Dosimetry Materials: Properties and Uses, Nuclear Technology Publishing, Ashford, Kent, England, 1995.
- [20] M. Takenaga, O. Yamamoto, T. Yamashita, Preparation and characteristics of Li2B4O7:Cu phosphor, Nucl. Instrum. Meth. 175 (1980) 77-78.
- [21] B. F. Wall, C. M. H. Driscoll, J. C. Strong and E. S. Fisher, The suitability of different preparations of thermoluminescent lithium borate for medical dosimetry, Phys. Med. Biol. 27 (1982) 1023-1034.
- [22] C.M.H. Driscoll, A.F. McWhan, J.B. O'Hagan, J.Dodson, S.J. Mundy, C.D.T. Todd, TL characteristics of new LiF preparations and sensitized LiF, Radiat. Prot. Dosim. 17 (1986) 367-371.
- [23] M. Prokic, L. Botter-Jensen, Comparison of main thermoluminescent properties of some TL dosemeters, Radiat. Prot. Dosim. 47 (1993) 195-199.
- [24] Z. Zha, S. Wang, W. Shen, J. Zhu, G. Cai, Preparation and characteristics of LiF:Mg,Cu,P thermoluminescent material, Radiat. Prot. Dosim. 47 (1993)111-118.
- [25] J.L. Kim, J.I. Lee, A.S. Pradhan, B.H. Kim, J.S. Kim, Further studies on the dosimetric characteristics of LiF:Mg,Cu,Si—A high sensitivity thermoluminescence dosimeter (TLD), Radiat. Meas. 43 (2008) 446-449.
- [26] M.S. Akselrod,V.S. Kortov, D.J. Kravetsky, V.I.Gotlib, Highly sensitive thermoluminescent anion-defective Al2O3:C single crystal detectors, Radiat. Prot. Dosim. 32 (1990) 15-20.
- [27] Bhuwan Chandra, A.R. Lakshmanan, R.C. Bhatt, Annealing and re-usability characteristics of LiF:Mg,Cu,P TLD phosphor, Radiat. Prot. Dosim. 3 (1982) 161-167.
- [28] M. Prokic, Development of highly sensitive CaSO4:Dy/ and MgB4O7:Dy/Tm sintered thermoluminescent dosimeters, Nucl. Instrum. Meth. 175 (1980) 83-86.
- [29] T. Hashizume, Y. Kato, T. Nakajima, H. Sakamoto, N. Kotera, S. Eguchi, A new thermoluminescence dosemeter of high sensitivity using a magnesium silicate phosphor. In: Proc. Symp. on Advanced Radiation Detectors, IAEA-SM143/11, Vienna, Austria (1971), p. 91.
- [30] M. Prokic, E.G. Yukihara, Dosimetric characteristics of high sensitive Mg2SiO4:Tb solid TL detector, Radiat. Meas. 43 (2008) 463–466.
- [31] B.C. Bhatt, S.S. Sanaye, S.S. Shinde, J.K. Srivastava, A comparative study of the dosimetric characteristics of BaSO4:Eu and CaSO4:Dy Teflon TLD discs, Radiat. Prot. Dosim. 69 (1997) 105-110.
- [32] P.R. Gonza´lez, C. Furetta, B.E. Calvo, M.I. Gaso, E. Cruz-Zaragoza, Dosimetric characterization of a new preparation of BaSO4 activated by Eu ions, Nucl. Instrum. Meth .B 260 (2007) 685-692.
- [33] K. Becker, Solid State Dosimetry, CRC Press, Boca Raton, Fl., USA, 1973.
- [34] A.F. McKinley, Thermoluminescence Dosimetry, Adam Hilger, Bristol, 1981.
- [35] M. Oberhofer and Scharmann, Applied Thermoluninescence Dosimetry, Adam Hilger, Bristol, 1981.
- [36] Y.S. Horowitz (Ed.), Thermoluminescence and Thermoluminescence Dosimetry, Vols.1-3, CRC Press, Boca Raton, Fl., USA, 1983.
- [37] S.W.S McKeever (Ed.), Thermoluminescence Marerials, Special Issue, Radiat. Prot. Dosim. 8 (1/2) (1984).
- [38] K. Mahesh, P.S. Weng and C. Furetta, Thermoluminescence in Solids and its Applications, Nuclear Technology Publishing, Ashford, UK, 1989.
- [39] D.R.Vij (Ed.), Thermoluminescence Materials, Prentice Hall, Englewood Cliffs, 1993.
- [40] A.S. Pradhan, Thermoluminescence dosimetry and its applications, Radiat. Prot. Dosim. 1 (1981) 153-167.
- [41] J. Azorin, C. Furetta and A. Scacco, Preparation and properties of thermoluminescent materials, Phys. Stat. Sol. (a) 138 (1993) 9-46.
- [42] G. Portal, Review of the principal materials available for thermoluminescence dosimetry, Radiat. Prot. Dosim. 17 (1986) 351-357.
- [43] A.J.J. Bos, High sensitivity thermoluminescence dosimetry, Nucl. Instrum. Meth. Phys. Res. B 184 (2001) 3-28.
- [44] T. Yamashita, N. Nada, H. Onishi, and S. Kitamura, Calcium sulphate activated by thulium or dysprosium for thermoluminescent dosimetry, Health Phys. 21(1971) 295–300.
- [45] Harshaw Chemical Company, US patent, 1059518, published (1967).
- [46] G. Portal, Rep. CEA-R-4943 (France), 1978.
- [47] T. Niewiadomski, 25 Years of TL Dosimetry at the Institute of Nuclear Physics, Krakow, Radiat. Prot. Dosim. 65 (1996) 1-6.
- [48] RADCARD (former TLD Poland) (www.radcard.pl)
- [49] Solid Dosimetric Detector & Method Laboratory (DML), P.R. China (www.chinadml.com).
- [50] V.V. Kolotilin, V.I. Hokhrekov, L.M. Tarasova and S.B. Zakhriapin, A high sensitivity LiF:Mg, Cu,P thermolumonscent dosimeter, Nucl. Tracks Radiat. Meas. 21 (1993) 169- 171.
- [51] P. Olko, L. Currivan, J. W. E. van Dijk, M. A. Lopez and C. Wernli, Thermoluminescent Detectors Applied in Individual Monitoring of Radiation Workers in Europe - A Review based on the Eurados Questionnaire, Radiat. Prot. Dosim. 120 (2006) 298-302.
- [52] C. M. H. Driscoll, A. McWhan and D.J. Richards, A Comparative Study of the Sensitivity and Fading Characteristics of Thermoluminescent LiF Chips, Radiat. Prot. Dosim. 11(1985) 119-121.
- [53] G. Holzapfel, J. Lesz and K. Sujak-Lesz, TLD system with a stacked dosimeter configuration. Radiat. Prot. Dosim. 47 (1993) 469–471.
- [54] F. Busch, J. Engelhardt, E. Martini and J. Lesz, A Whole-Body Dosimetry System for Personal Monitoring Based on Hot-Pressed Thin Layer TLD, Radiat. Prot. Dosim. 144 (2011) 246-248.
- [55] M.R. Mayhugh and G.D. Fullerton, Thermoluminescence in LiF: Usefulness of sensitization by pre-irradiation, USAEC Report COO-1105-209 (1974).
- [56] M.W. Charles, H.D. Mistry and Z. U. Khan, The theory and practice of simultaneous sensitization and re-estimation in lithium fluoride, Nucl. Instrum. Meth. 175 (1980) 51-53.
- [57] Bhuwan Chandra, A. R. Lakshmanan and R. C. Bhatt, Effect of Deep Traps on the Sensitization in LiF (TLD-100) Phosphor, Phys. Stat. Solidi (a) 60 (1980) 593.
- [58] A.R. Jones, The applicability of sensitized lithium fluoride TLDs to personnel and environmental dosimetry, Nucl. Instrum. Meth. 175 (1980) 145-146.
- [59] Bhuwan Chandra, A.R. Lakshmanan and R.C. Bhatt, Incompatibility of Radiation Induced Sensitization and Re- estimation at Low Absorbed Doses in LiF TLD-100, Nucl. Tracks. 10 (1985) 77-81.
- [60] T. Nakajima, Y. Murayama, T. Matsuzawa, and A. Koyano, Development of a New Highly Sensitive LiF Thermoluminescent Dosimeter and its Application, Nucl. Instrum. Methods 157 (1978) 155-162.
- [61] T. Nakajima, Y. Murayama, and T. Matsuzawa, Preparation and Dosimetric Properties of a Highly Sensitive LiF Thermoluminescent Dosimeter, Health Phys. 36 (1979) 79-82.
- [62] D. K. Wu, F.Y. Sun, H.C. Dai, A High Sensitivity LiF Thermoluminescent Dosimeter-LiF(Mg, Cu, P), Health Phys. 46 (1984) 1063-1063.
- [63] T. Niwa, H. Morishima, T. Koga, H. Kawai and Y. Nishiwaki, Single Crystal LiF Thermoluminescence Dosemeters, Radiat. Prot. Dosim. 6 (1983) 333-334.
- [64] S. Wang, G.R. Chen, F. Wu, Y.F. Li, Z.Y. Zha, and J.H. Zhu, Newly Developed Highly Sensitive LiF:Mg,Cu,P TL Chips with High Signal-to-Noise Ratio, Radiat. Prot. Dosim. 14 (1986) 223-227.
- [65] S. Wang, The Dependence of Thermoluminescence Response and Glow Curve Structure of LiF:Mg,Cu,P Material on Mg, Cu, P Dopants Concentration. Radiat. Prot. Dosim. 25 (1988) 133-136.
- [66] S. Wang, G. Cai, K. Q. Zhou and R. X. Zhou, Thermoluminescent Response of 6LiF(Mg,Cu,P) and 7LiF(Mg,Cu,P) TL Chips in Neutron and Gamma Ray Mixed Radiation Fields, Radiat. Prot. Dosim. 33 (1990) 247-250.
- [67] W. Shen, K. Tang, H. Zhu and B. Liu, New Advances in LiF:Mg,Cu,P TLD(GR-200A), Radiat. Prot. Dosim. 100 (2002) 357-360.
- [68] A. Horowitz and Y.S. Horowitz, Optimisation of LiF:Mg,Cu,P for Radiation Protection Dosimetry, Radiat. Prot. Dosim. 33 (1990) 267-270.
- [69] J. Azorin, A. Gutiérrez, T. Niewiadomski and P. González, Dosimetric Characteristics of LiF:Mg,Cu,P TL Phosphor Prepared at ININ, Mexico, Radiat. Prot. Dosim. 33 (1990) 283- 286.
- [70] S. S. Shinde, B. S. Dhabekar, T. K. Gundu Rao, and B. C. Bhatt, Preparation, thermoluminescent and electron spin resonance characteristics of LiF:Mg,Cu,P phosphor, J. Phys. D: Appl. Phys. 34(2001) 2683-2689.
- [71] R. R. Patil and S. V. Moharil, On the role of copper impurity in LiF:Mg,Cu,P phosphor, J. Phys.: Condens. Matter 7 (1995) 9925-9933.
- [72] Y.M. Nam, J.L. Kim and S.Y. Chang, Dependence of glow curve structure on the concentration of dopants in LiF:Mg,Cu,Na,Si phosphor. Radiat. Prot. Dosim. 84 (1999) 231–234.
- [73] H. Jung, K. J. Lee, J. L. Kim, A personal thermoluminescence dosimeter using LiF:Mg,Cu,Na,Si detectors for photon fields, Appl. Radiat. Isot. 59 (2003) 87-93.
- [74] Lee, J. I., Kim, J. L., Chang, S. Y., Chung, K. S. and Choe, H. S. On the roles of dopants in LiF:Mg,Cu,Na,Si thermoluminescent material, Radiat. Prot. Dosim. 115 (2005) 340–344.
- [75] K. Tang, H. Zhu, W. Shen, B. Liu, A new high sensitivity thermoluminescent phosphor with low residual signal and good stability to heat treatment: LiF:Mg,Cu,Na,Si, Radiat Prot. Dosim.100 (2002) 239-242.
- [76] K. Tang, Dependence of thermoluminescence in LiF:Mg,Cu,Na,Si phosphor on Na dopant concentration and thermal treatment, Radiat. Meas. 37 (2003) 133-140.
- [77] J.I. Lee, J.S. Yang, J.L. Kim, A.S. Pradhan, J.D. Lee, K.S. Chung, and H.S. Choe, Dosimetric characteristic of LiF:Mg,Cu,Si thermoluminescence materials, Appl. Phys. Lett. 89 (2006) 094110-3.
- [78] J.I. Lee, J.L. Kim, A.S. Pradhan, B.H. Kim, K.S. Chung, and H.S. Choe, Role of dopants in LiF TLD materials, Radiat. Meas. 43 (2008) 303–308.
- [79] J.I. Lee, J.L. Kim, M.S. Rahman, S.Y. Chang, K.S. Chung, H.S. Choe, Development of LiF:Mg,Cu,Si TL material (new KLT-300) with a low-residual signal and high-thermal stability, Radiat Prot Dosimetry, 125 (2007) 229-232.
- [80] M.S. Rahman, J.I. Lee, J.L. Kim, G. Cho, Dosimetric Properties of the Newly Developed LiF:Mg,Cu,Si TL Material, J. Sci. Res. 5(1) (2013) 25.
- [81] J.L. Kim, J.I. Lee, I. Chang, A.S. Pradhan, S.I. Kim, B.H. Kim, TL response of pairs of 6LiF:Mg,Cu,Si/7LiF:Mg,Cu,Si and TLD-600/TLD-700 to 0.1–12 MeV neutrons, Radiat. Meas. 56 (2013) 223-227.
- [82] K. Tang, H. Cui, H. Zhu, Z. Liu and H. Fan, Newly developed highly sensitive LiF:Mg,Cu,Si TL discs with good stability to heat treatment. Radiat. Meas. 47 (2012) 185– 189.
- [83] K. Tang, H. Cui, H. Zhu, Z. Liu, H. Fan, On the Roles of Dopants in LiF:Mg,Cu,Si Thermoluminescent Material, Radiat. Prot. Dosim. 155 (2013) 141-145.
- [84] S. W. S. McKeever, Measurements of emission spectra during thermoluminescence (TL) from LiF(Mg,Cu,P) TL dosemeters, J. Phys. D: Appl. Phys. 24 (1991) 988-996.
- [85] S. Mahajna, D. Yossian and Y.S. Horowitz, Defect mechanisms in the thermoluminescence of LiF:Mg, Cu, P, Radiat. Eff. Def. Solids 136 (1995) 181-185.
- [86] A.J.J. Bos, K. Meijvogel, J.T.M. de Haas, P. Bilski, P. Olko, Thermoluminescence properties of LiF(Mg,Cu,P) with different copper concentrations, Rad. Prot. Dosim. 65 (1996) 199-202.
- [87] P.Bilski, M. Budzanowski and P. Olko, A systematic evaluation of the glow curve structure on the concentration of dopants in LiF:Mg,Cu,P, Rad. Prot. Dosim. 65 (1996) 195- 198.
- [88] T.C. Chen and T.G. Stoebe, Role of copper in LiF:Mg,Cu,P thermoluminescent phosphors, Radiat. Prot. Dosim. 78 (1998) 101–106.
- [89] P.Bilski, Lithium fluoride: from LiF:Mg,Ti to LiF:Mg,Cu,P, Radiat. Prot. Dosim. 100, (2002) 196–206.
- [90] P. Bilski, J.M. Bordy, J. Daures, M Denoziere, E. Fantuzzi, P. Ferrari, G. Gualdrini, M. Kopec, F. Mariotti, F. Monteventi, S. Wach, The new EYE-DTM dosemeter for measurements of HP (3) for medical staff, Radiat. Meas. 46 (2011) 1239-1242.
- [91] R.T. Devine, M. Moscovitch and P.K. Blake, The US Naval Dosimetry Center Thermoluminescence Dosimetry System, Radiat. Prot. Dosim. 30 (1990) 231-236.
- [92] M. Moscovitch, Personnel dosimetry using LiF:Mg,Cu,P, Radiat. Prot. Dosim. 85 (1999) 49-56.
- [93] J. R. Cassata, M. Moscovitch, J.E. Rotunda and K.J. Velbeck, A new paradigm in personal dosimetry using LiF:Mg,Cu,P, Radiat. Prot. Dosim. 101 (2002) 27-42.
- [94] M. Moscovitch, J. T. St. John, J.R. Cassata, P. K. Blake, J.E. Rotunda, M. Ramlo, K.J. Velbeck and L.Z. Luo, The application of LiF:Mg,Cu,P to large scale personnel dosimetry: current status and future directions, Radiat. Prot. Dosim. 119 (2006) 248-254.
- [95] L.A. DeWerd, J.R. Cameron, D.K. Wu, T. Papini and I.J. Das, Characterisation of a new dosemeter material;LiF(Mg,Cu,P), Radiat. Prot. Dosim. 6 (1983) 350-352.
- [96] B. C. Bhatt, S.S. Shinde and R.C. Bhatt, Comparative dosimetric studies of three LiF phosphors, Radiat. Prot. Dosim. 27 (1989) 21-27.
- [97] A.S. Pradhan and R.C. Bhatt, Thermoluminescence response of LiF(Mg,Cu,P) and LiFTLD-100 to thermal neutrons, 241Am alpha and gamma rays, Radiat. Prot. Dosim. 27 (1989) 185-188.
- [98] J.-L. Kim, B.-H. Kim, S.-Y. Chang and J.-K. Lee, Comparison of TLD Algorithms by Monochromatic Fluorescent Radiation and Continuous Spectrum X Rays, Radiat. Prot. Dosim. 101 (2002) 217-220.
- [99] J.H. Schulman, R.D. Kirk, E.J. West, Use of lithium borate for thermoluminescence dosimetry, Proceedings of the International Conference on Luminescence Dosimetry, Stanford University, CONF-650637, 1967, pp. 113-118.
- [100] M. Prokic, Progress in thermoluminescence dosimetry at The Institute of Nuclear Sciences, Vinca, Radiat. Prot. Dosim. 33 (1990) 99-102.
- [101] O. Annalakshmi, M.T. Jose and G. Amarendra, Dosimetric characteristics of manganese doped lithium tetraborate – An improved TL phosphor, Radiat. Meas. 46 (2011) 669- 675.
- [102] M. Takenaga, O. Yamamoto, T. Yamashita, A new TLD phosphor based on Li2B4O7, Proc. 5th. Intl. Conf. on Luminescence Dosimetry, Sao Paulo, Brazil, (Ed.) A. Scharmann, (1977), pp. 148-154.
- [103] A.S. Pradhan, R.C. Bhatt, K.G. Vohra, Some preparation parameters of Li2B4O7:Cu TLD phosphor, Radiochem. Radioanal. Lett. 52(2) (1982) 103-110.
- [104] M. Prokic, Lithium borate solid TL detectors, Radiat. Meas. 33 (2001) 393-396.
- [105] C. Furetta, M. Prokic, R. Salamon, V. Prokic, G. Kitis, Dosimetric characteristics of tissue equivalent thermoluminescent solid TL detectors based on lithium borate, Nucl. Instrum. Meth. Phys. Res. A 456 (2001) 411- 417.
- [106] M. Prokic, Dosimetric characteristics of Li2B4O7:Cu,Ag,P solid TL detectors, Radiat. Prot. Dosim. 100 (2002) 265-268.
- [107] Babita Tiwari, N.S.Rawat, D.G.Desai, S.G.Singh, M.Tyagi, P.Ratna, S.C. Gadkari, M.S.Kulkarni, Thermoluminescence studies on Cu-doped Li2B4O7 single crystals, J. Lumin.130 (2010) 2076–2083.
- [108] N.S. Rawat, M.S. Kulkarni, M. Tyagi, P. Ratna, D.R. Mishra, S.G. Singh, B. Tiwari, A. Soni, S.C. Gadkari, S.K. Gupta, TL and OSL studies on lithium borate single crystals doped with Cu and Ag, J. Lumin. 132 (2012) 1969-1975.
- [109] M. Martini, F. Meinardi, L. Kovács and K. Polgar, Spectrally Resolved Thermoluminescence of Li2B4O7:Cu Single Crystals, Radiat. Prot. Dosim. 65 (1996) 343-346.
- [110] B.M. Rzyski and S.P. Morato, Luminescence studies of rare earth doped lithium tetraborate, Nucl. Instrum. Meth. 175 (1980) 62-64.
- [111] L. Singh, Vibha Chopra, S.P. Lochab, Synthesis and characterization of thermoluminescent Li2B4O7 nanophosphor, J. Lumin. 131 (2011) 1177-1183.
- [112] G.D. Patra, S.G.Singh, B.Tiwari, S.Sen, D.G.Desai, S.C.Gadkari, Thermally stimulated luminescence process in copper and silver co-doped lithium tetraborate single crystals and its implication to dosimetry, J. Lumin. 137 (2013) 28-31.
- [113] A.R. Lakshmanan, B. Chandra and R.C. Bhatt, Dosimetry Characteristics of Thermoluminescent Li2B407:Cu Phosphor, Radiat. Prot. Dosim. 1 (1981) 191-198.
- [114] A.R. Lakshmanan, B. Chandra and R.C. Bhatt, Further Studies on the Radiation Dosimetry Characteristics of Thermoluminescent Li2B4O7:Cu Phosphor, Radiat. Prot.Dosim. 2 (1982) 231-239.
- [115] V.A. Kazanskaya, V.V. Kuzmin, E.E. Minaeva, A.d. Sokolov, Magnesium borate radiothermoluminescent detectors, In: Proc. 4th. Intl. Conf. on Lumin. Dosimetry, Krakow, Poland, (1974) pp.581-592.
- [116] A.R. Lakshmanan, Bhuwan Chandra, A.S. Pradhan and R.C. Bhatt, Development of MgB4O7:Dy TLD phosphor, Radiochem. Radioanal. Lett. 37 (1979) 377-382.
- [117] M. Prokic, New sintered thermoluminescent dosimeters for personnel and environmental dosimetry, Health Phys. 42 (1982) 849-855.
- [118] G. Kitis, C. Furetta, M. Prokic, V. Prokic, Kinetic parameters of some tissue equivalent thermoluminescent materials, J. Phys. D: Appl. Phys. 33 (2000) 1252-1262.
- [119] M. Prokic, Individual monitoring based on magnesium borate, Radiat. Prot. Dosim. 125(2007) 247-250.
- [120] M. Prokic, MgB4O7:Mn as a new TL dosemeter, Radiat. Prot. Dosim. 47 (1993) 191-193.
- [121] M. Prokic, Optimization of magnesium borate thermoluminescent material for radiation protection dosimetry, http://www.irpa.net/irpa9/cdrom/VOL.4/V4_120.PDF,Vienna, April 14-19, 1996, pp.4-296-4-298.
- [122] C. Furetta, M. Prokic, R. Salamon, G. Kitis, Dosimetric characterisation of a new production of MgB4O7:Dy,Na thermoluminescent material, Appl. Radiat. Isot. 52 (2000) 243-250.
- [123] L.L. Campos and O.O. Fernandes Filho, Thermoluminescent characterization of MgB4O7:Dy sintered pellets, Radiat. Prot. Dosim. 33 (1990) 111-113.
- [124] M.R. Rao, B.S. Rao, K. Somaiah and K.V.R. Murthy, Thermoluminescent characteristics of MgB4O7, MgB4O7:Mn and MgB4O7:Cu phosphors, Ind. J. Pure Appl. Phys. 47 (2009) 456-458.
- [125] O. Annalakshmi, M.T. Jose, U. Madhusoodanan, B. Venkatraman, G. Amarendra, Synthesis and thermoluminescence characterization of MgB4O7:Gd,Li, Radiat. Meas. (2013) (Accepted manuscript).(doi:10.1016/j.radmeas.2013.10.002)
- [126] Y. Fukuda, K. Mizuguchi and N. Takeuchi, Thermoluminescence in sintered CaB4O7:Dy and CaB4O7:Eu, Radiat. Prot. Dosim. 17 (1986) 397- 401.
- [127] E. Tekin (Ekdal), A. Ege, T. Karali, P.D. Townsend, M. Prokić, Thermoluminescence studies of thermally treated CaB4O7:Dy, Radiat. Meas. 45 (2010) 764-767.
- [128] C. Furetta, C. Bacci, B. Rispoli, C. Sanipoli and A. Scacco, Luminescence and Dosimetric Performances of KMgF3 Crystals Doped with Metal Impurity Ions, Radiat. Prot. Dosim. 33 (1990) 107-110.
- [129] S. V. Moharil, S. J. Dhoble, S. M. Dhopte, P. L. Muthal, V. K. Kondawar, Preparation and characterization of KMgF3:Eu phosphor, Radiat. Eff. Def. Solids 138 (1996) 159-166.
- [130] C. Bacci, S. Fioravanti, C. Furetta, M. Missouri, G. Ramogida, R. Rossetti, C. Sanipoli and A. Scacco, Photoluminescence and Thermally Stimulated Luminescence in KMgF3:Eu2+ Crystals, Radiat. Prot. Dosim. 47 (1993) 277-280.
- [131] G. Kitis, C. Furetta, C. Sanipoli and A. Scacco, Thermoluminescence Properties of KMgF3 Doped with Pb, Cr and Ag, Radiat. Prot. Dosim. 65 (1996) 93-96.
- [132] G. Kitis, C. Furetta, C. Sanipoli, and A. Scacco, KMgF3:Ce, an ultra-high sensitivity thermoluminescent material, Radiat. Prot. Dosim. 82 (1999) 151–152.
- [133] N. J. M. Le Masson, A. J. J. Bos, C. W. E. Van Eijk, C. Furetta and J. P. Chaminade, Optically and thermally stimulated luminescence of KMgF3:Ce3+ and NaMgF3:Ce3+, Radiat. Prot. Dosim. 100 (2002) 229-34.
- [134] C. Furetta, F. Santopietro, C. Sanipoli, G. Kitis, Thermoluminescent (TL) properties of the perovskite KMgF3 activated by Ce and Er impurities, Appl. Radiat. Isot. 55 (2001) 533- 542.
- [135] U. Madhusoodanan, M.T. Jose, R. Indira, T.K. Gundu Rao, Luminescence studies in KMgF3:Eu, Ag, Indian J. Pure Appl. Phys. 47 (2009) 459-460.
- [136] G. Kitis, C. Furetta and C. Sanipoli, Thermoluminescence properties of LiMgF3 doped with Ce, Er and Dy, Radiat. Prot. Dosim. 100 (2002) 247- 50.
- [137] R. Bernal, K. R. Alday-Samaniego, C. Furetta, E. Cruz-Zaragoza, G. Kitis, F. Brown and C. Cruz-Vázquez, Thermoluminescence characterization of LiMgF3:DyF3 phosphors exposed to beta radiation, Radiat. Eff. Def. Sol. 162 (2007) 699-708.
- [138] B. C. Bhatt, B. S. Dhabekar, S. S. Sanaye, S. S. Shinde, S. V. Moharil and T. K. Gundu Rao, Preparation, Dosimetric Characterisation and Investigation of Related TSL Defect Centres in Li3PO4:Mg,Cu Phosphor, Radiat. Prot. Dosim. 100 (2002) 251-253.
- [139] Manveer Singh, P.D. Sahare, Pratik Kumar, Synthesis and Dosimetry Characteristics of a New High Sensitivity TLD Phosphor NaLi2PO4:Eu3+, Radiat. Meas. (Accepted manuscript), Doi: 10.1016/j.radmeas.2013.10.002.
- [140] G. A. Aghalte, S. K. Omanwar, and S. V. Moharil, Luminescence characteristics of LiCaAlF6:Eu phosphor, Phys. Stat. Sol. (a) 204 (2007) 1561–1566.
- [141] S. J. Dhoble, S.P. Pappalwar and N.S. Dhoble, Li-based phosphors for thermoluminescence dosimetry, In: "Radiation Synthesis of Materials and Compounds", (Eds.) B. I. Kharisov, O. V. Kharissova, U. O. Mendez, CRC Press (Taylor and Francis), (2013), pp. 147-192.
- [142] S.J. Dhoble, S.P. Puppalwar, N.S. Dhoble and A.K. Mohanty, One step synthesis of Cu+ activated Li2BPO5 low Z phosphor for thermoluminescence dosimetry, Indian. J. Pure and Appl. Phys. 50 (2012) 520-523.
- [143] B. Dhabekar, S.N. Menon, E. Alagu Raja, A.K. Bakshi, A.K. Singh, M.P. Chougaonkar, Y. S. Mayya, LiMgPO4:Tb,B - A new sensitive OSL phosphor for dosimetry, Nucl. Instrum. Meth. Phys. Res. B 269 (2011) 1844–1848.
- [144] S.R. Anishia, M.T.Jose, O.Annalakshmi, V.Ponnusamy, V.Ramasamy, Dosimetric properties of rare earth doped LiCaBO3 thermoluminescence phosphors, J. Lumin. 130 (2010) 1834–1840.
- [145] S.R. Anishia, M.T.Jose, O.Annalakshmi, V.Ramasamy, Thermoluminescence properties of rare earth doped lithium magnesium borate phosphors, J.Lumin. 131 (2011) 2492-2498.
- [146] K.N. Shinde and S.J. Dhoble, Thermoluminescence and photoluminescence in the NaCaPO4:Dy3+ phosphor, Radiat. Prot. Dosim. 152 (2012) 463-467.
- [147] S.D. More, S.P. Wankhede, M. Kumar, G. Chourasiya and S.V. Moharil, Synthesis and dosimetric characterization of LiCaPO4:Eu phosphor, Radiat.Meas. 46 (2011) 196-198.
- [148] K. Ayyangar, A. R. Lakshmanan, Bhuwan Chandra, and K. Ramadas, A Comparison of Thermal Neutron and Gamma Ray Sensitivities of Common TLD Materials, Phys. Med. Biol. 19 (1974) 665- 676.
- [149] T. Toryu, H. Sakamoto, N. Kotera, H. Yumada, Compositions dependency of thermoluminescence of new phosphors for radiation dosemetry. In Proceedings of the International Conference on Luminescence, Leningrad, USSR, 1973, pp. 685–689.
- [150] A.R. Lakshmanan and K.G. Vohra, Gamma radiation induced sensitization and phototransfer in Mg2SiO4:Tb TLD phosphor, Nucl. Instrum. Meth. 159 (1979) 585-592.
- [151] A.R. Lakshmanan, S.S. Shinde, and R.C. Bhatt, Ultraviolet-induced thermoluminescence and phosphorescence in Mg2SiO4:Tb, Phys. Med. Biol. 23 (1978) 952-960.
- [152] A.R. Lakshmanan and R.C. Bhatt, Photon energy dependence of sensitized TLD phosphors, Nucl. Instrum. Meth. 171(1980) 259-263.
- [153] J. S. Jun and K. Becker, TLD with terbium-activated magnesium orthosilicate, Health Phys. 28 (1975) 459-461.
- [154] B. D. Bhasin, R. Sasidharan and C. M. Sunta, Preparation and thermoluminescent characteristics of terbium doped magnesium orthosilicate phosphor, Health Phys. 30 (1976) 139-42.
- [155] T. Nakajima, Magnesium silicate, In: Thermoluminescent materials, D.R. Vij (Ed.), PTR Prentice Hall, Englewood Cliffs, New Jersey, (1993), pp. 322-336.
- [156] T. Yamashita, N. Nada, H. Onishi, and S. Kitamura, Calcium sulphate activated by rare earth, In: Proc. Second Int. Conf. on Luminescence Dosimetry, Tennessee, USA, Sept. 23- 26, 1968, CONF 680920, (Eds.) J. A. Auxier, K. Becker, E. M. Robinson (1968), pp. 4-17.
- [157] M. Prokic, Improvement of the thermoluminescence properties of the non-commercial dosimetry phosphors CaSO4:Dy and CaSO4:Tm, Nucl. Instrum. Meth. 151(1978) 603-608.
- [158] Bhuwan Chandra and R.C. Bhatt, Effect of dysprosium concentration on the characteristics of CaSO4:Dy phosphor, Nucl. Instrum. Meth. 164 (1979) 571-577.
- [159] J. Azorin, R. Salvi, A. Moreno, Improvement in the preparation of CaSO4:Dy as a TL dosimeter, Nucl. Instrum. Meth. 175 (1980) 81-82.
- [160] I. Kasa, Dependence of Thermoluminescence Response of CaSO4:Dy and CaSO4:Tm on Grain Size and Activator Concentration, Radiat. Prot. Dosim. 33 (1990) 299-302.
- [161] S.-H. Li and P.-C. Hsu, The Role of Annealing: Effect on CaSO4:Dy Phosphor with Manganese and Sodium Impurities, Radiat. Prot. Dosim. 33 (1990) 147- 150.
- [162] A.R. Lakshmanan, photoluminescence and thermostimulated luminescence processes in rare-earth-doped CaSO4 phosphors, Progr. Mater. Sci. 44 (1999) 1-187.
- [163] A.R. Lakshmanan, M. T. Jose and O. Annalakshmi, High-sensitive CaSO4: thermoluminescent phosphor synthesis by co-precipitation technique, Radiat. Prot. Dosim. 132 (2008) 42-50.
- [164] T. Rivera, J. Romana, J. Azorin, R. Sosa, J. Guzman, A.K. Serrano, M. Garcia, G. Alarcon, Preparation of CaSO4:Dy by precipitation method to gamma radiation dosimetry, Appl. Radiat. Isot. 68 (2010) 623–625.
- [165] G.S. Rao, R.K. Iyer, Y.W. Gokhale, S.K. Gupta, S.G. Deshpande and S.S. Gupta, Preparation of CaSO4:Dy phosphor, Bhabha Atomic Research Centre, Report No. BARC/I-591 (1980).
- [166] C.M. Sunta, A review of thermoluminescence of calcium fluoride, calcium sulphate and calcium carbonate, Radiat. Prot. Dosim. 8 (1984) 25-44.
- [167] J. Azorin and A. Gutierrez, Preparation and performance of a CaSO4:Dy/Tm thermoluminescent phosphor for long-term gamma measurements, Health Phys. 56 (1989) 551-559.
- [168] M.S. Atone, S.V. Moharil and T.K. Gundu Rao, Effective co-dopants for CaSO4:Dy and CaSO4:Tm, J. Phys. D:Appl. Phys. 28 (1995) 1263-1267.
- [169] M.S. Atone, S.J. Dhoble, S.V. Moharil, S.M. Dhopte, P.L. Muthal, V.K. Kondawar, Sensitization of luminescence of CaSO4:Dy, Phys. Stat. Sol.(a) 135 (1993) 299-305.
- [170] U. Madhusoodanan, M.T. Jose, A. Tomita, A.R. Lakshmanan, New thermostimulated luminescence phosphors based on CaSO4 : Ag, RE, J. Lumin. 87-89 (2000) 1300 -1302.
- [171] M T Jose, U Madhusoodanan and A R Lakshmanan, Influence of (group IIB) codopants on the thermostimulated luminescence sensitivity of CaSO4:Dy/Tm, J. Phys. D: Appl. Phys. 4 (2001) 717-721.
- [172] S.J. Dhoble, S.V. Moharil, S.M. Dhopte, P.L. Muthal and V.K. Kondawar, Preparation and characterization of the K3Na(SO4)2:Eu, Phys. Stat. Sol.(a) 135 (1993) 289-297.
- [173] P. D. Sahare and S. V. Moharil, A new high-sensitivity phosphor for thermoluminescence dosimetry, J. Phys. D: Appl. Phys. 23 (1990) 567-570.
- [174] S. C. Gedam, S. J. Dhoble, S. K. Omanwar and S. V. Moharil, TL in halosulphate phosphors prepared by wet chemical method, Eur. Phys. J. Appl. Phys. 39 (2007) 39-43.
- [175] S. C.Gedam and S.J. Dhoble, Luminescence and evaluation of trapping parameters in NaMgSO4Cl:X ($X = Cu$ or Ce) phosphor, J. Lumin. 132 (2012) 2670-2677.
- [176] S.C. Gedam, S.J. Dhoble, R.B. Pode, 5D0-7F1 and 5D0-7F2 transition in europium doped halosulphates for mercury-free lamps, J. Lumin. 132 (2012) 2693–2696.
- [177] G. Portal, Preparation and properties of principal TL products, In: Applied Thermoluninescence Dosimetry, (Eds.) M. Oberhofer and Scharmann, Adam Hilger, Bristol, 1981, pp. 97-122.
- [178] W. Binder and J.R. Cameron, Dosimetric properties of CaF2:Dy, Health Phys. 17 (1969) 613-618.
- [179] A.C. Lucas and B.M. Kapser, The thermoluminescence of thulium doped calcium fluoride, Proc. 5th. Intl. Conf. on Luminescence Dosimetry, Sao Paulo, Brazil, (Ed.) A. Scharmann, 1977, pp. 131-139.
- [180] W. Hoffmann, G. Moller, H. Blattmann and M. Salzmann, Pion dosimetry with thermoluminescent materials, Phys. Med. Biol. 25(1980) 913-921.
- [181] B.C. Bhatt, S.S. Shinde, P.S. Iyer and K.S.V. Nambi, Relative Efficiencies of TL Peaks for Alpha and Beta Radiations in Fine Grains of High Z Phosphors, Radiat. Prot. Dosim. 62 (1995) 175-178.
- [182] W. Hoffmann, TL Dosimetry in High LET Radiotherapeutic Fields, Radiat. Prot. Dosim. 66(1996)243-248.
- [183] A.S. Pradhan, J. Rassow and W. Hoffmann, Fast Neutron Responses of CaF2: Tm Teflon TLD Discs of Different Thicknesses, Radiat. Prot. Dosim. 15 (1986) 233-236.
- [184] A. R. Lakshmanan, Bhuwan Chandra and R. C. Bhatt, Estimation of Quality and Intensity of Low Energy Photon Radiation using a Single Sample of CaF2:Tm, Int. J. Appl. Radiat. Isot. 33 (1982) 703- 706.
- [185] K. Prokert and M. Sommer, A new hypersensitive thermoluminophor based on CaF2, Radiat. Prot. Dosim. 78 (1998) 249-256.
- [186] S. K. Mehta and S. Sengupta, Gamma dosimetry with Al2O3 thermoluminescent phosphor, Phys. Med. Biol. 21 (1976) 955.
- [187] M. Osvay and T. Biro, Aluminium oxide, In:, Applied Thermoluninescence Dosimetry (Eds.) M. Oberhofer and Scharmann, Adam Hilger, Bristol, 1981, pp. 243-263.
- [188] G. Portal, S. Lorrain, Very deep traps in Al2O3 and CaSO4 : Dy, Nucl. Instrum. Meth. 175 (1980) 12-14.
- [189] P. Pokorny and A. Ibarra, On the origin of the thermoluminescence of A12O3:Cr,Ni, J. Phys.: Condens. Matter 5 (1993) 7387-7396.
- [190] A.C. Lucas and B. K. Lucas, High dose TL response of Al2O3 single crystals, Radiat. Prot. Dosim. 85 (1999) 455–458.
- [191] G. Scarpa, Dosimetric use of beryllium oxide as a thermoluminescent material- A preliminary study, Phys. Med. Biol. 15 (1970) 667-672.
- [192] K.W. Crase and R.B. Gammage, Improvements in the use of ceramic BeO for TLD, Health Phys. 29 (1975) 739-746.
- [193] L. Lembo, G. Scarpa, Beryllium oxide, In: Thermoluminescent materials, D.R. Vij (Ed.), PTR Prentice Hall, Englewood Cliffs, New Jersey, 1993, pp. 264-280.
- [194] G. Busuoli, L. Lembo, R. Nanni and I. Sermenghi, Use of BeO in Routine Personnel Dosimetry, Radiat. Prot. Dosim. 6 (1983) 317-320.
- [195] M. Sommer, A. Jahn, J. Henniger, A new personal dosimetry system for HP(10) and HP(0.07) photon dose based on OSL-dosimetry of beryllium oxide, Radiat. Meas. 46 (2011) 1818-21.
- [196] Y. Okamoto, S. Kawaguchi, S. Kino, S. Miono, T. Kitajima, A. Misaki, T. Saito, Thermoluminescent sheets for the detection of high energy hadronic and electromagnetic showers, Nucl. Instrum. Meth. Phys. Res. A 243 (1986) 219-224.
- [197] J. Azorin, C. Furetta, A. Gutierrez, P. Gonzalez, Thermoluminescence Characteristics of BaSO4: Eu, Appl. Radiat. Isot. 42 (1991) 861-863.
- [198] B.C. Bhatt, S.S. Sanaye, S.S. Shinde, J.K. Srivastava, A comparative study of the dosimetric characteristics of BaSO4: Eu and CaSO4:Dy Teflon TLD discs, Radiat. Prot. Dosim. 69 (1997) 105-110.
- [199] O. Annalakshmi, M. T. Jose and U. Madhusoodanan, Synthesis and characterisation of BaSO4:Eu thermoluminescence phosphor, Radiat. Prot. Dosim. 150 (2012) 127-133.
- [200] V.S. Kortov, Nanophosphors and outlooks for their use in ionizing radiation detecion, Radiat. Meas. 45 (2010) 512–515.
- [201] Numan Salaha, P.D. Sahare, S.P. Lochab, Pratik Kumar, TL and PL studies on CaSO4: Dy nanoparticles, Radiat. Meas. 41 (2006) 40- 47.
- [202] Numan Salaha, P.D. Sahare, A.A. Rupasov, Thermoluminescence of nanocrystalline LiF: Mg, Cu, P, J. Lumin. 124 (2007) 357–364.
- [203] Numan Salah, S.S. Habib, Z.H. Khan, S. Al-Hamedi, S.P.Lochab, Nanoparticles of BaSO4:Eu for heavy-dose measurements, J. Lumin. 129 (2009) 192–196.
- [204] S. P. Lochab, D. Kanjilal, Numan Salah, Sami S. Habib, Jyoti Lochab, Ranju Ranjan, V. E. Aleynikov, A. A. Rupasov, and A. Pandey, Nanocrystalline Ba0.97Ca0.03SO4 :Eu for ion beams dosimetry, J. Appl. Phys. 104 (2008) 033520 - 4.
- [205] P.D.Sahare, J.S.Bakare, S.D.Dhole, N.B.Ingale, A.A.Rupasov, Synthesis and luminescence properties of nanocrystalline LiF:Mg,Cu,P phosphor, J. Lumin. 130 (2010) 258–265.
- [206] L. G. Jacobsohn, M. W. Blair, S. C. Tornga, L. O. Brown, B. L. Bennett, and R. E. Muenchausen,Y2O3 :Bi nanophosphor: Solution combustion synthesis, structure, and luminescence, J. Appl. Phys.104 (2008) 124303-7.
- [207] M. Zahedifar, M. Mehrabi, S. Harooni, Synthesis of CaSO4:Mn nanosheets with high thermoluminescence sensitivity, Appl. Radiat. Isot. 69 (2011) 1002–1006.
- [208] M. Zahedifar, M. Mehrabi, Thermoluminescence and photoluminescence of cerium doped CaSO4 nanosheets, Nucl. Instrum. Meth. Phys. Res. B 268 (2010) 3517–3522.
- [209] M.Benabdesselam, P. Iacconi, D. Briand, D. Lapraz and J.E. Butler, Selected Thermoluminescent Properties in CVD Diamond Film, Radiat. Prot. Dosim. 84 (1999) 257- 60.
- [210] J. Morales, R. Bernal, C. Cruz-Vazquez, E. G. Salcido-Romero and V. M. Castaño, Thermoluminescence of Tequila-based nanodiamond, Radiat. Prot. Dosim. 139 (2010) 580- 583.
- [211] M.S. Akselrod and S.W.S. McKeever, A radiation dosimetry method using pulsed optically stimulated luminescence, Radiat. Prot. Dosim. 81(1999) 167-175.
- [212] M.S. Akselrod, L. Botter-Jensen, S.W.S. McKeever, Optically stimulated luminescence and its use in medical dosimetry, Radiat. Meas. 41 (2007) S78-S99.
- [213] L.Botter-Jensen, S.W.S. McKeever, and A.G. Wintle (Eds.), Optically Stimulated Luminescence dosimetry, Elsevier, Oxford (2003).
- [214] E.G. Yukihara, and S.W.S. McKeever (Eds.), Optically Stimulated Luminescence: Fundamentals and Applications, Wiley (2011).
- [215] E. Piesch, B. Burgkhardt, M. Fischer, H.G. Röber and S. Ugi, Properties of Radiophotoluminescent Glass Dosemeter Systems Using Pulsed Laser UV Excitation, Radiat. Prot. Dosim. 17 (1986) 293- 297.
- [216] N. Juto, Glass badge dosimetry system for large scale personal monitoring, In: Proc. of AOCRP-1, Korea, Oct. 20-24, 2002, 1-7.
- [217] M. Ranogajec-Komor, Passive solid state dosimeters in environmental monitoring personnel monitoring, In: New Techniques for the Detection of Nuclear and Radioactive Agents, G.A. Aycik (Ed.), NATO Science for Peace and Security Series – B: Physics and Biophysics, Springer Science (2009), pp. 97-111.
- [218] S.W.S. McKeever, M. Moscovitch, Topics under Debate On the advantages and disadvantages of optically stimulated luminescence dosimetry and thermoluminescence dosimetry, Radiat. Prot. Dosim. 104 (2003) 263-270.
- [219] P. Olko, Advantages and disadvantages of luminescence dosimetry, Radiat. Meas. 45 (2010) 506-511.
- [220] B.C. Bhatt, Thermoluminescence (TL), Optically Stimulated Luminescence (OSL) and Radiophotoluminescence (RPL) Dosimetry– An Overall Perspective, Radiat. Prot. Envir. 34 (2011) 6-16.
- [221] International Commission on Radiological Protection, 1990 Recommendations of the International Commission on Radiological Protection, ICRP Publication 60. (Oxford: Pergamon Press) (1991).
- [222] International Commission on Radiological Protection. General Principles for the Radiation Protection of Workers. ICRP Publication 75. Ann. ICRP 27 (1) (Oxford: Pergamon Press) (1997).
- [223] United Nations. Sources and Effects of Ionizing Radiation. Volume I: Report to the General Assembly, Scientific Annexes A and B, UNSCEAR 2008 Report. United Nations Sales and Publications E.10.XI.3 (2010).
- [224] R. Czarwinski, and M. J. Crick, Occupational exposures worldwide and revision of international standards for protection, Radiat. Prot. Dosim. 144 (2011) 2-11.
- [225] B.C.Bhatt and M.S. Kulkarni, Worldwide status of personnel monitoring using thermoluminescent (TL), optically stimulated luminescent (OSL) and radiophotoluminescent (RPL) dosimeters, Int. J. Lumin. Appl. 3 (2013) 6-10.
- [226] IEC. International Electrotechnical Commission. Radiation protection instrumentation-Passive integrating dosimetry systems for personal and environmental monitoring –Part 1: General characteristics and performance requirements, IEC/CWI 62387-1, 2007.
- [227] IEC. International Electrotechnical Commission. Radiation protection instrumentation Passive integrating dosimetry systems for personal and environmental monitoring of photon and beta radiation, IEC 62387, Edition 1.0 2012-12, Geneva, Switzerland (2012).
- [228] K.S.V. Nambi, V.N. Bapat, M. David, V.K. Sundaram, C.M. Sunta and S.D. Soman, Country-wide environmental radiation monitoring using thermoluminescence dosemeters, Radiat. Prot. Dosimi. 28 (1987) 31-38.
- [229] K.S.V. Nambi, N.K. Mehta, A.S. Basu and S. Gopalakrishnan, Validation of environmental TLDs used in Indian nuclear programmes, Radiat. Prot. Dosim. 58 (1995) 229-231.
- [230] M.P. Chougaonkar, P.G. Shetty, Y.S. Mayya, V.D. Puranik, M.L. Joshi, H.S. Kushwaha Environmental Gamma Radiation Monitoring Around Nuclear Power Stations in India, an Indian Scenario. J. Nucl. Sci. and Tech. (Suppl. 5) (2008) 619-622.
- [231] G.A. Klemic, N. Azziz, S.A. Marino, The Neutron Response of Al2O3:C, 7LiF:Mg,Cu,P and 7LiF:Mg,Ti TLDs, Radiat. Prot. Dosim. 65 (1996) 221-226.
- [232] F. Spurný, Enhancement of fast neutron response of some luminescent detectors due to external proton radiators, Radiat. Prot. Dosim. 9 (1984) 257-261.
- [233] E.G. Yukiharaa, J.C. Mittania, F. Vanhavere, M.S. Akselrod, Development of new optically stimulated luminescence (OSL) neutron dosimeters, Radiat Meas. 43 (2008) 309.
- [234] T. Kron, Applications of Thermoluminescence Dosimetry in Medicine, Radiat. Prot. Dosim. 85, (1999) 333-340.
- [235] A.S. Pradhan, J.I. Lee, J.L. Kim, Recent developments of optically stimulated luminescence materials and techniques for radiation dosimetry and clinical applications, J. Med. Phys. 33 (2008)85-99.
- [236] D. Banerjee, L. Botter-Jensena, A.S. Murray, Retrospective dosimetry: estimation of the dose to quartz using the single-aliquot regenerative-dose protocol, Appl. Radiat. Isot. 52 (2000) 831- 844.
- [237] H.Y. Goksu, Telephone chip-cards as individual dosemeters, Radiat. Meas. 37 (2003) 617- 620.
- [238] V.K. Mathur, J.H. Barkyoumb, E.G.Yukihara, H.Y. Göksu, Radiation sensitivity of memory chip module of an ID card, Radiat. Meas. 42 (2007) 43-48.
- [239] C. Woda, S. Greilich, K. Beerten, On the OSL curve shape and preheat treatment of electronic components from portable electronic devices, Radiat. Meas. 45 (2010) 746–748.
- [240] E. A. Ainsbury, E. Bakhanova, J. F. Barquinero, M. Brai, V. Chumak et al., Review of retrospective dosimetry techniques for external ionising radiation exposures, Radiat. Pro. Dosim.147 (2011) 573-592.
- [241] A.R. Lakshmanan and R.C. Bhatt, High-level gamma-ray dosimetry using common TLD phosphors, Phys. Med. Biol. 24 (1979) 1258-67.
- [242] R.C. Bhatt and S.J. Supe, High level γ-dosimetry using CaSO4: Dy phosphor with high Dyconcentration, Int. J. Appl. Radiat. Isot. 32 (1981) 553-558.
- [243] Bhuwan Chandra, Thermoluminescence studies on some common TL phosphors and their application in Radiation dosimetry, Ph. D. Thesis , University of Bombay, 1982 (Unpublished).
- [244] B. Obryk, P. Bilski and P. Olko, Method of thermoluminescent measurement of radiation doses from micro-Grays up to a mega-Gray with a single LiF:Mg,Cu,P detector, Radiat. Prot. Dosim. 144 (2011) 543-47.
- [245] V. Kortov, Yu. Ustyantsev, Advantages and challenges of high-dose thermoluminescent detectors, Radiat. Meas . 56(2013) 299-302.
- [246] Anuj Soni, D.R. Mishra, B.C. Bhatt, S.K. Gupta, N.S. Rawat, M.S. Kulkarni, D.N. Sharma, Characterization of deep energy level defects in a-Al2O3:C using thermally assisted OSL, Radiat. Meas. 47(2012) 111-120.
- [247] S. W. S. McKeever, New Millennium Frontiers of Luminescence Dosimetry, Radiat. Meas.100 (2002) 27-32.
- [248] E.G. Yukihara, R. Gaza, S.W.S. McKeever, C.G. Soares, Optically stimulated luminescence and thermoluminescence efficiencies for high-energy heavy charged particle irradiation in Al2O3:C, Radiat. Meas. 38 (2004) 59-70.
- [249] E.G.Yukihara, G.O. Sawakuchi, S. Guduru, S.W.S. McKeever, R. Gaza, E.R. Benton, N.Yasuda,Y. Uchihori, H. Kitamura, Application of the optically stimulated luminescence (OSL) technique in space dosimetry, Radiat. Meas. 41 (2006) 1126-1135.

Luminescence Related Phenomena and their Applications

[10.4028/www.scientific.net/DDF.347](http://dx.doi.org/10.4028/www.scientific.net/DDF.347)

Thermoluminescent Phosphors for Radiation Dosimetry

[10.4028/www.scientific.net/DDF.347.179](http://dx.doi.org/10.4028/www.scientific.net/DDF.347.179)